



US009289306B2

(12) **United States Patent**
Goldberg et al.

(10) **Patent No.:** **US 9,289,306 B2**
(45) **Date of Patent:** **Mar. 22, 2016**

(54) **HUMERAL ARTHROPLASTY**

(71) Applicant: **Catalyst Orthopaedics LLC**, Naples, FL (US)

(72) Inventors: **Steven Scott Goldberg**, Naples, FL (US); **Daniel F. Justin**, Orlando, FL (US)

(73) Assignee: **CATALYST ORTHOPAEDICS LLC**, Naples, FL (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 51 days.

(21) Appl. No.: **14/069,154**

(22) Filed: **Oct. 31, 2013**

(65) **Prior Publication Data**

US 2014/0277522 A1 Sep. 18, 2014

Related U.S. Application Data

(60) Provisional application No. 61/794,348, filed on Mar. 15, 2013.

(51) **Int. Cl.**
A61F 2/40 (2006.01)
A61F 2/30 (2006.01)

(52) **U.S. Cl.**
CPC **A61F 2/4014** (2013.01); **A61F 2/4003** (2013.01); **A61F 2002/3028** (2013.01); **A61F 2002/30278** (2013.01); **A61F 2002/30803** (2013.01); **A61F 2002/30892** (2013.01); **A61F 2002/4007** (2013.01)

(58) **Field of Classification Search**
CPC **A61F 2/36–2/3676**; **A61F 2/3859**; **A61F 2/3877**; **A61F 2/4059**; **A61F 2002/30118**; **A61F 2002/3012**; **A61F 2002/4085**; **A61F 2002/4018**; **A61F**

2002/4022; **A61F 2002/4241–2002/4248**; **A61F 2/4014–2/4261**; **A61F 2002/30112**; **A61F 2002/30121**; **A61F 2002/30123**; **A61F 2002/30199**; **A61F 2002/30245–2002/30261**
USPC **623/21.12–21.14**, **22.43**, **23.12**, **23.11**, **623/23.15**, **19.11–19.14**
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,106,130	A	8/1978	Scales	
4,206,517	A	6/1980	Pappas et al.	
4,550,450	A	11/1985	Kinnett	
D285,968	S *	9/1986	Kinnett	D24/155
4,986,833	A	1/1991	Worland	
5,032,132	A *	7/1991	Matsen et al.	623/19.11
5,370,702	A	12/1994	Jones	
5,489,309	A	2/1996	Lackey	
5,549,682	A	8/1996	Roy	
5,549,684	A *	8/1996	Amino et al.	623/20.35
5,593,450	A *	1/1997	Scott et al.	623/20.18
5,776,200	A	7/1998	Johnson	

(Continued)

FOREIGN PATENT DOCUMENTS

EP	1518519	3/2005
EP	2446859	5/2012

(Continued)

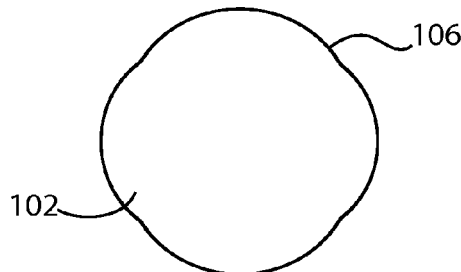
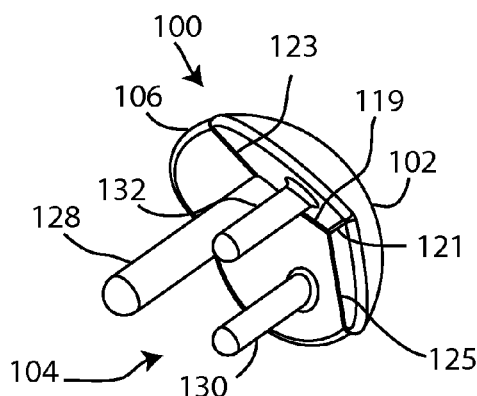
Primary Examiner — Alvin Stewart

(74) *Attorney, Agent, or Firm* — Maywood IP Law; G. Jo Hays; David W. Meibos

(57) **ABSTRACT**

Arthroplasty components include an articular surface and a bone-facing surface. The bone-facing surface includes a concave arrangement of planar surfaces which converge as they approach a middle portion of the articular surface. Instruments and implantation methods are also disclosed.

20 Claims, 66 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

5,800,551	A	9/1998	Williamson	
5,800,557	A *	9/1998	Elhami	623/23.12
5,876,456	A	3/1999	Sederholm	
5,928,285	A	7/1999	Bigliani	
5,938,700	A *	8/1999	Lippincott, III	623/21.15
5,944,758	A	8/1999	Mansat	
5,961,555	A	10/1999	Huebner	
6,056,777	A	5/2000	McDowell	
6,139,582	A	10/2000	DeCarlo, Jr.	
6,152,960	A *	11/2000	Pappas	623/20.31
6,162,256	A	12/2000	Ostiguy, Jr.	
6,171,340	B1	1/2001	McDowell	
6,171,341	B1	1/2001	Boileau	
6,187,012	B1	2/2001	Masini	
6,197,062	B1	3/2001	Fenlin	
6,197,063	B1	3/2001	Dews	
6,228,120	B1	5/2001	Leonard	
6,245,074	B1	6/2001	Allard	
6,379,386	B1	4/2002	Resch	
6,398,812	B1	6/2002	Masini	
6,508,840	B1	1/2003	Rockwood, Jr.	
6,520,964	B2 *	2/2003	Tallarida et al.	606/71
6,673,115	B2	1/2004	Resch	
6,679,917	B2 *	1/2004	Ek	623/20.14
6,783,549	B1	8/2004	Stone et al.	
7,160,329	B2	1/2007	Cooney, III	
7,255,717	B2 *	8/2007	Park et al.	623/23.12
7,294,149	B2	11/2007	Hozack	
7,517,364	B2 *	4/2009	Long et al.	623/19.14
7,621,962	B2	11/2009	Lakin	
7,670,382	B2 *	3/2010	Parrott et al.	623/19.14
8,007,538	B2	8/2011	Gunther	
8,128,704	B2 *	3/2012	Brown et al.	623/20.15
8,157,866	B2	4/2012	Winslow	
8,308,809	B2 *	11/2012	Bishop et al.	623/22.12
8,361,163	B2 *	1/2013	Quaid	623/23.12
8,439,978	B2 *	5/2013	Ebbitt	623/23.12
8,444,646	B2	5/2013	Long	
8,465,548	B2	6/2013	Long	
8,690,958	B2 *	4/2014	Klawitter et al.	623/23.12
8,747,478	B2 *	6/2014	Ries et al.	623/20.18
D721,459	S	1/2015	Smith	
D723,692	S	3/2015	Meyer	
2001/0047210	A1	11/2001	Wolf	
2002/0082702	A1	6/2002	Resch	
2003/0135280	A1 *	7/2003	Kopylov et al.	623/21.12
2003/0181984	A1 *	9/2003	Abendschein	623/20.19
2003/0204263	A1	10/2003	Justin et al.	
2004/0193276	A1 *	9/2004	Maroney et al.	623/19.14
2004/0193277	A1 *	9/2004	Long et al.	623/19.14
2004/0225367	A1 *	11/2004	Glien et al.	623/19.14
2005/0049709	A1	3/2005	Tornier	
2005/0177242	A1 *	8/2005	Lotke	623/20.19
2006/0009852	A1 *	1/2006	Winslow et al.	623/19.14
2006/0036328	A1 *	2/2006	Parrott et al.	623/19.14
2006/0111787	A1	5/2006	Bailie et al.	
2006/0247790	A1 *	11/2006	McKay	623/23.44
2007/0112431	A1 *	5/2007	Kofoed	623/21.18
2007/0219638	A1	9/2007	Jones	
2007/0225818	A1	9/2007	Reubelt	
2008/0004709	A1 *	1/2008	O'Neill et al.	623/20.35
2008/0021564	A1 *	1/2008	Gunther	623/19.14
2008/0188855	A1 *	8/2008	Brown et al.	606/88
2008/0188942	A1 *	8/2008	Brown et al.	623/20.15
2008/0221700	A1 *	9/2008	Howald et al.	623/23.12
2009/0043397	A1 *	2/2009	Park	623/23.11
2009/0192621	A1	7/2009	Winslow et al.	
2009/0198341	A1 *	8/2009	Choi et al.	623/21.18
2009/0226068	A1	9/2009	Fitz	
2009/0248170	A1 *	10/2009	Tuke et al.	623/23.11
2009/0281583	A1 *	11/2009	Brown et al.	606/86 R
2009/0326663	A1 *	12/2009	Dun	623/20.21
2010/0076567	A1 *	3/2010	Justin et al.	623/20.35
2010/0076570	A1 *	3/2010	Band et al.	623/23.12
2010/0161068	A1 *	6/2010	Lindner et al.	623/21.15
2010/0174379	A1 *	7/2010	McMinn	623/20.35
2010/0241235	A1	9/2010	Basamania	
2010/0305713	A1 *	12/2010	Grundei	623/23.12
2011/0153026	A1 *	6/2011	Heggendorn et al.	623/20.35
2011/0230972	A1	9/2011	Katrana	
2012/0130498	A1	5/2012	Long	
2012/0130500	A1	5/2012	Moroney	
2012/0136443	A1 *	5/2012	Wenzel	623/17.14
2012/0209392	A1	8/2012	Angibaud	
2012/0296436	A1	11/2012	Klawitter et al.	
2012/0310360	A1	12/2012	Parott	
2013/0024000	A1	1/2013	Bojarski	
2013/0226305	A1 *	8/2013	Donno et al.	623/20.35
2014/0121709	A1 *	5/2014	Gonzalez-Hernandez	606/286
2014/0121780	A1 *	5/2014	Faure et al.	623/20.35
2015/0045901	A1 *	2/2015	Brown et al.	623/20.35
2015/0045902	A1 *	2/2015	Perler	623/21.18

FOREIGN PATENT DOCUMENTS

EP	2474288	9/2013
WO	WO9815241	4/1998
WO	WO0018335	4/2000
WO	WO0217822	3/2002
WO	WO2006110896	10/2006
WO	WO2012030794	A1 3/2012
WO	WO2013020026	A1 2/2013
WO	WO2014005644	1/2014

* cited by examiner

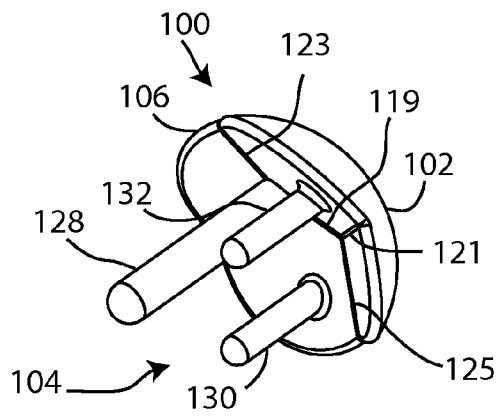


Fig. 1A

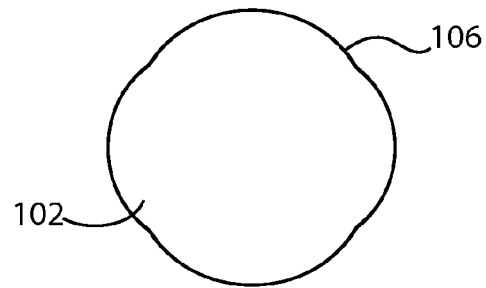


Fig. 1B

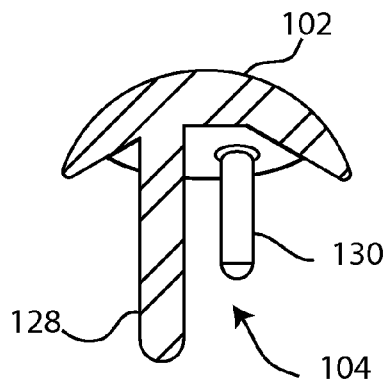


Fig. 1C

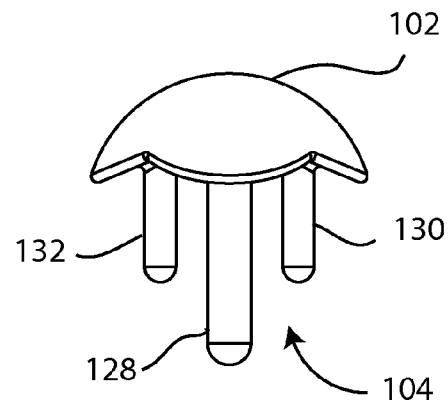


Fig. 1D

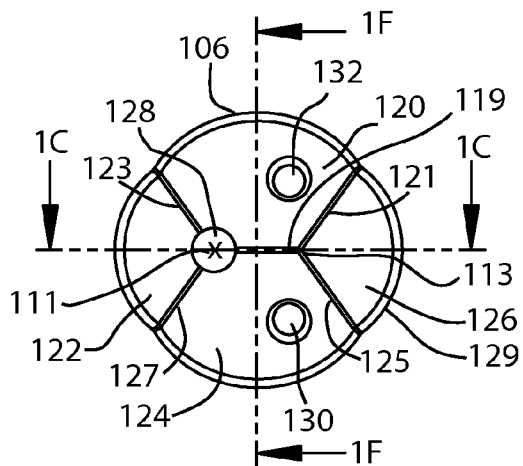


Fig. 1E

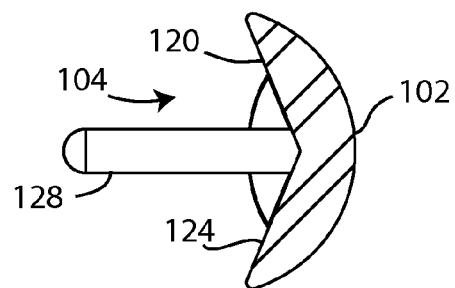
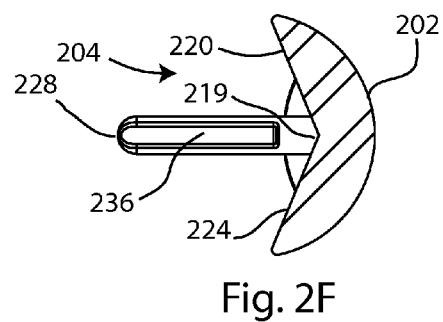
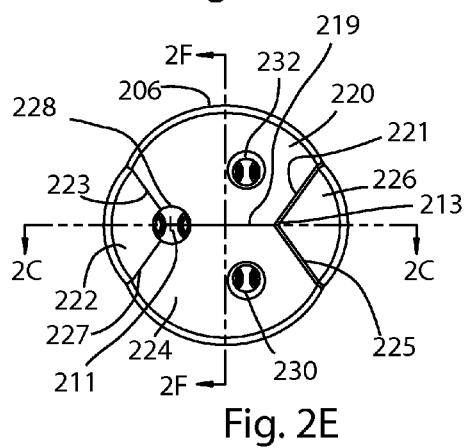
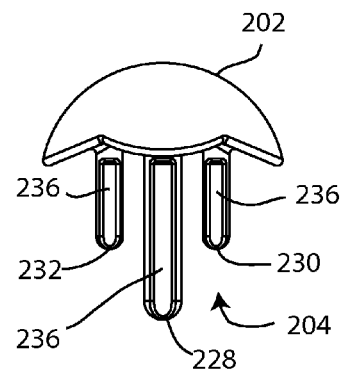
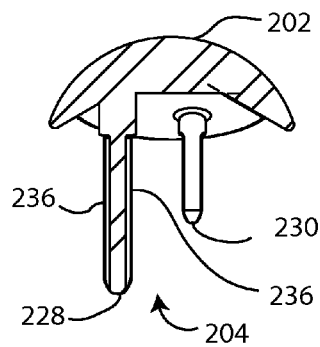
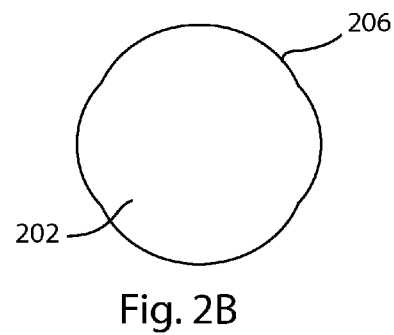
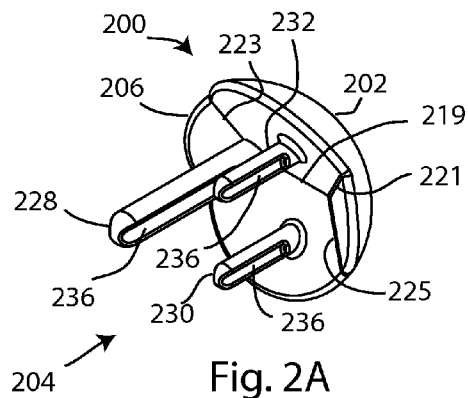
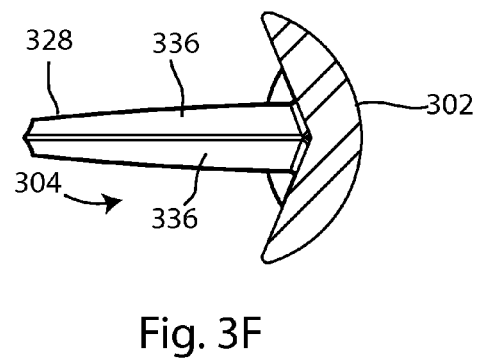
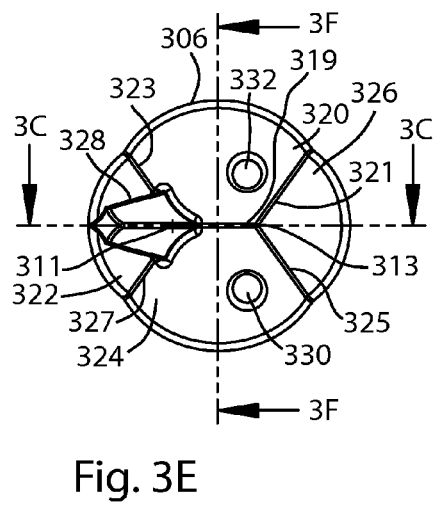
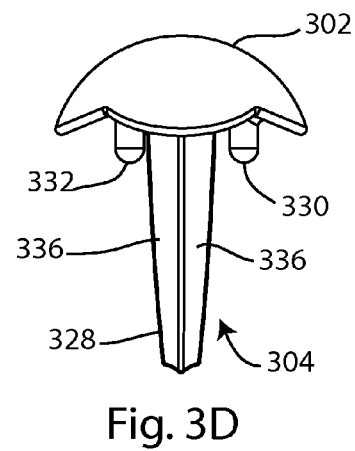
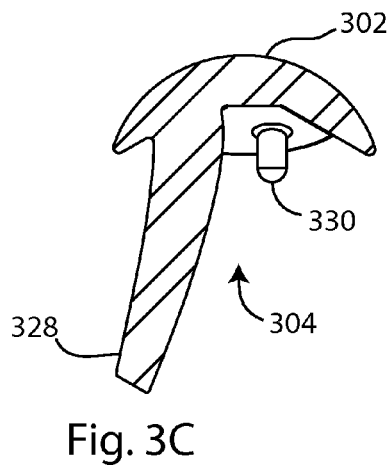
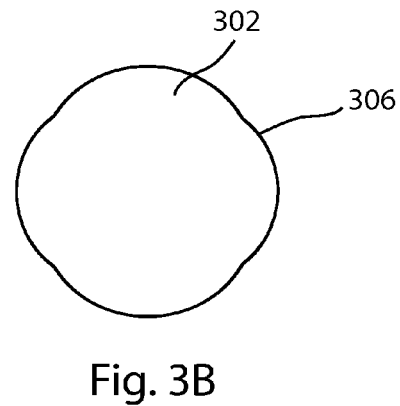
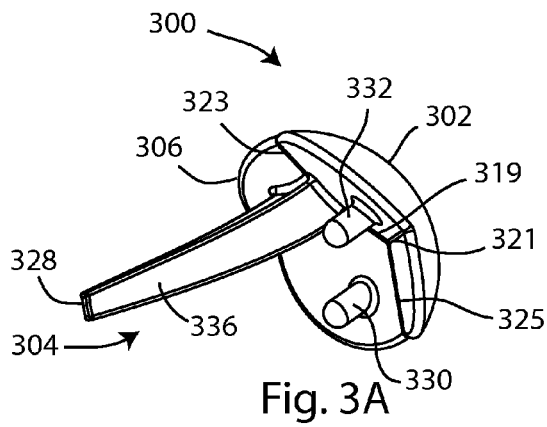


Fig. 1F





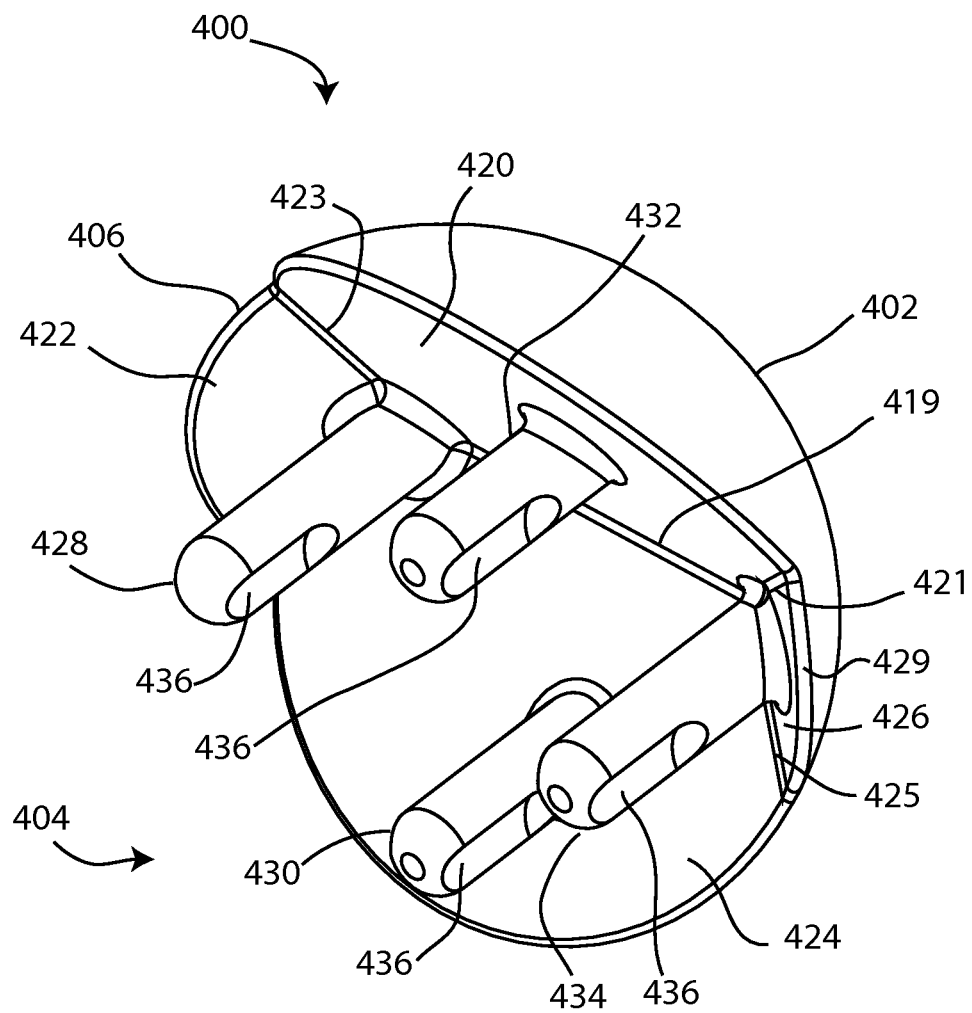


Fig. 4A

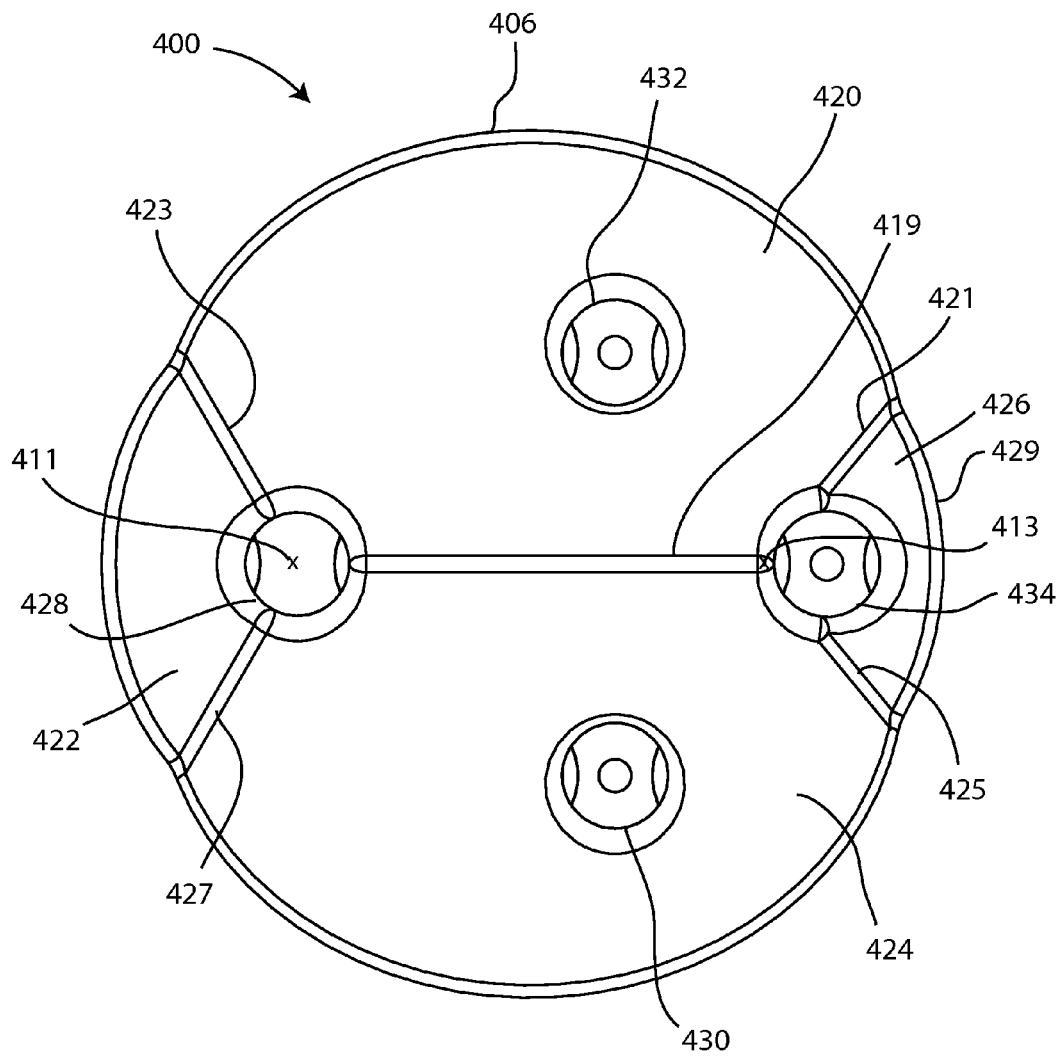


Fig. 4B

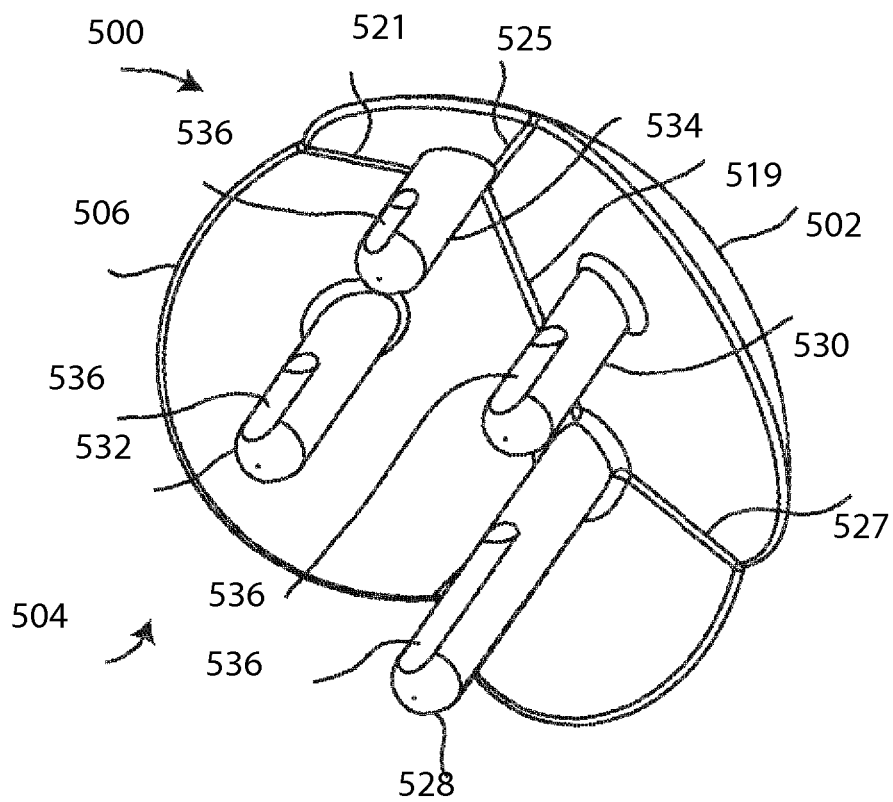


Fig. 5A

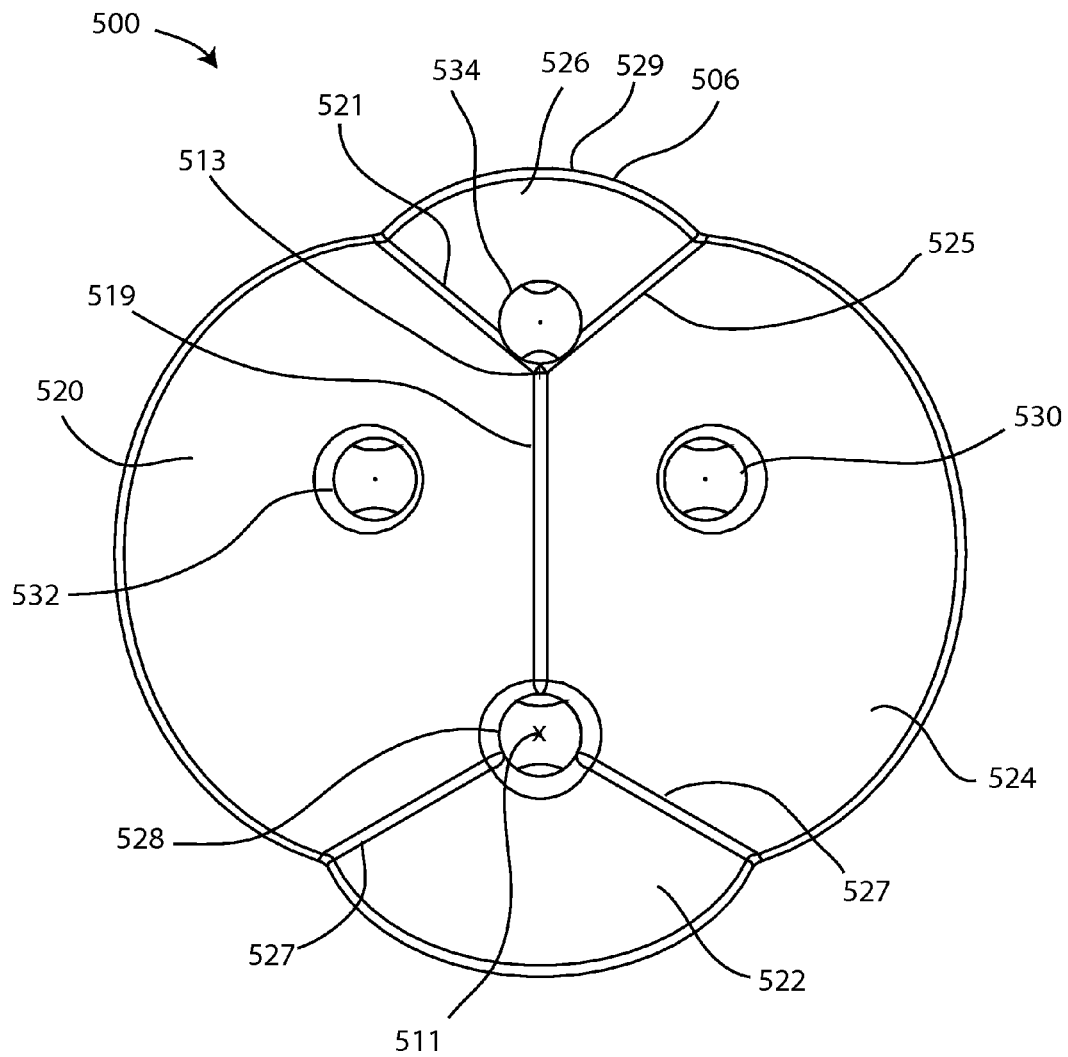


Fig. 5B

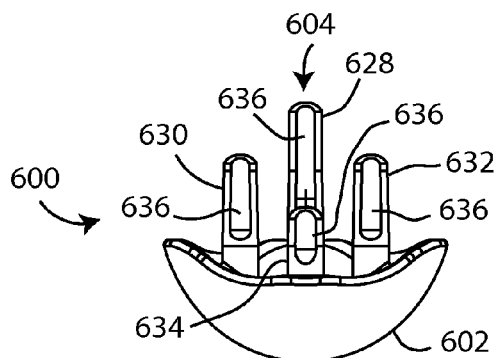


Fig. 6A

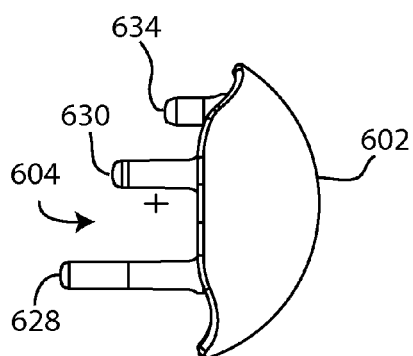


Fig. 6B

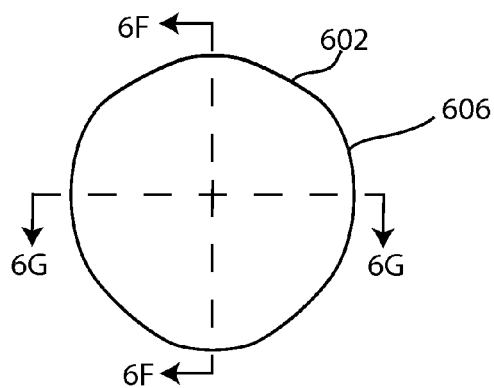


Fig. 6C

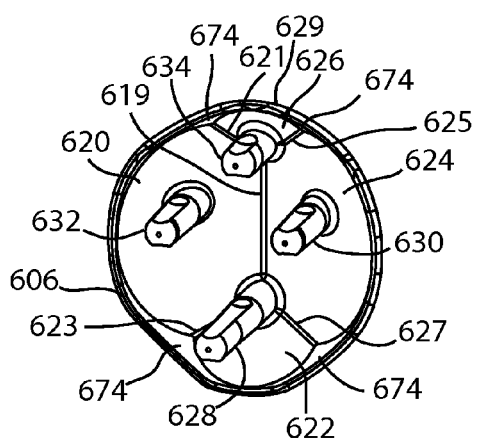


Fig. 6D

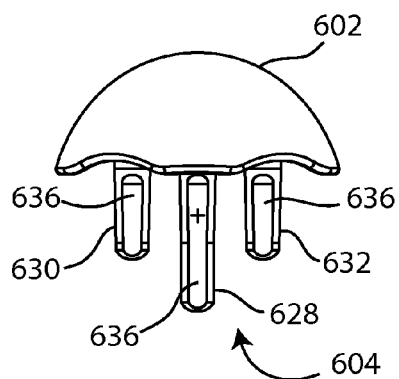
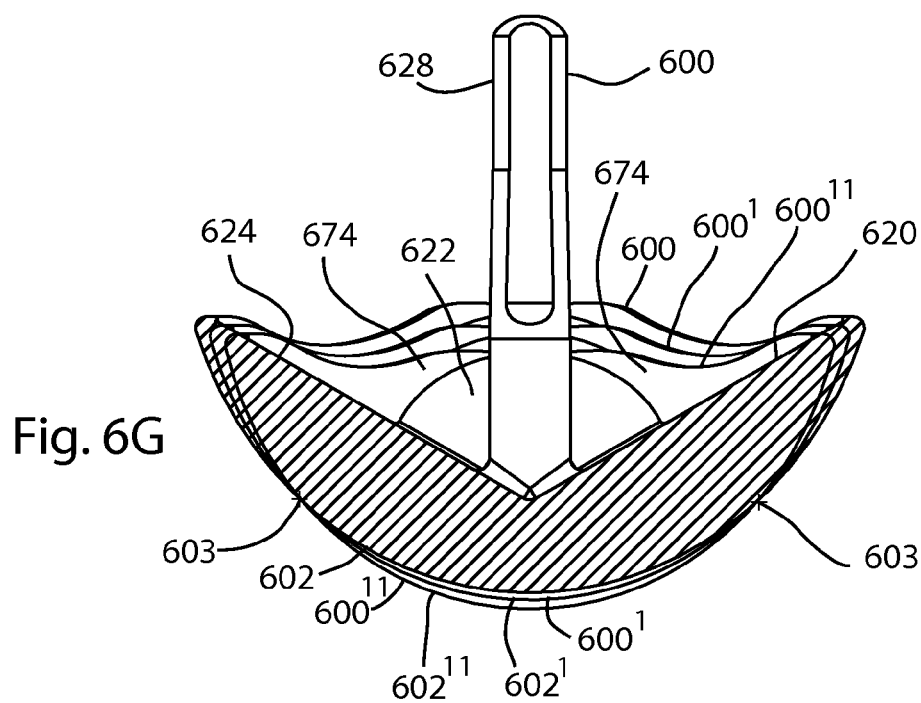
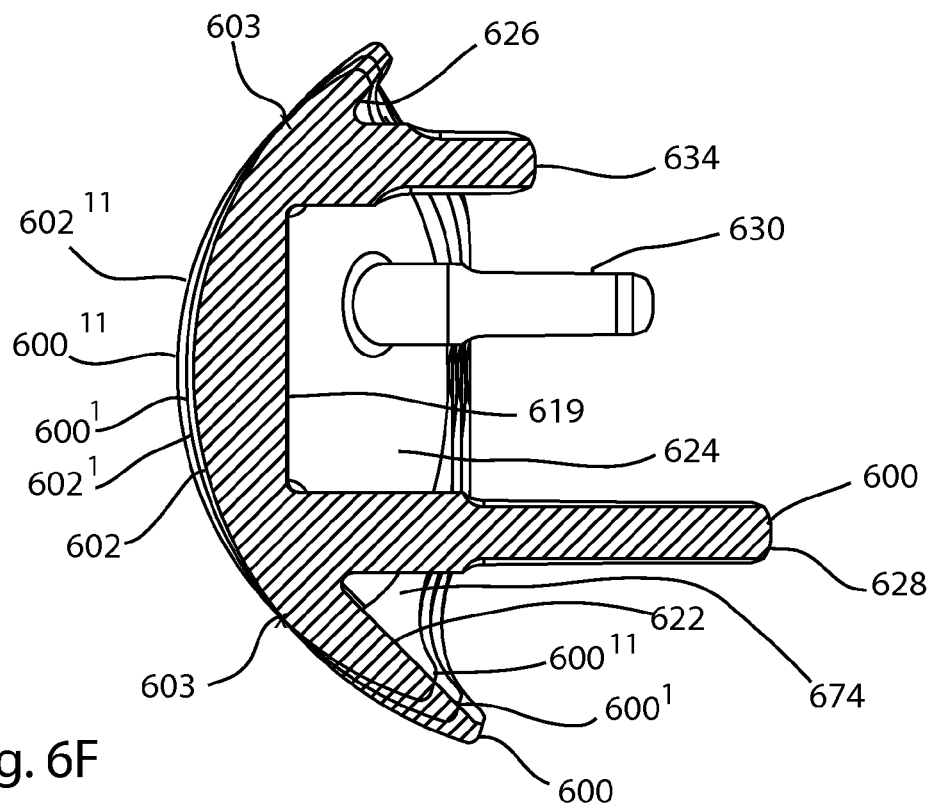


Fig. 6E



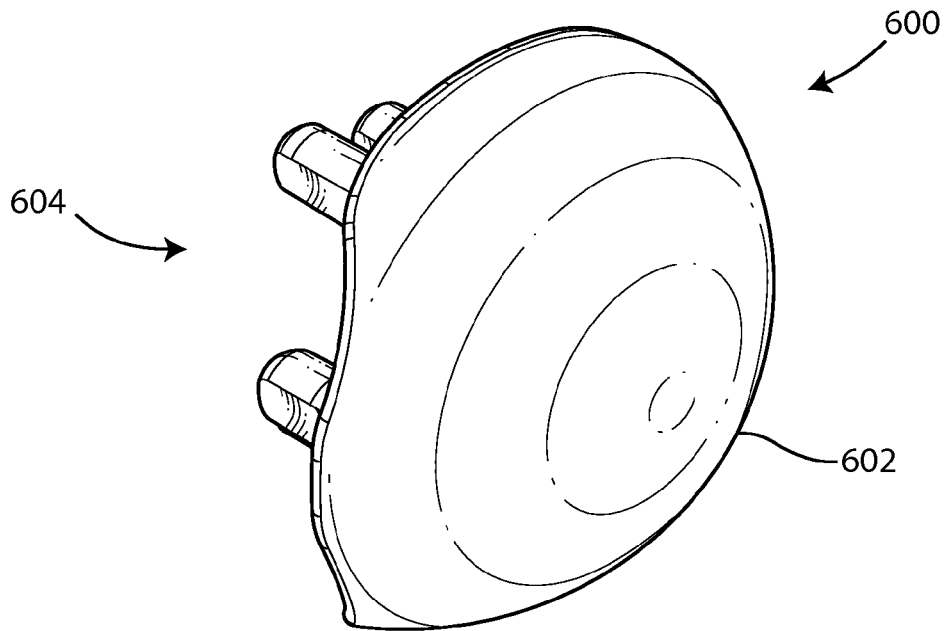


Fig. 6H

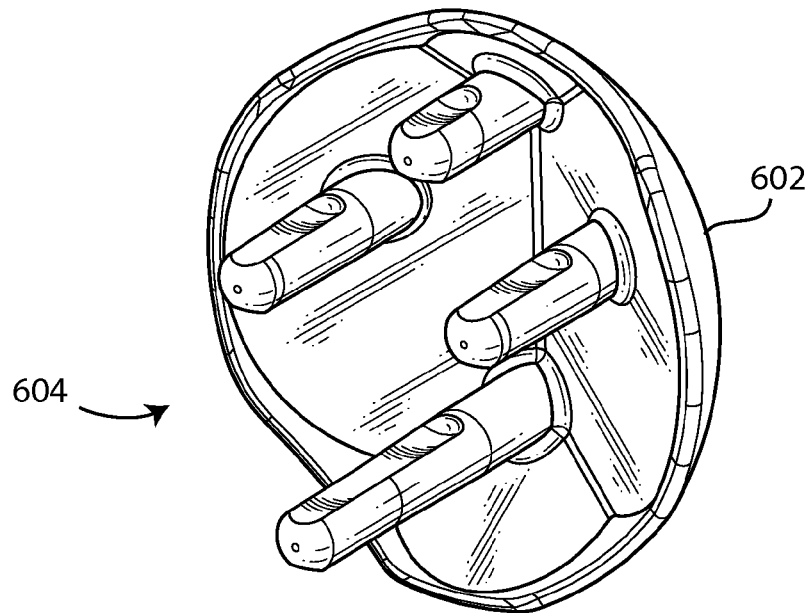


Fig. 6I

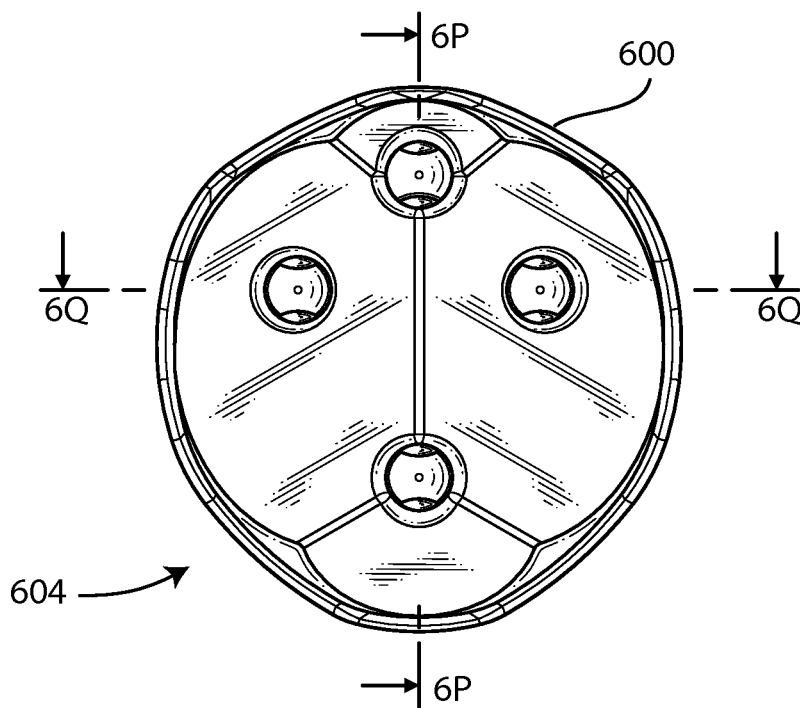


Fig. 6J

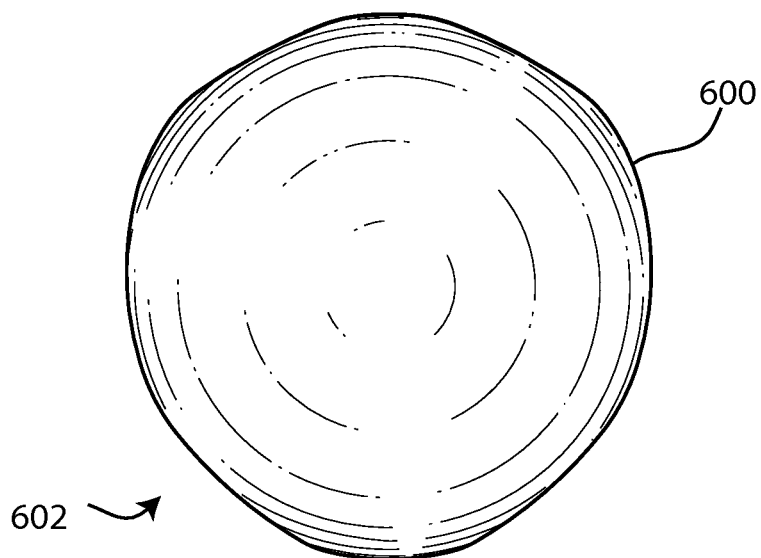


Fig. 6K

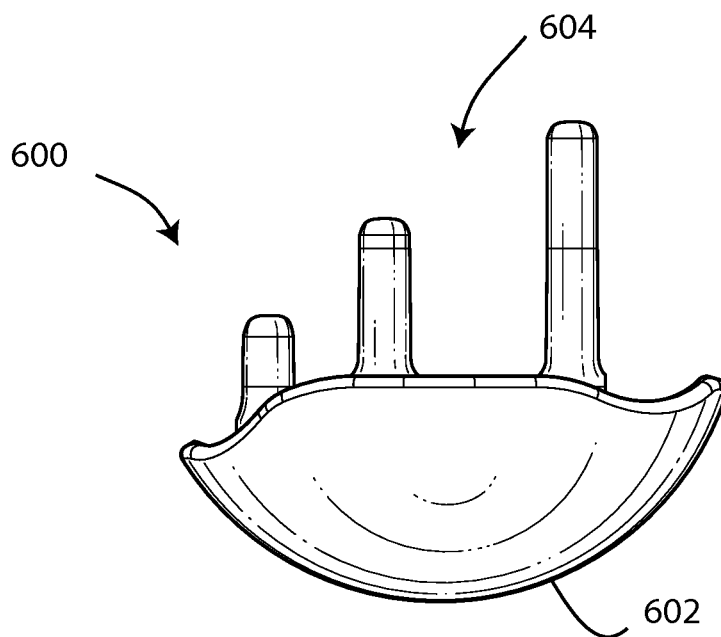


Fig. 6L

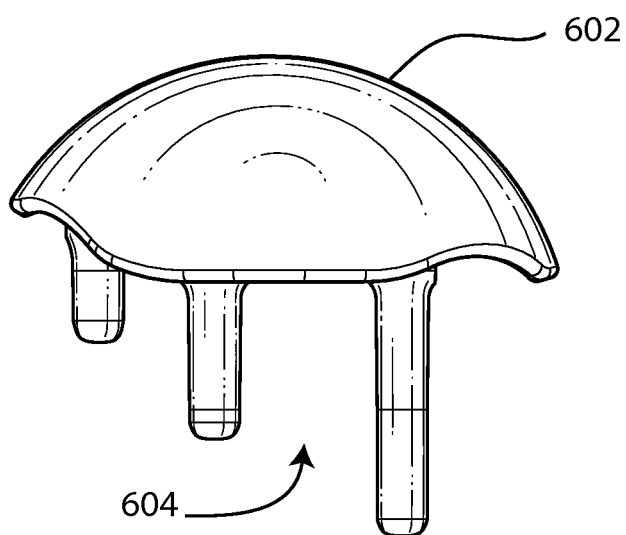


Fig. 6M

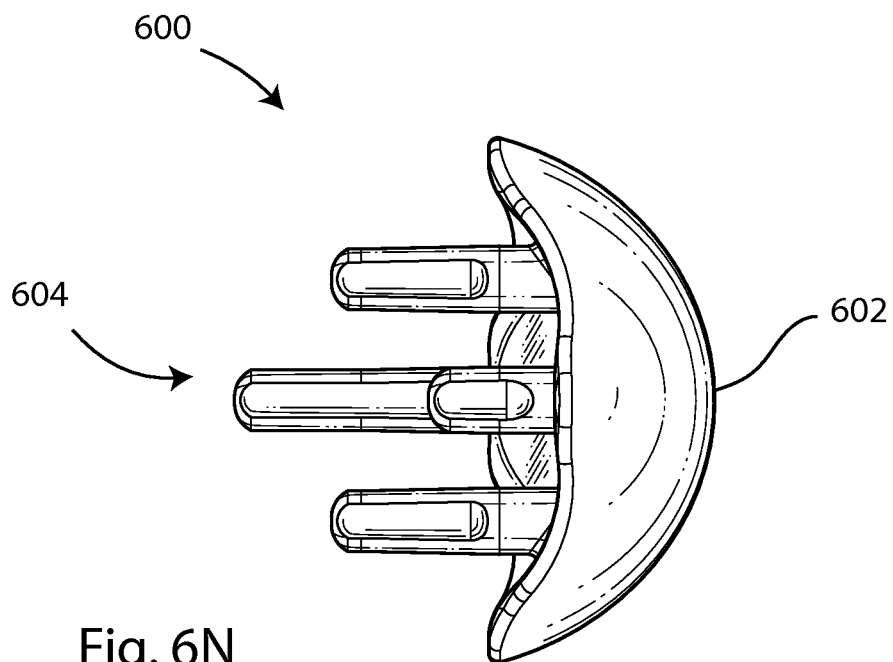


Fig. 6N

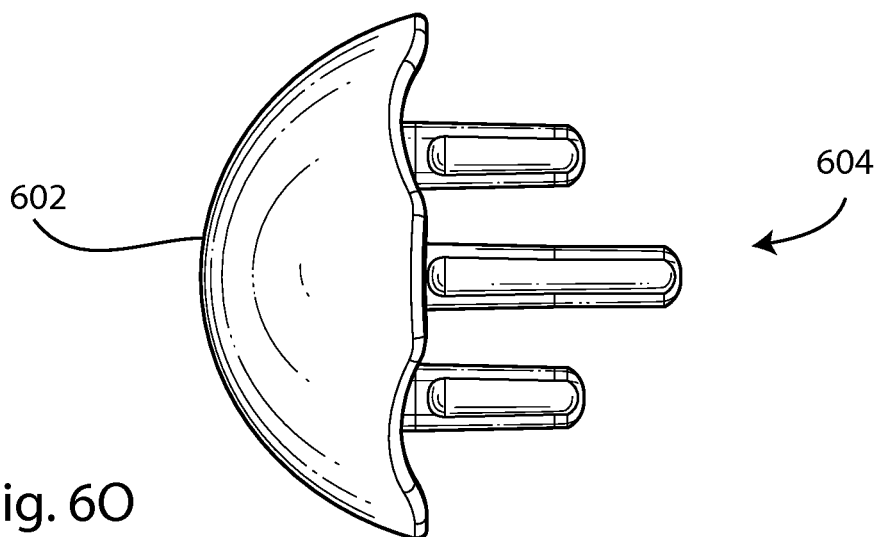


Fig. 6O

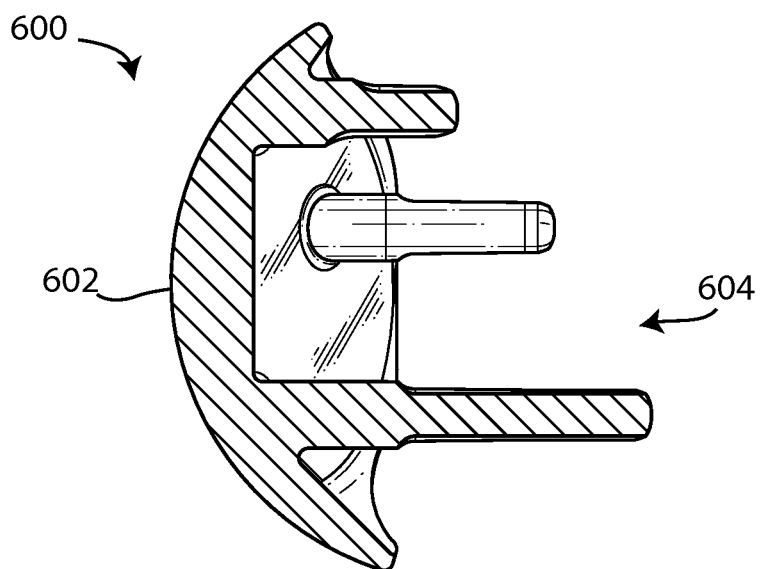


Fig. 6P

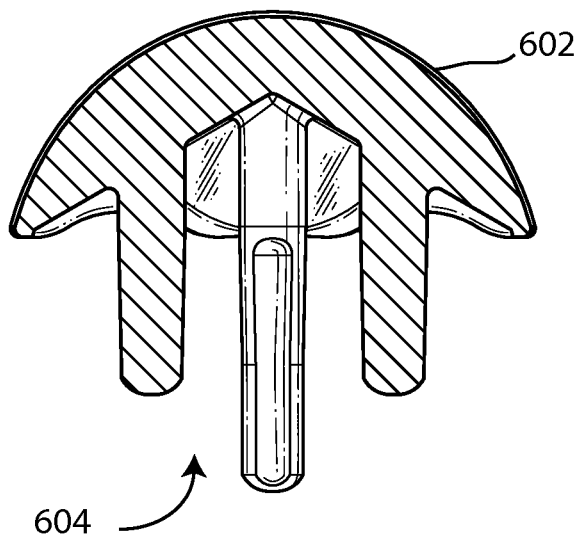
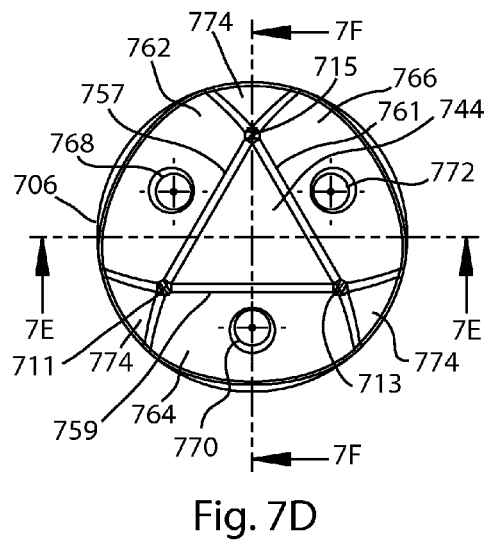
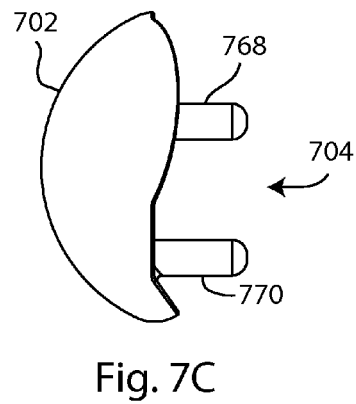
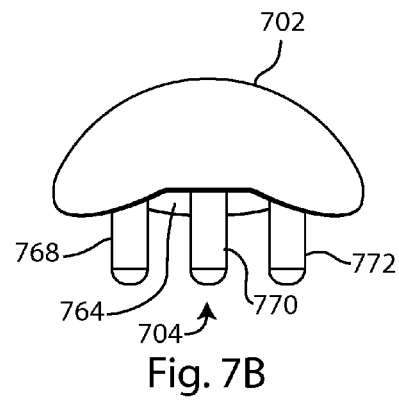
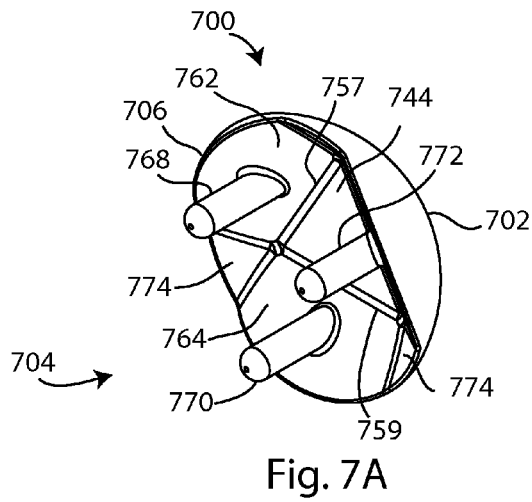


Fig. 6Q



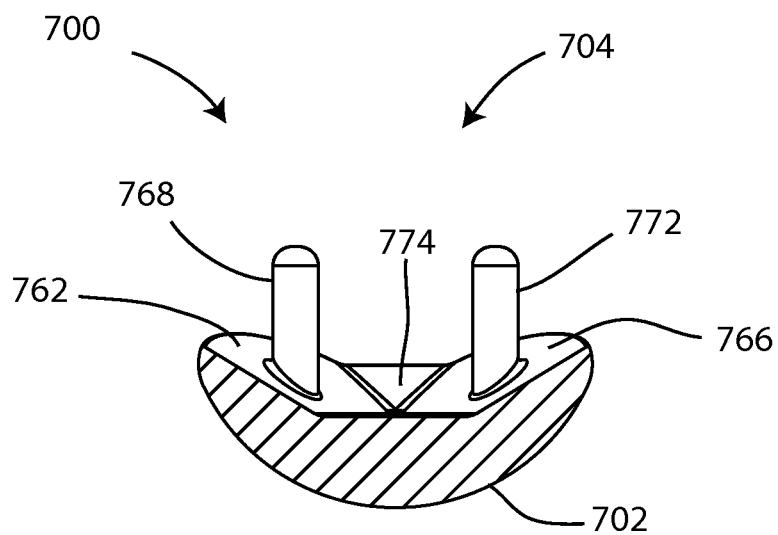


Fig. 7E

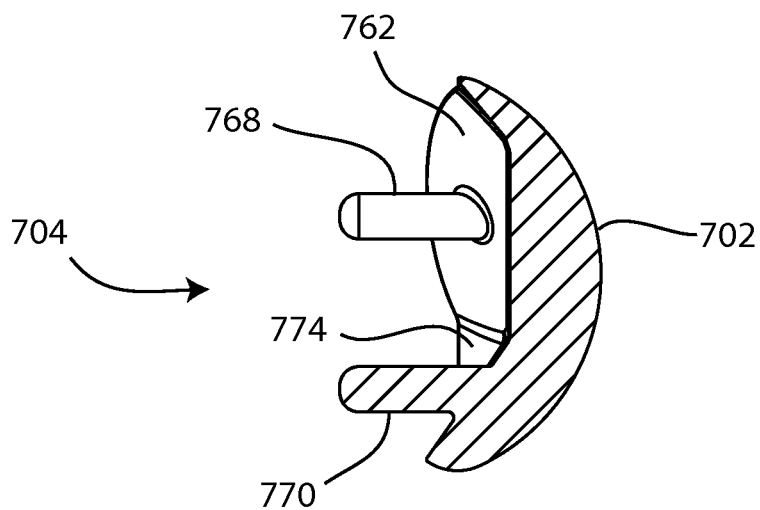


Fig. 7F

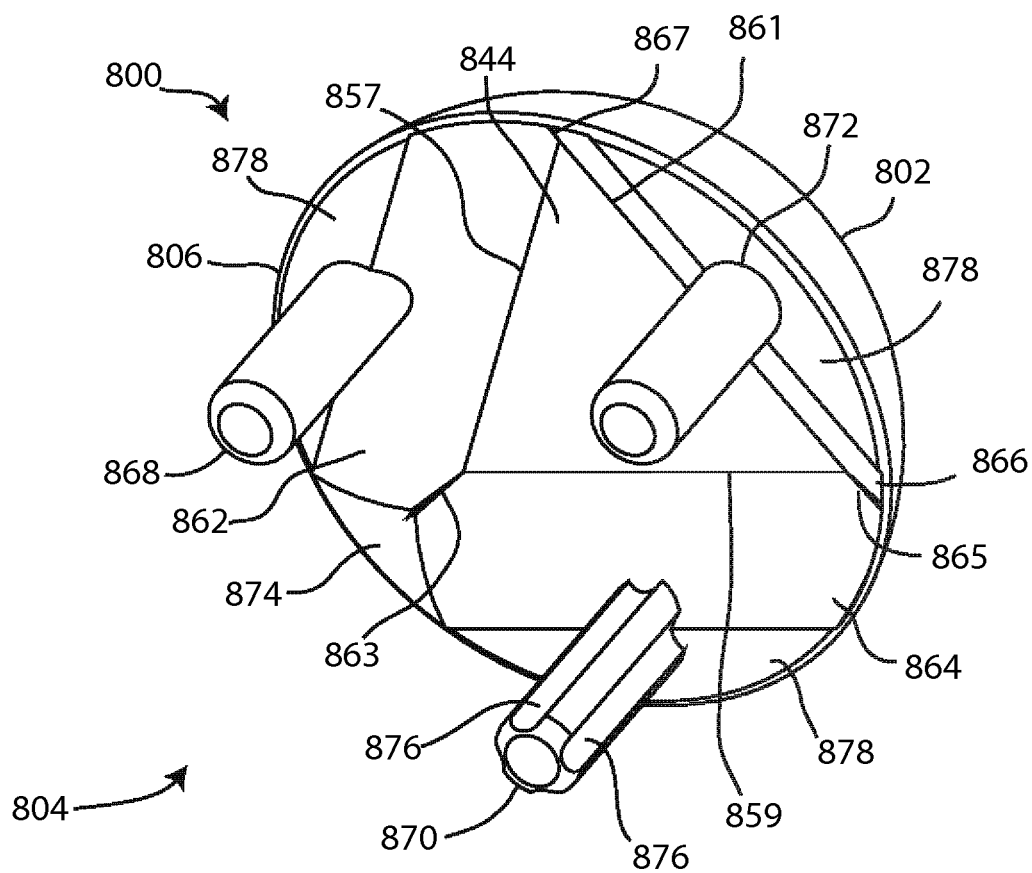


Fig. 8A

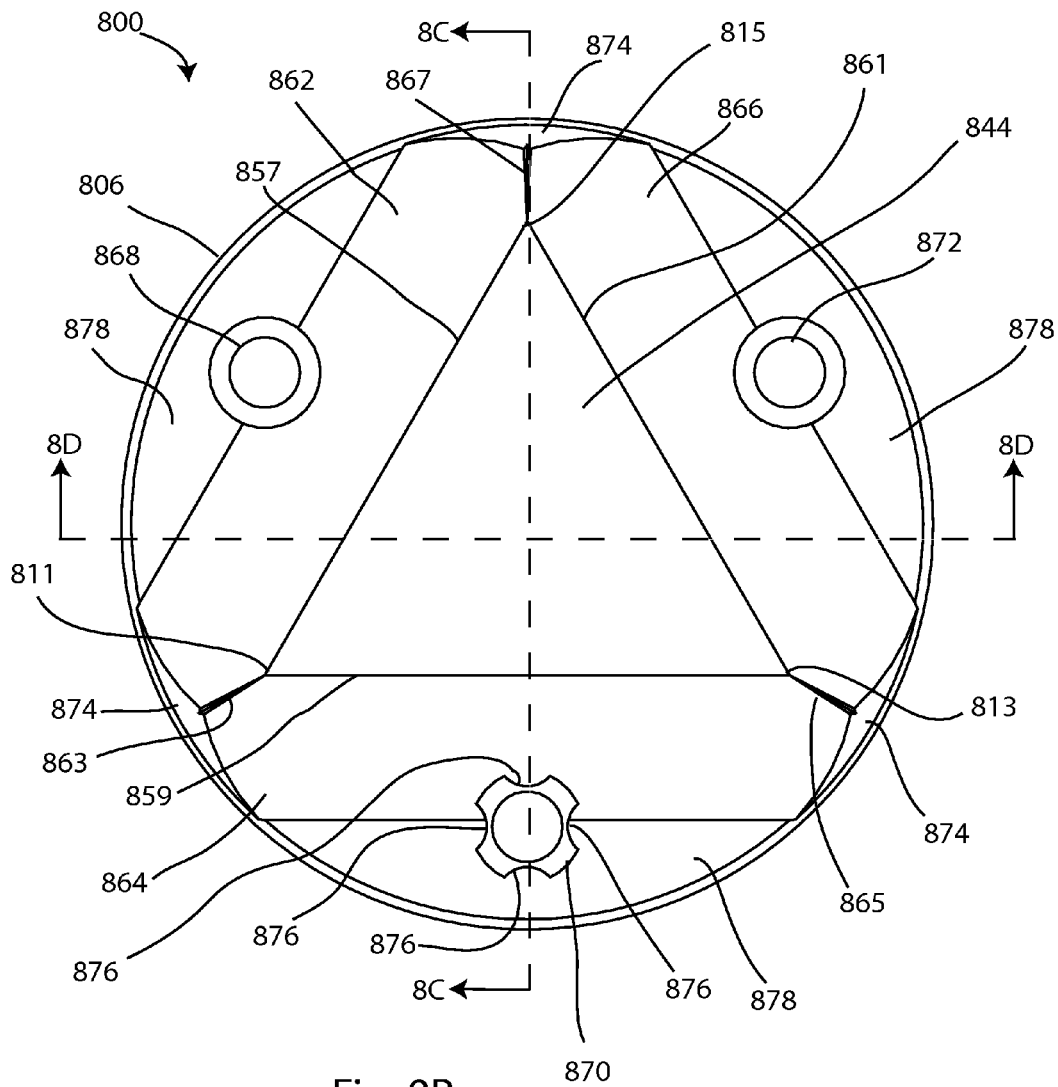


Fig. 8B

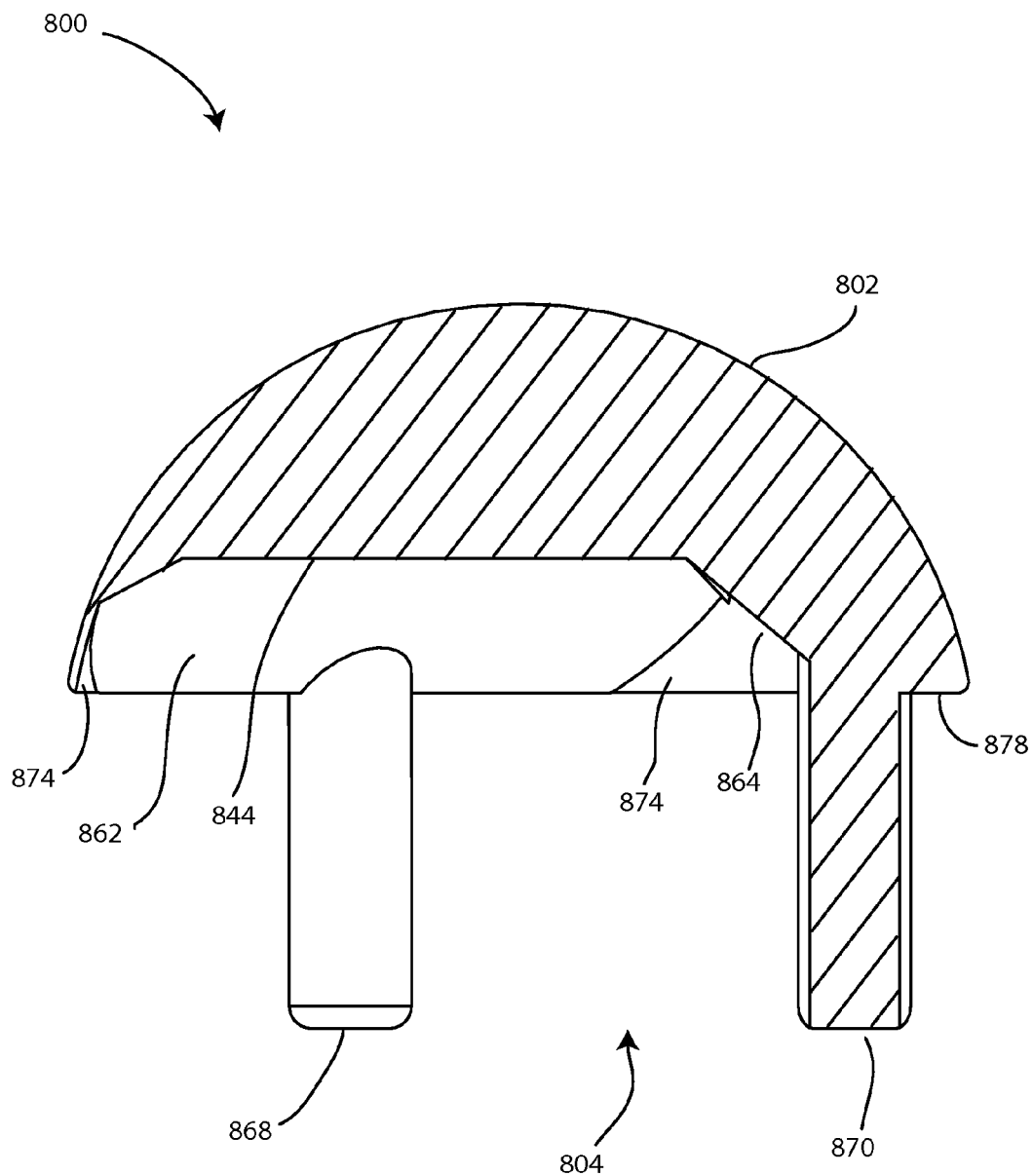


Fig. 8C

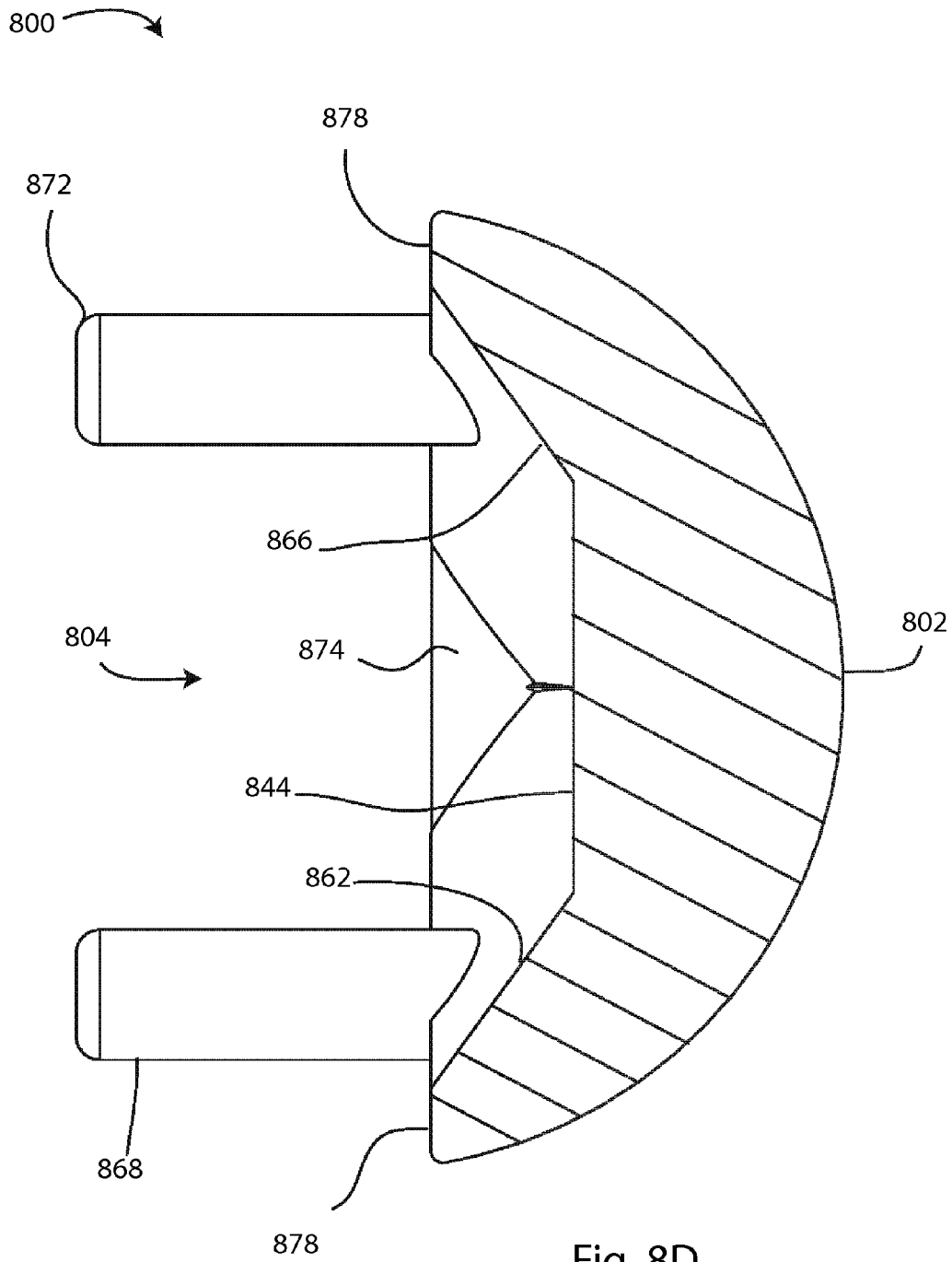


Fig. 8D

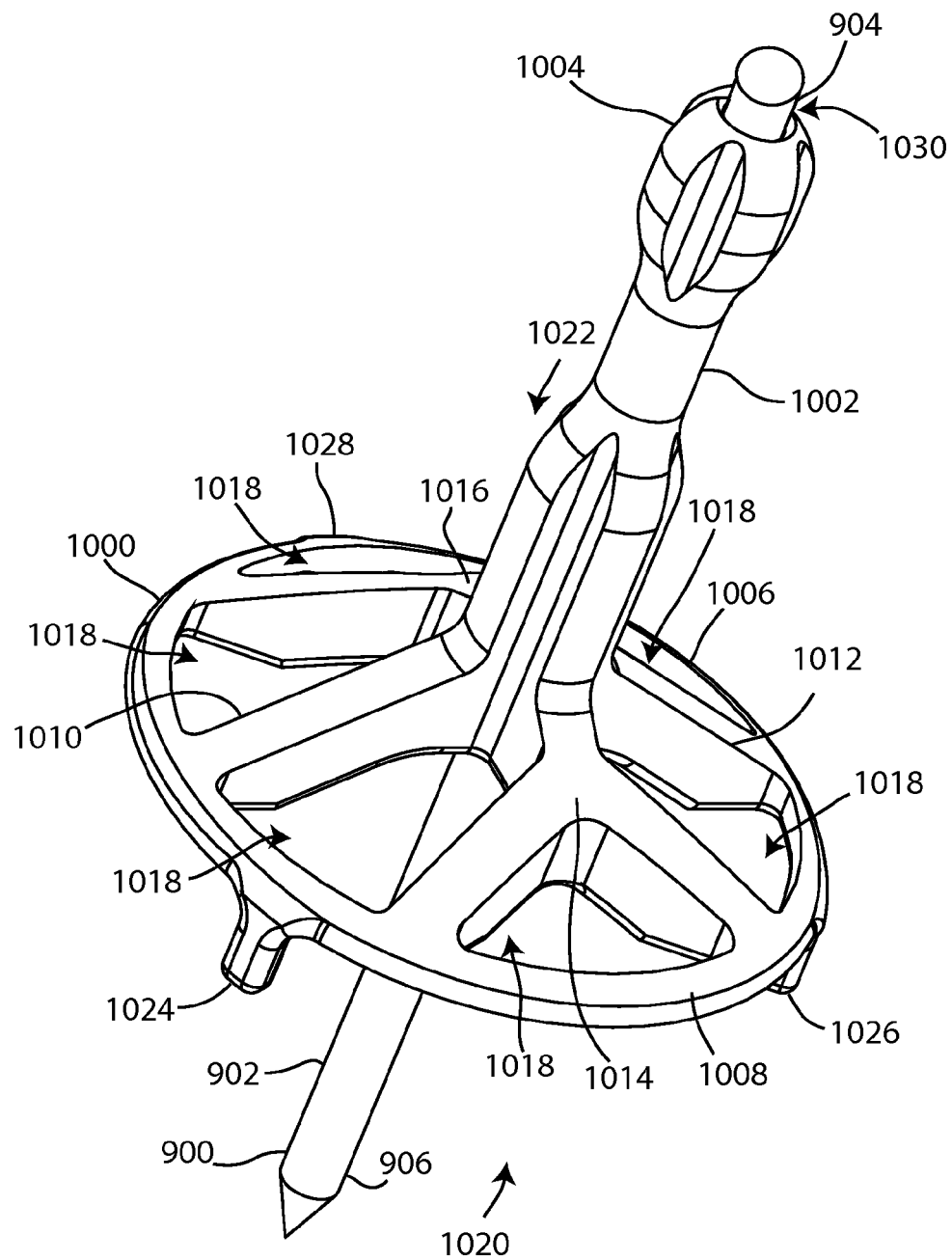


Fig. 9A

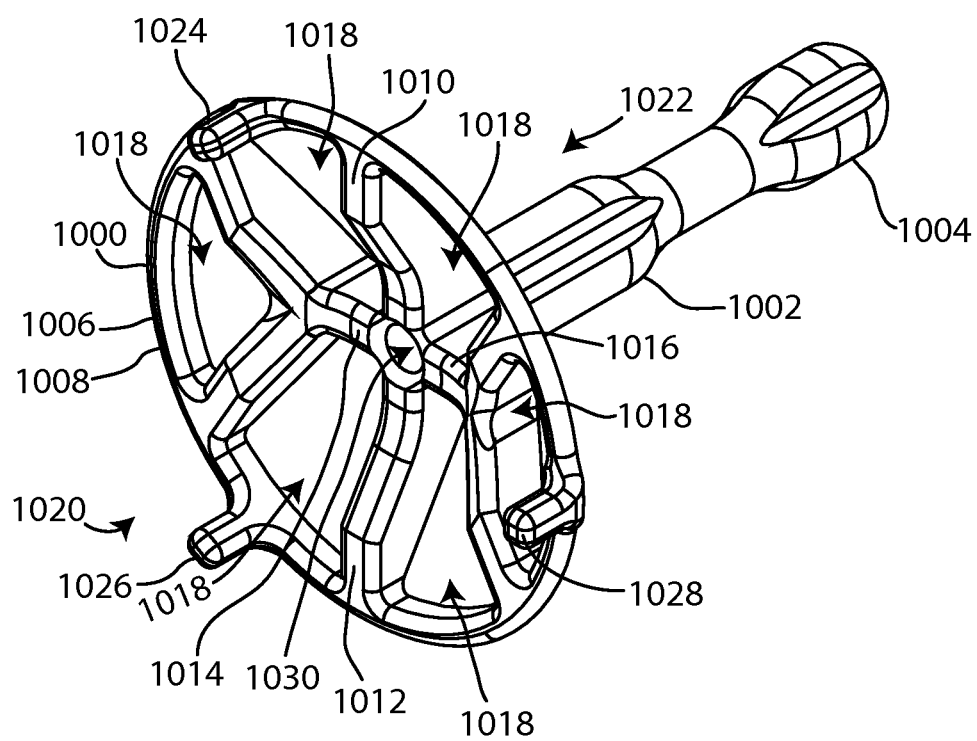


Fig. 9B

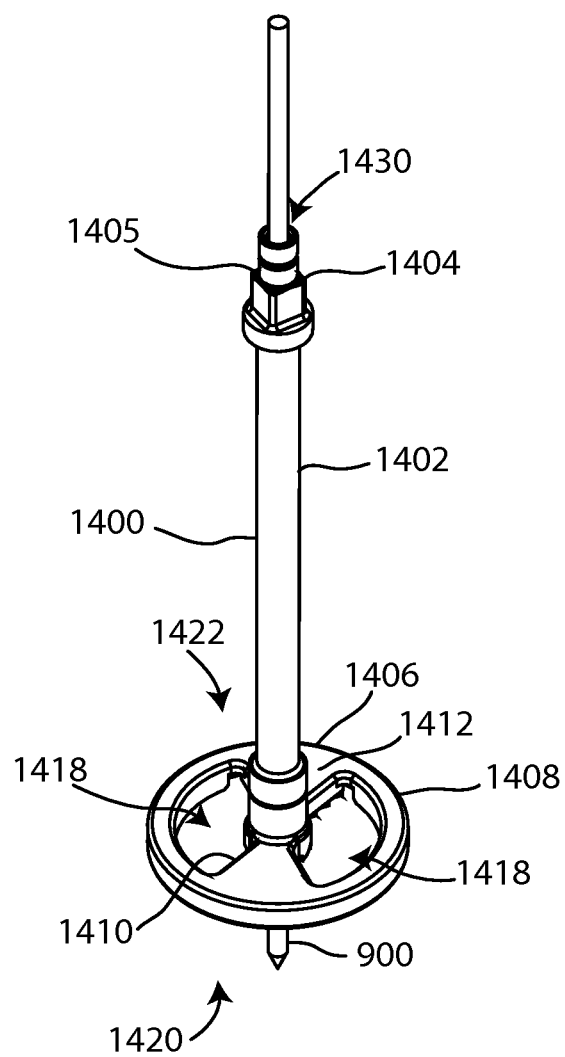
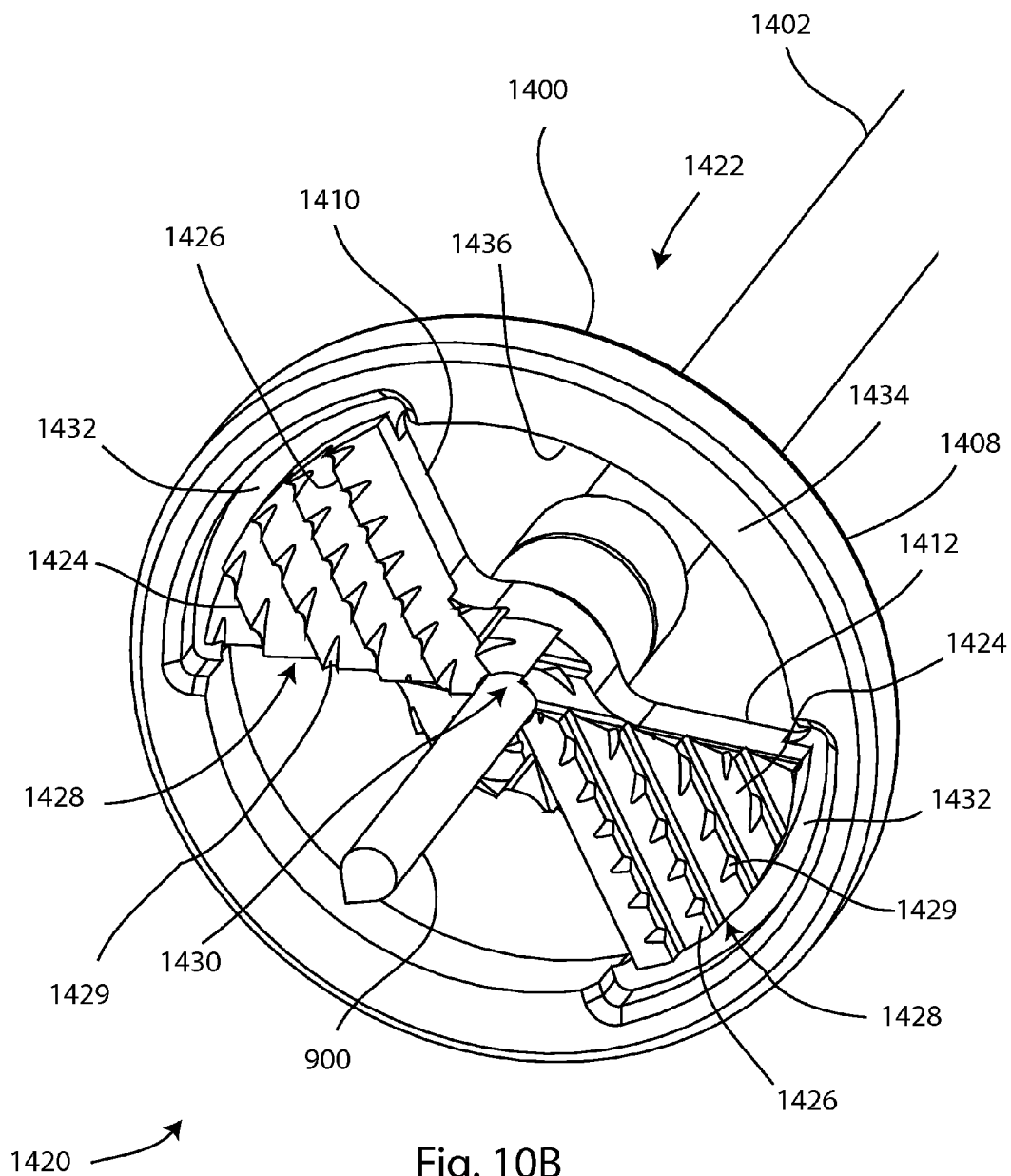


Fig. 10A



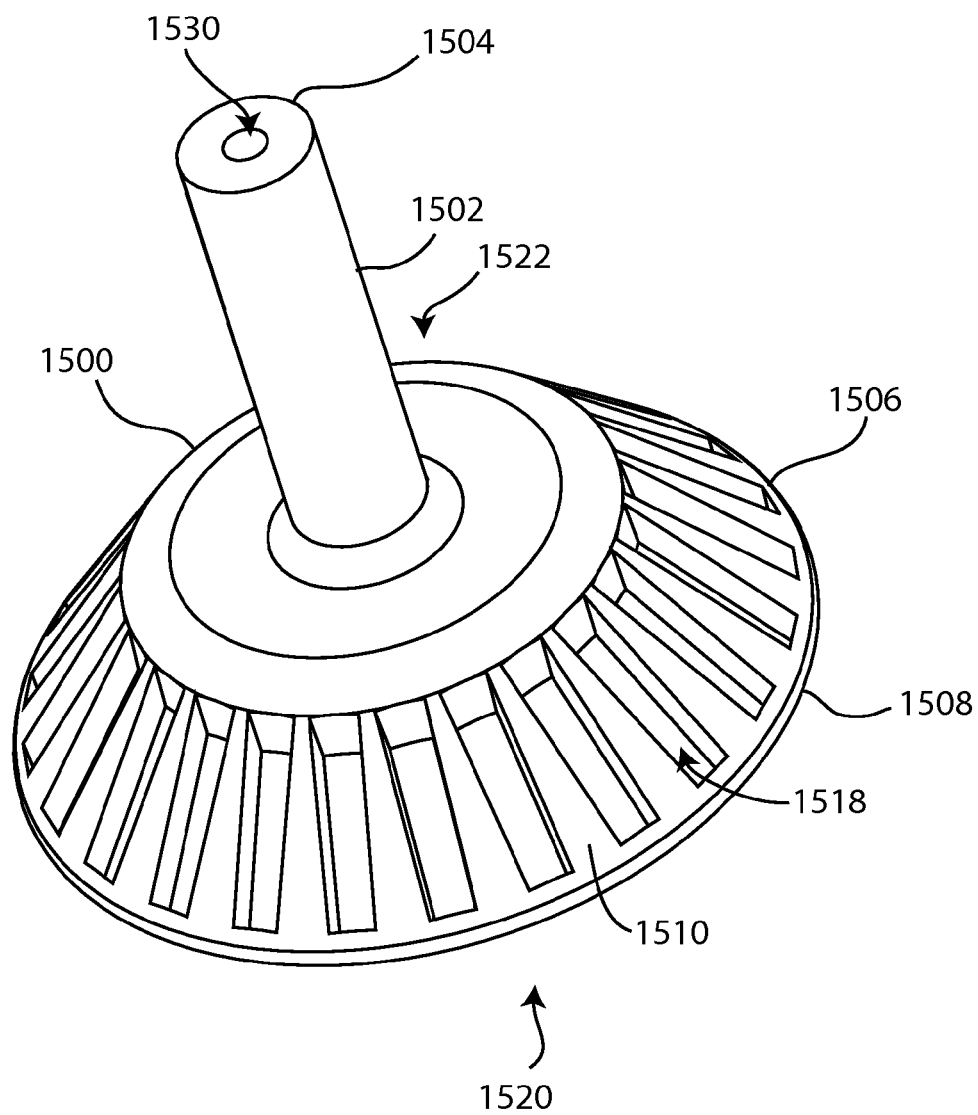


Fig. 11A

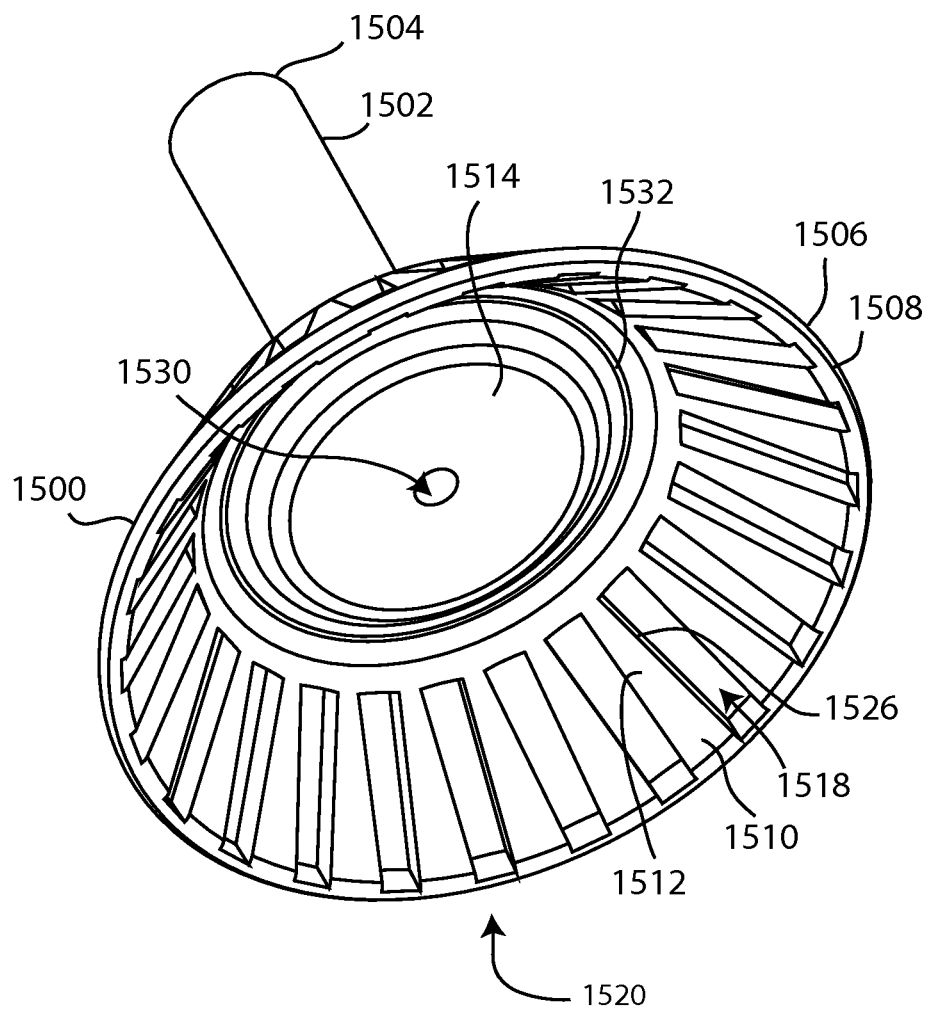
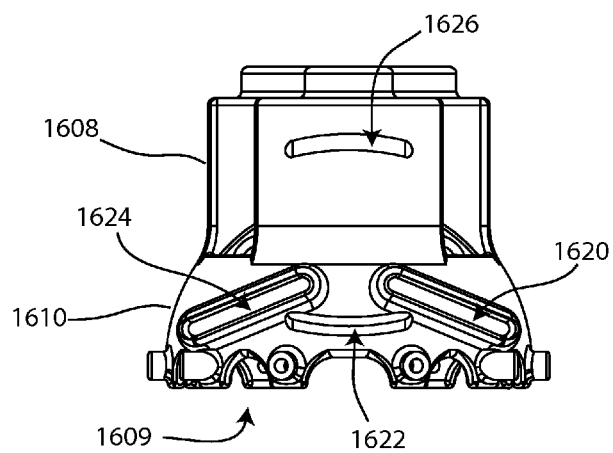
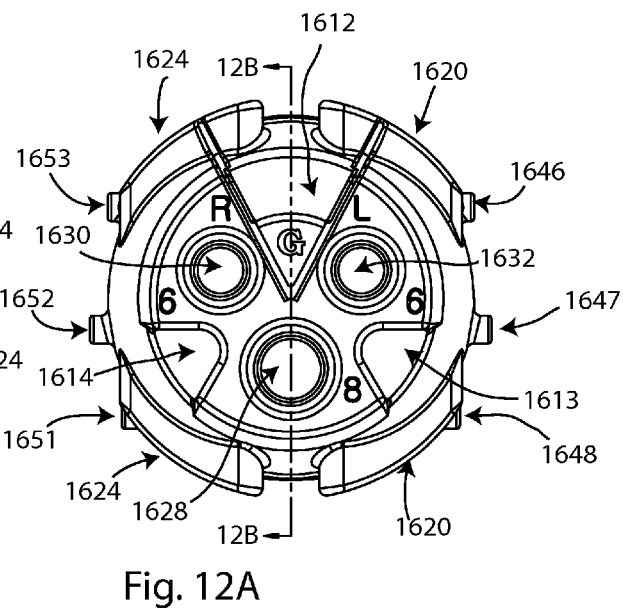
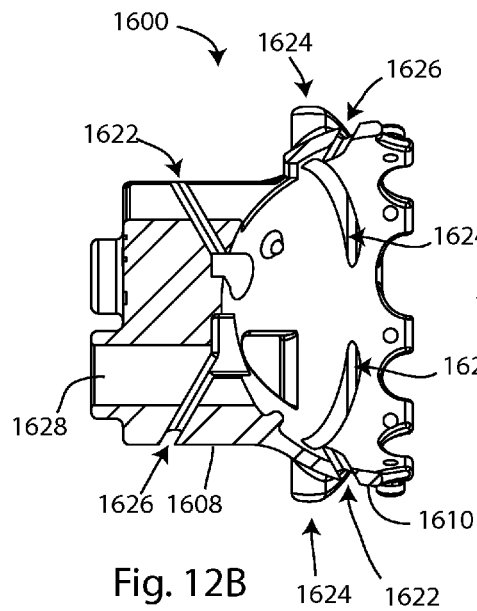
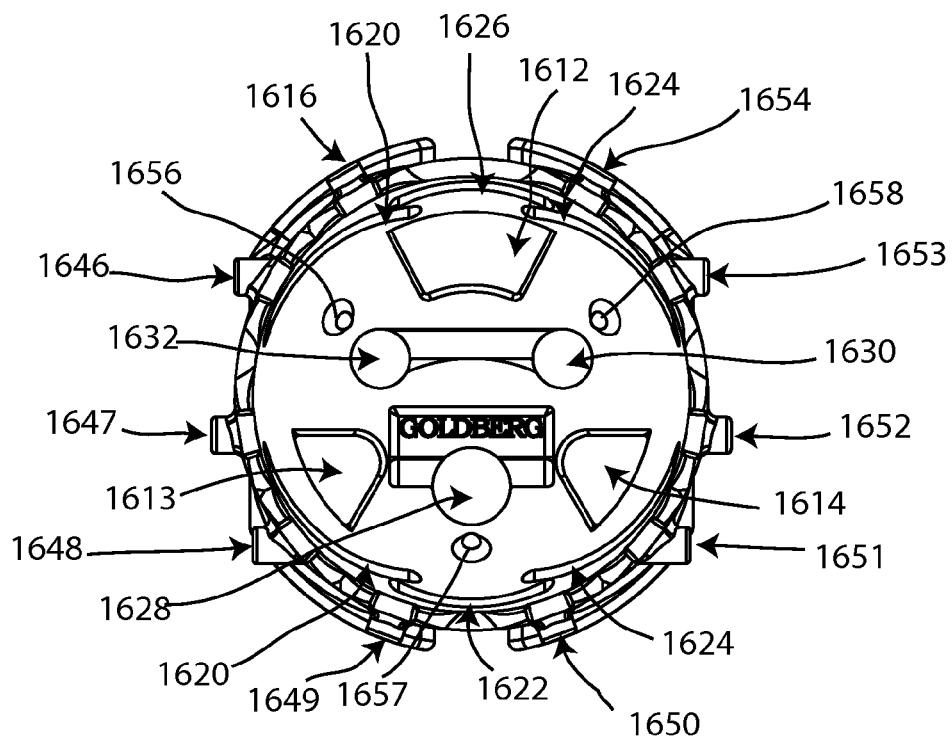
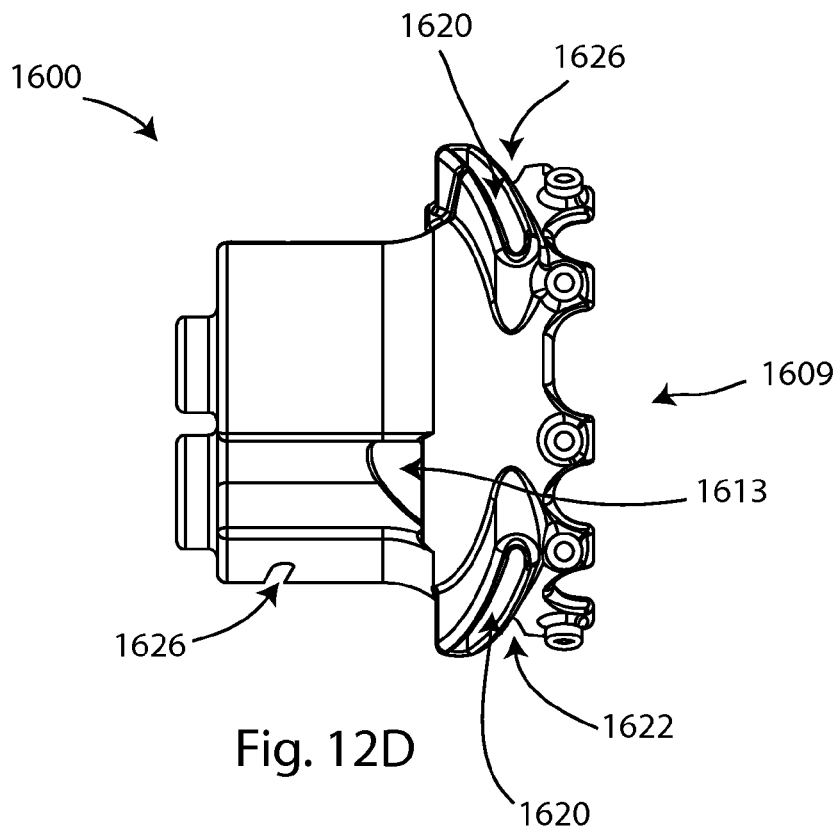


Fig. 11B





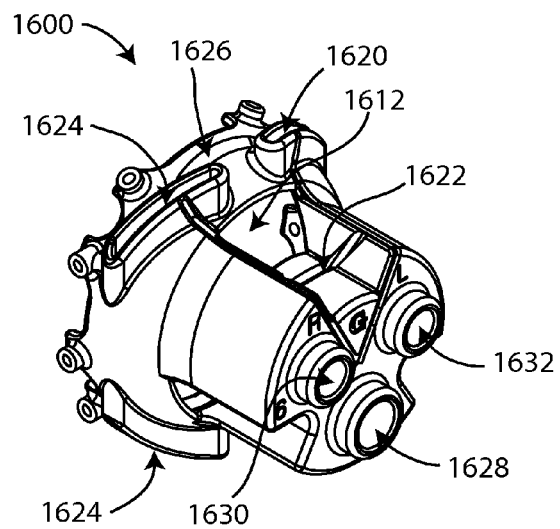


Fig. 12F

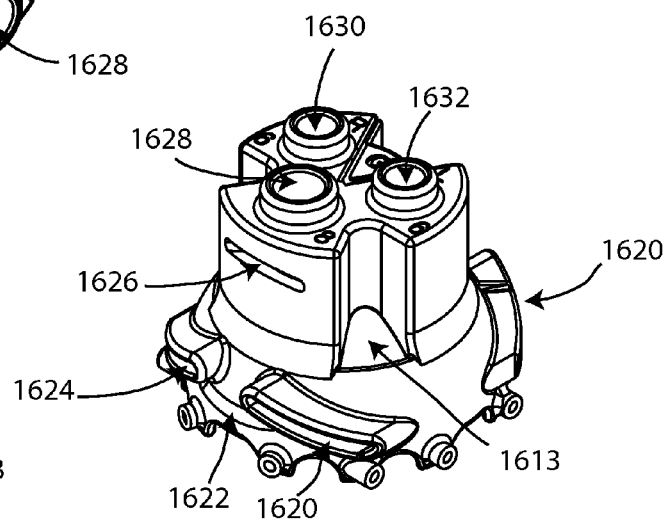


Fig. 12G

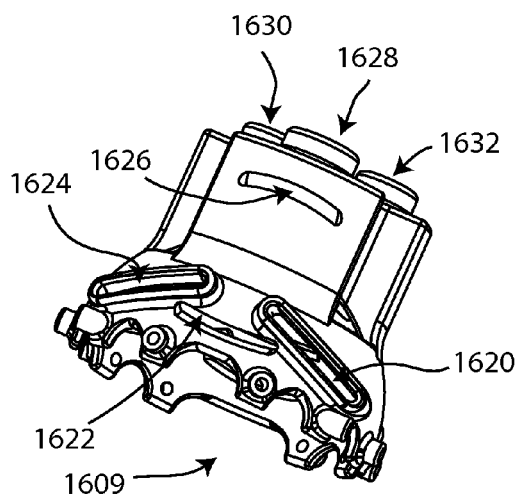


Fig. 12H

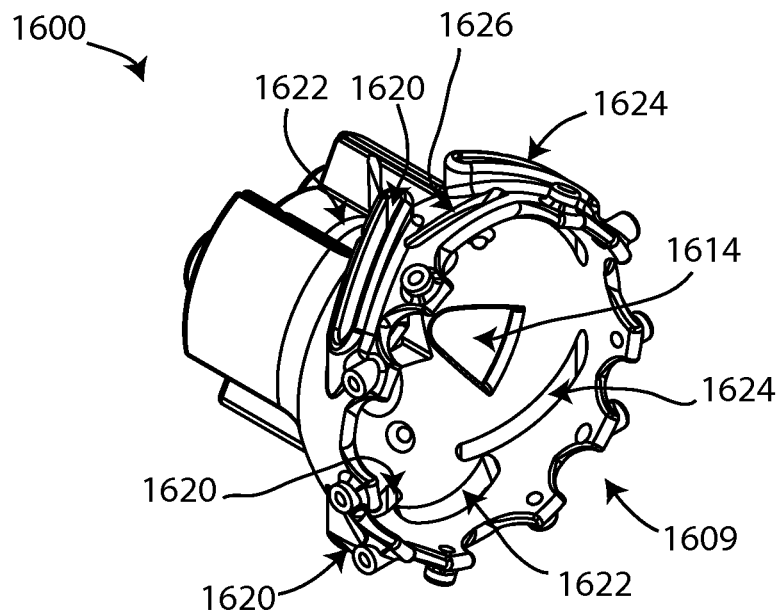


Fig. 12I

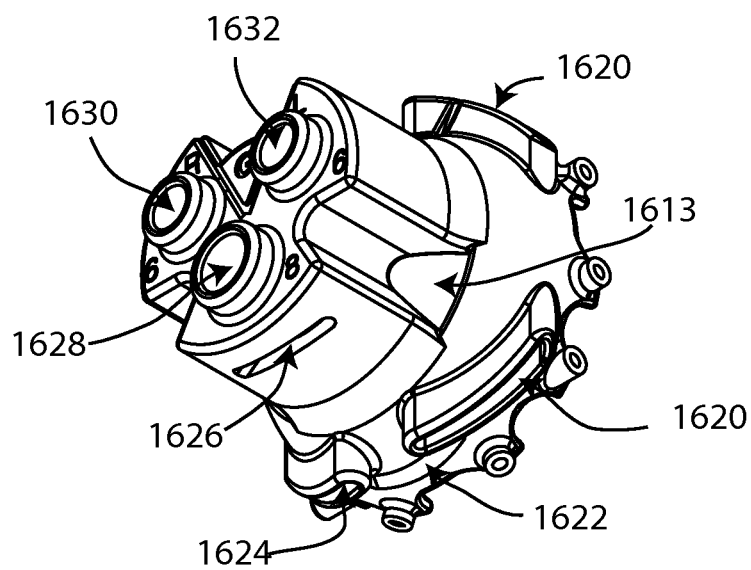


Fig. 12J

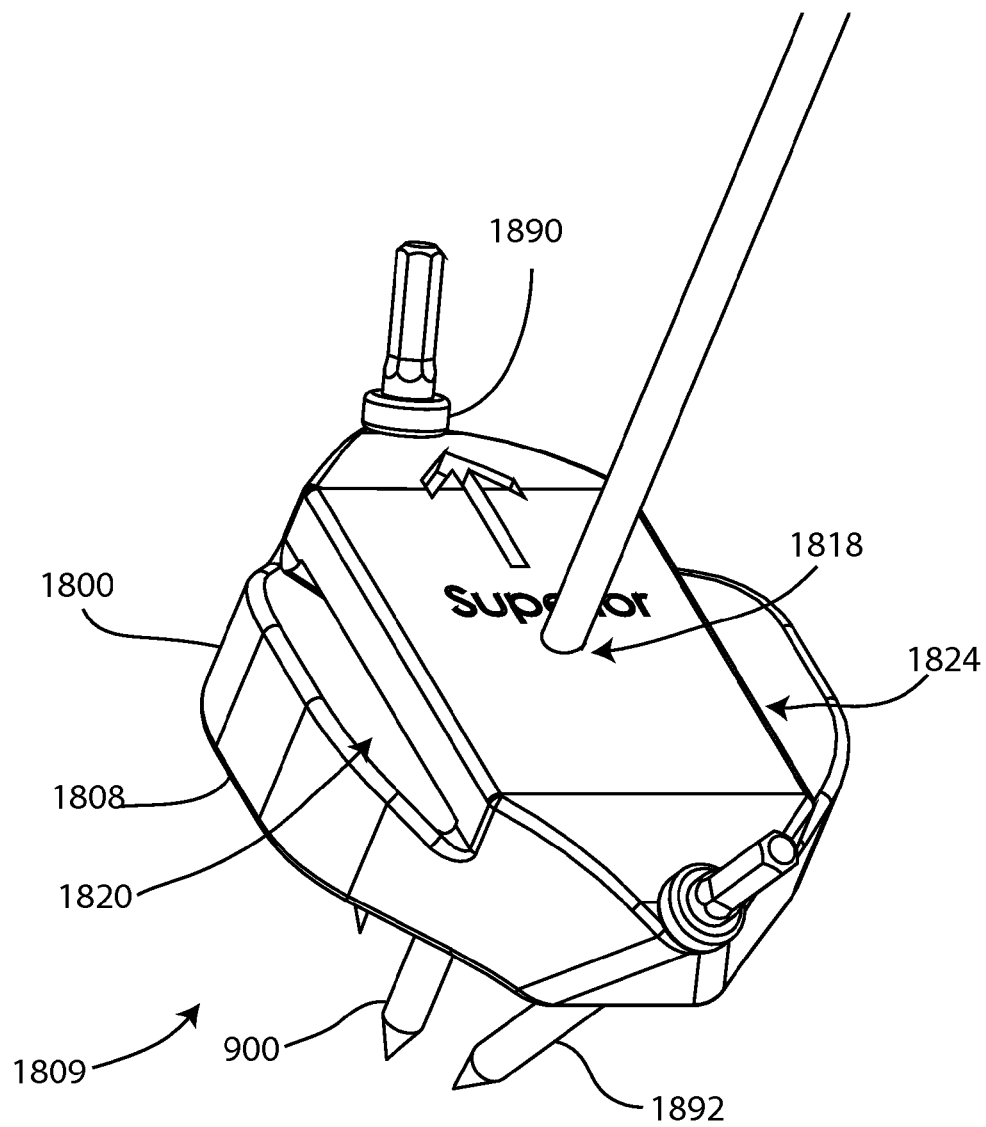


Fig. 13A

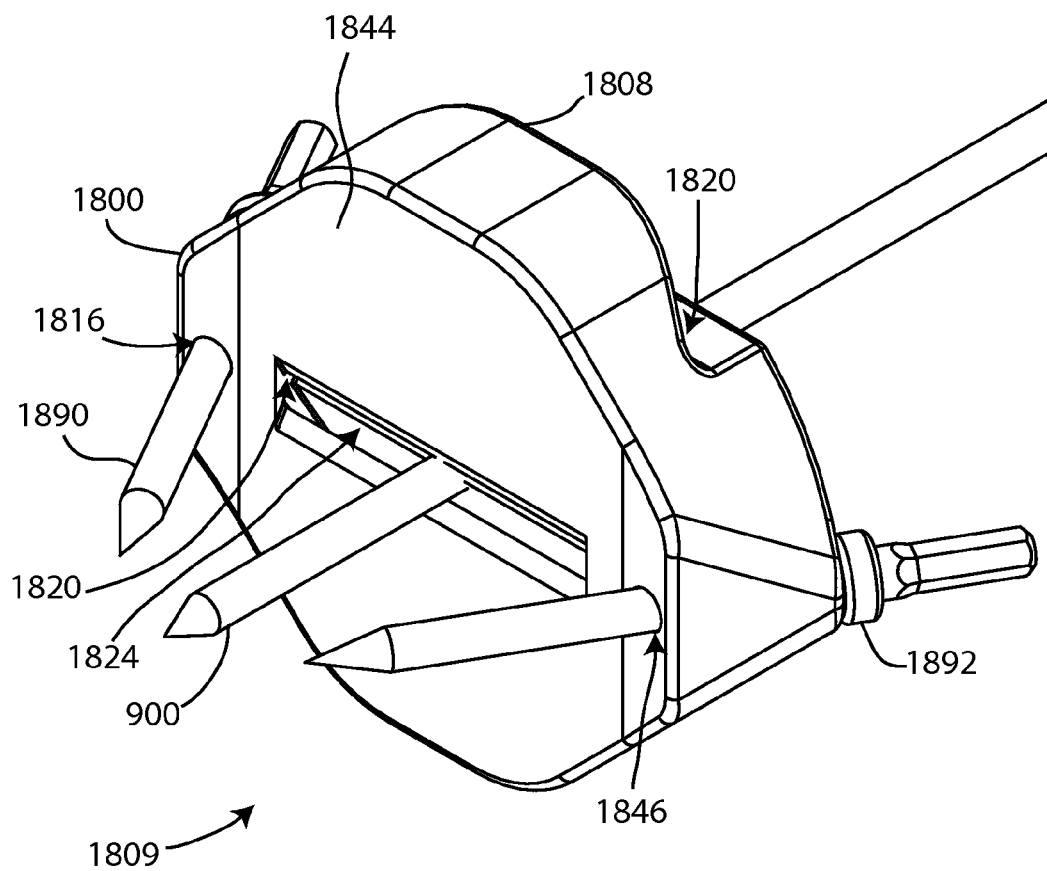


Fig. 13B

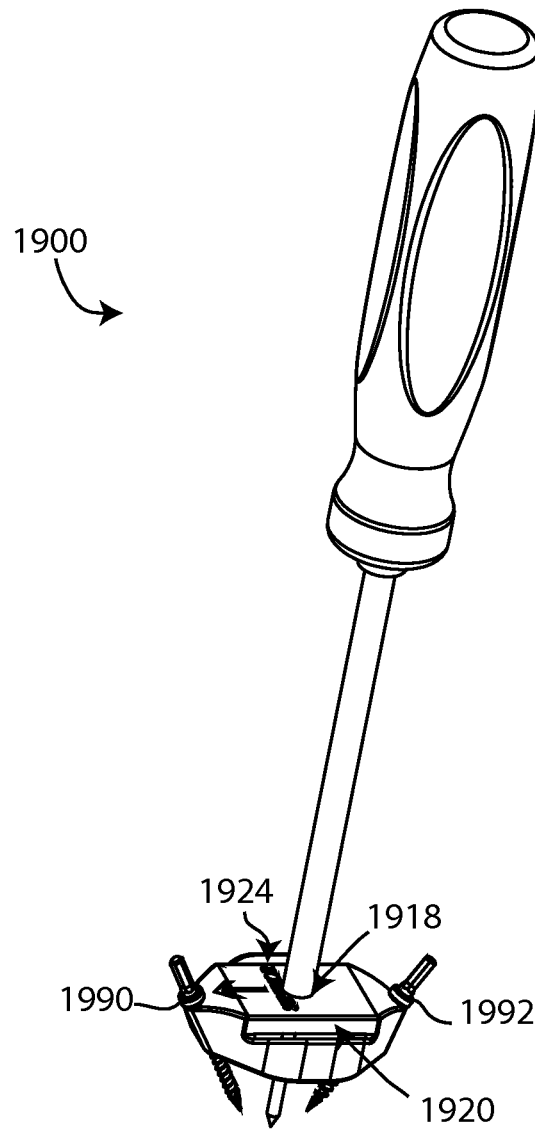


Fig. 14

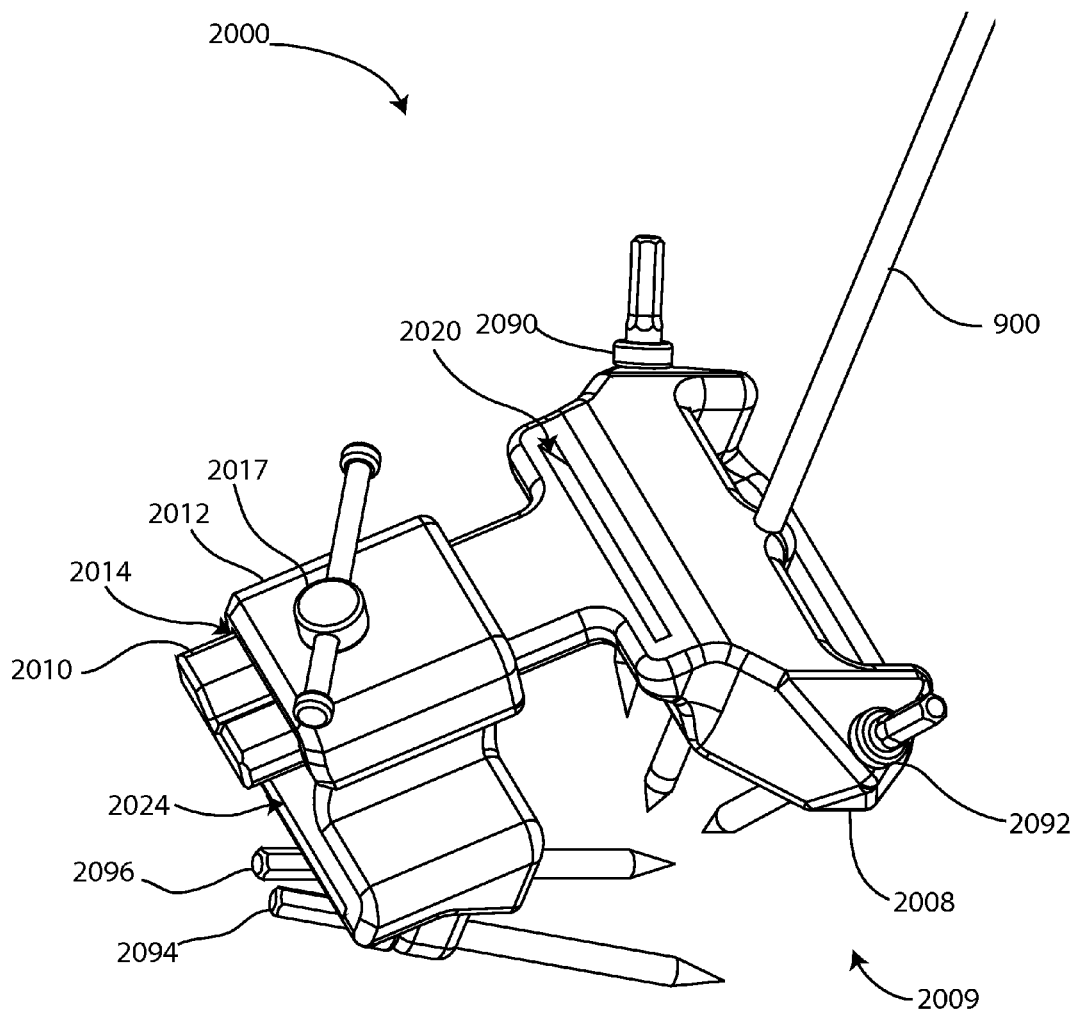


Fig. 15A

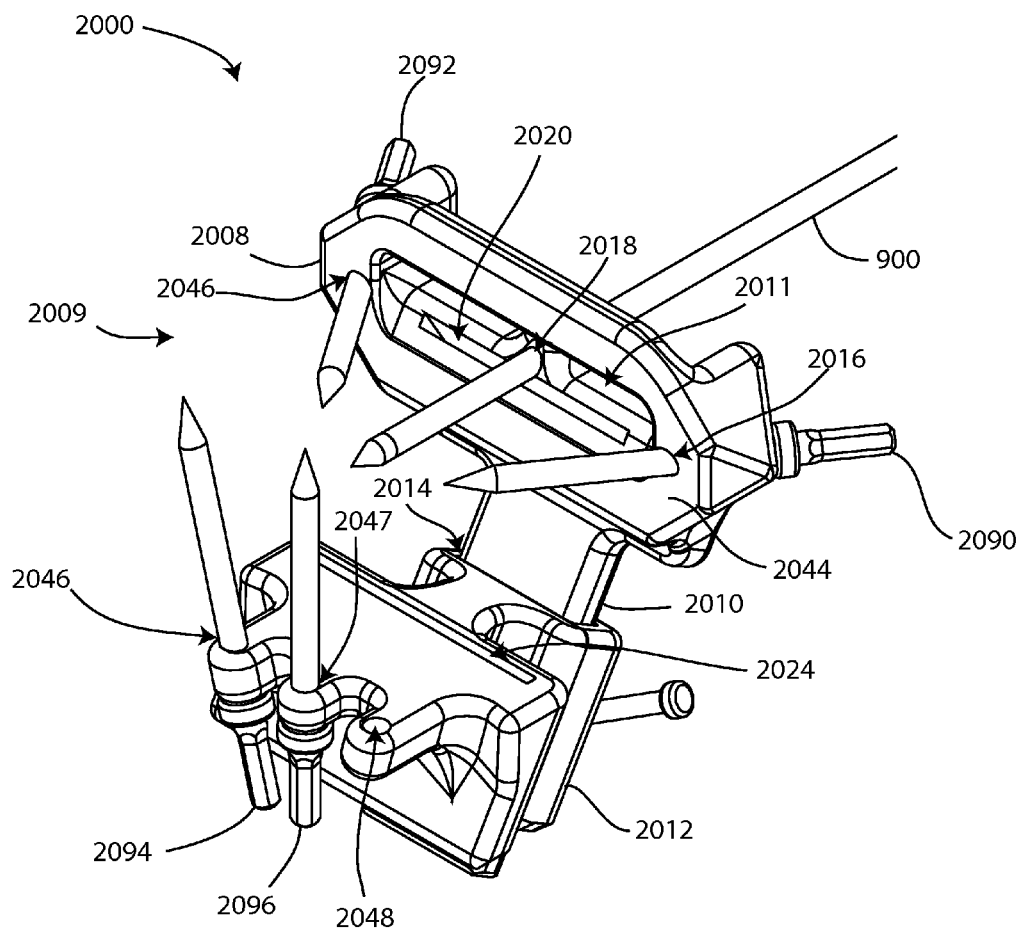


Fig. 15B

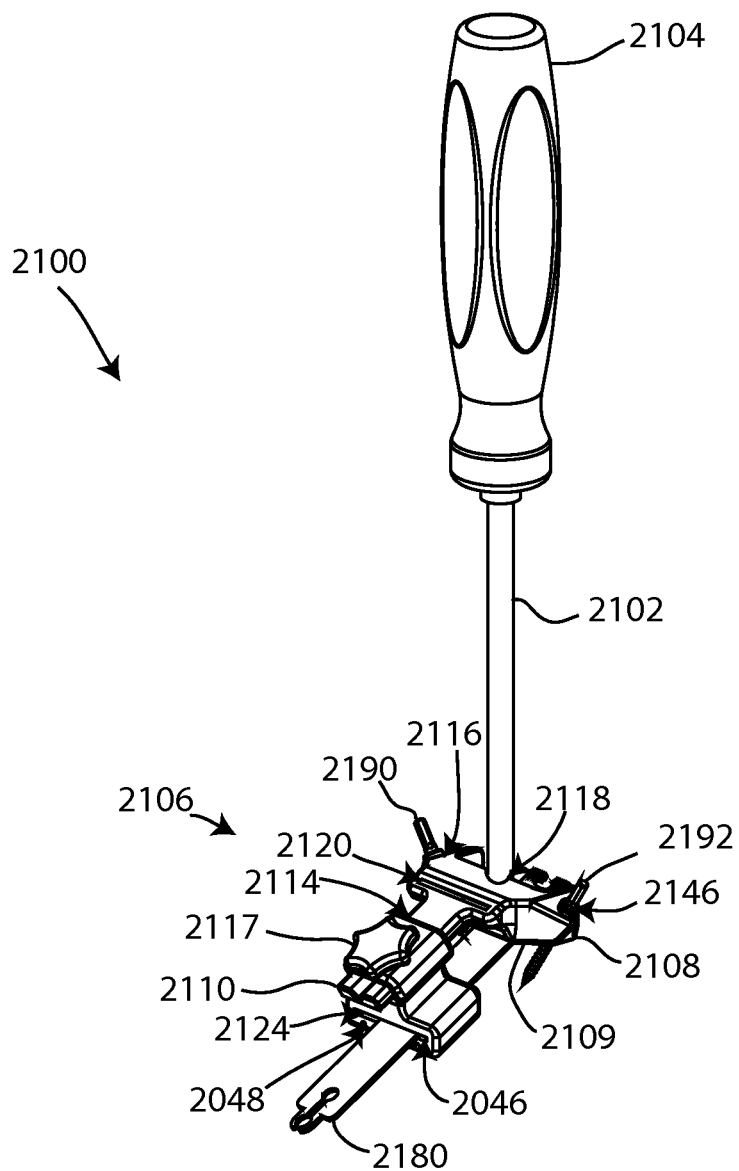


Fig. 16

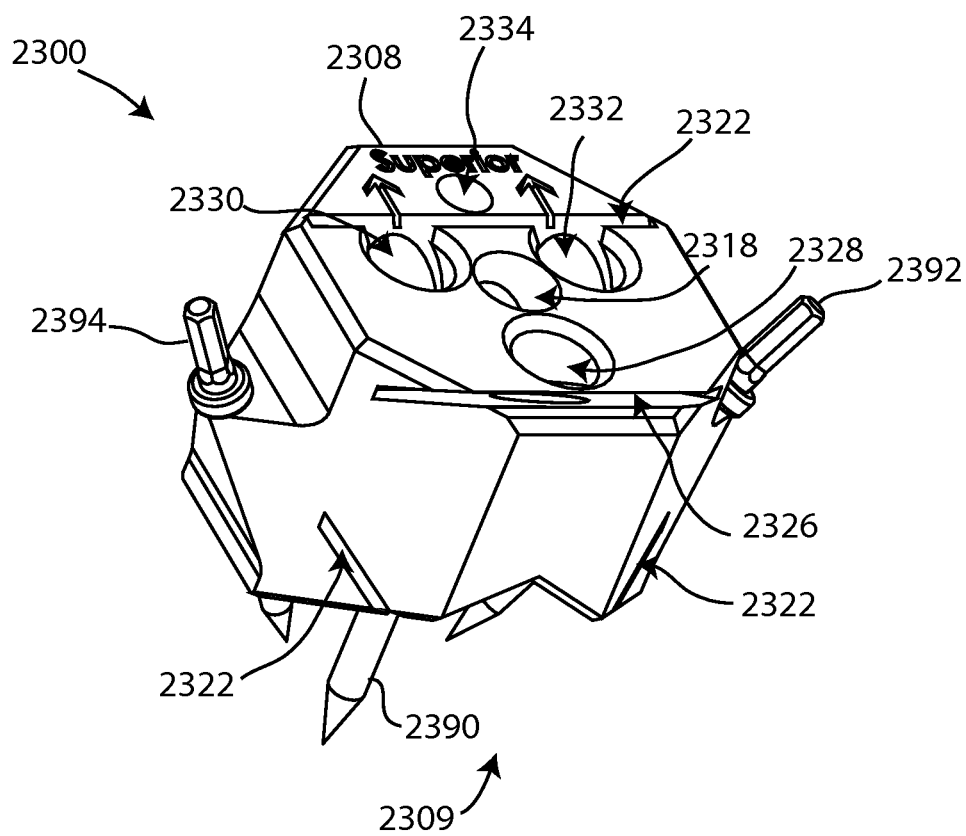


Fig. 17A

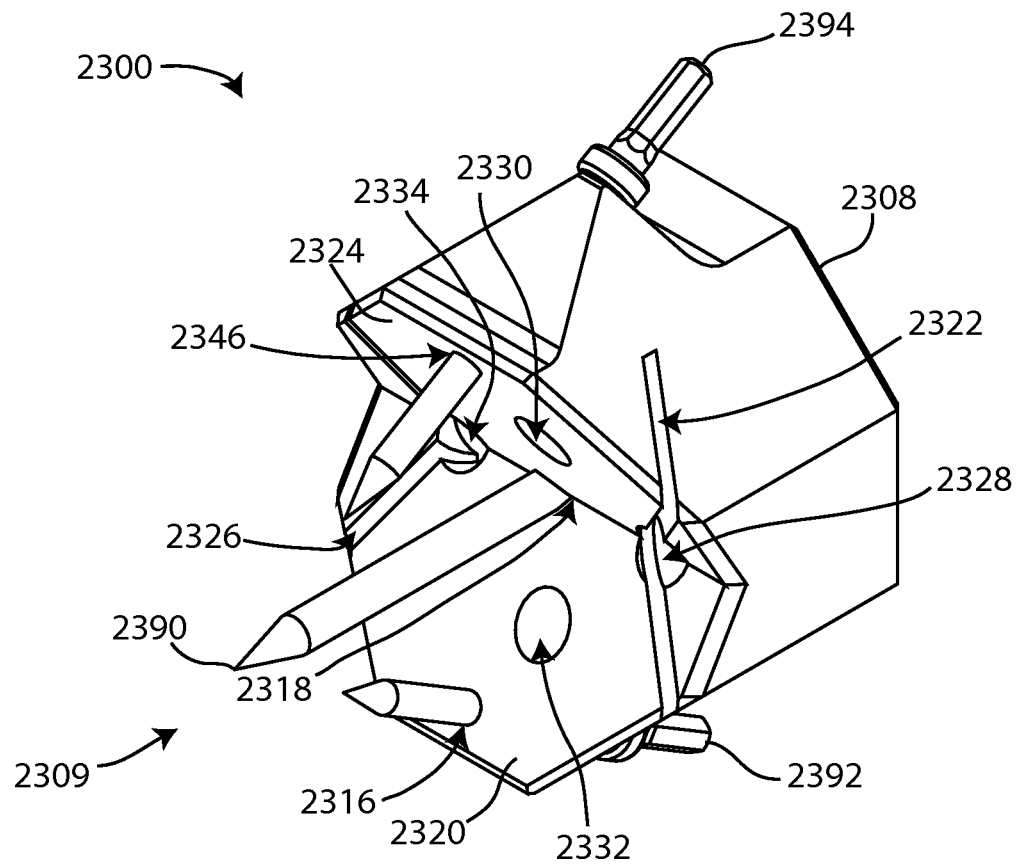


Fig. 17B

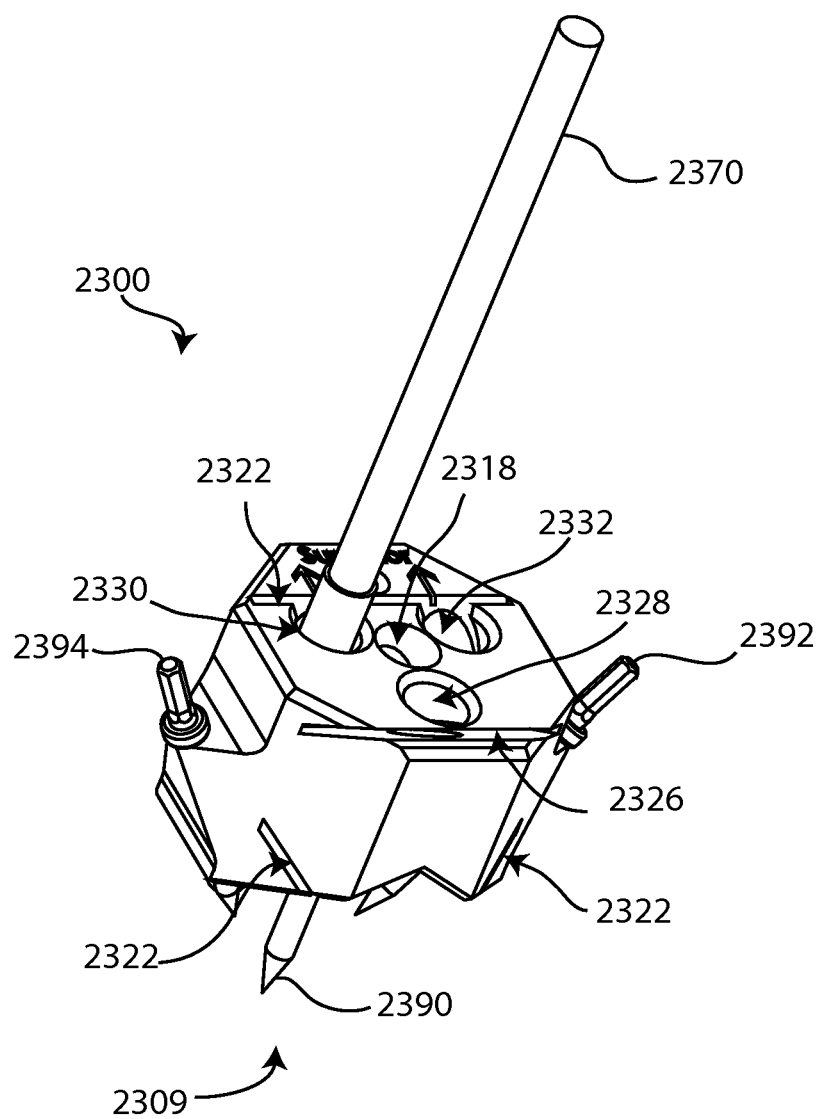


Fig. 17C

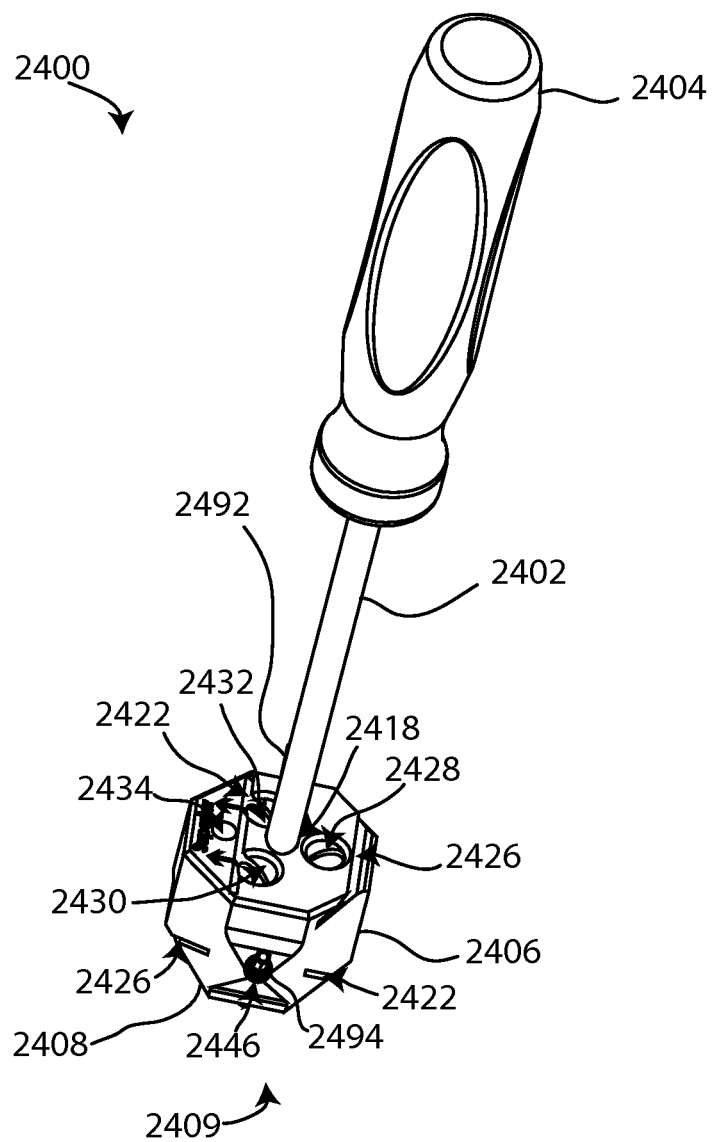
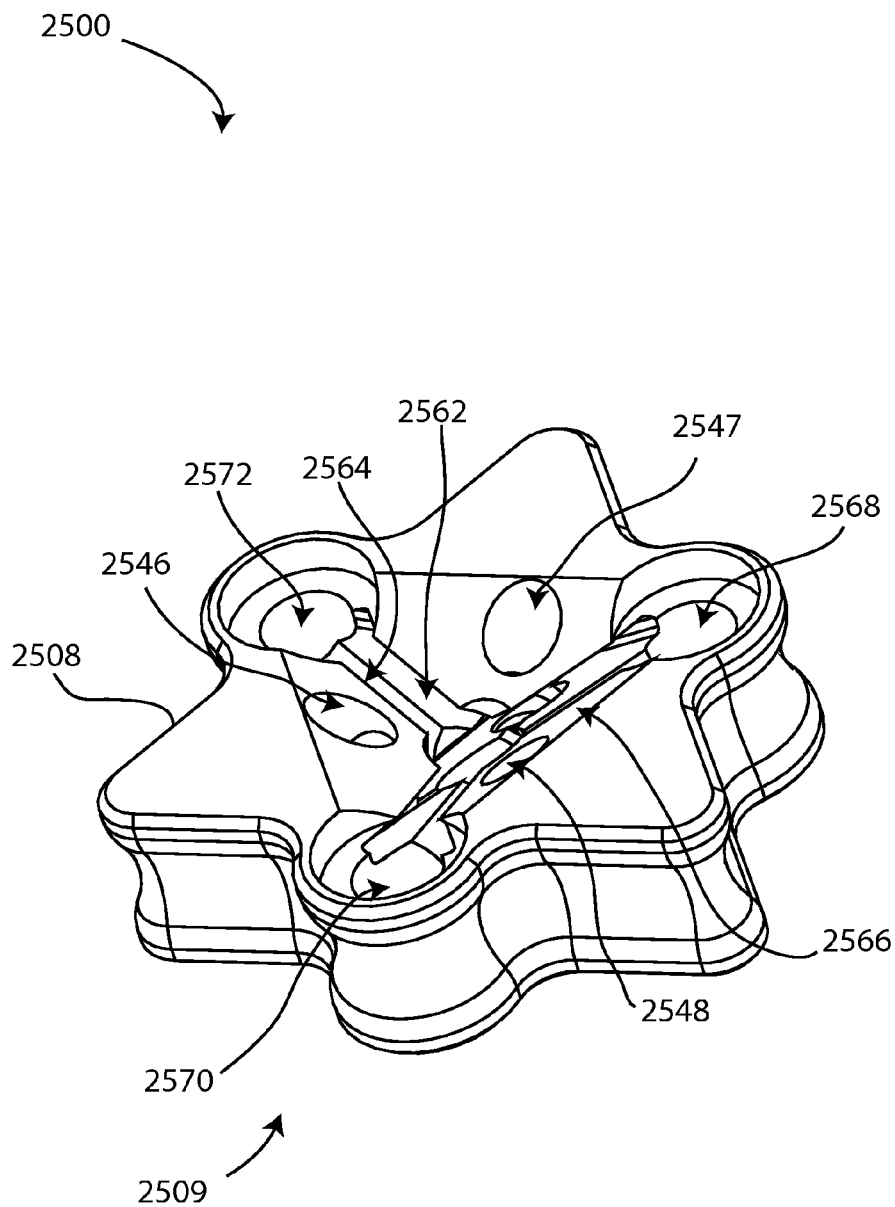


Fig. 18



Fig, 19A

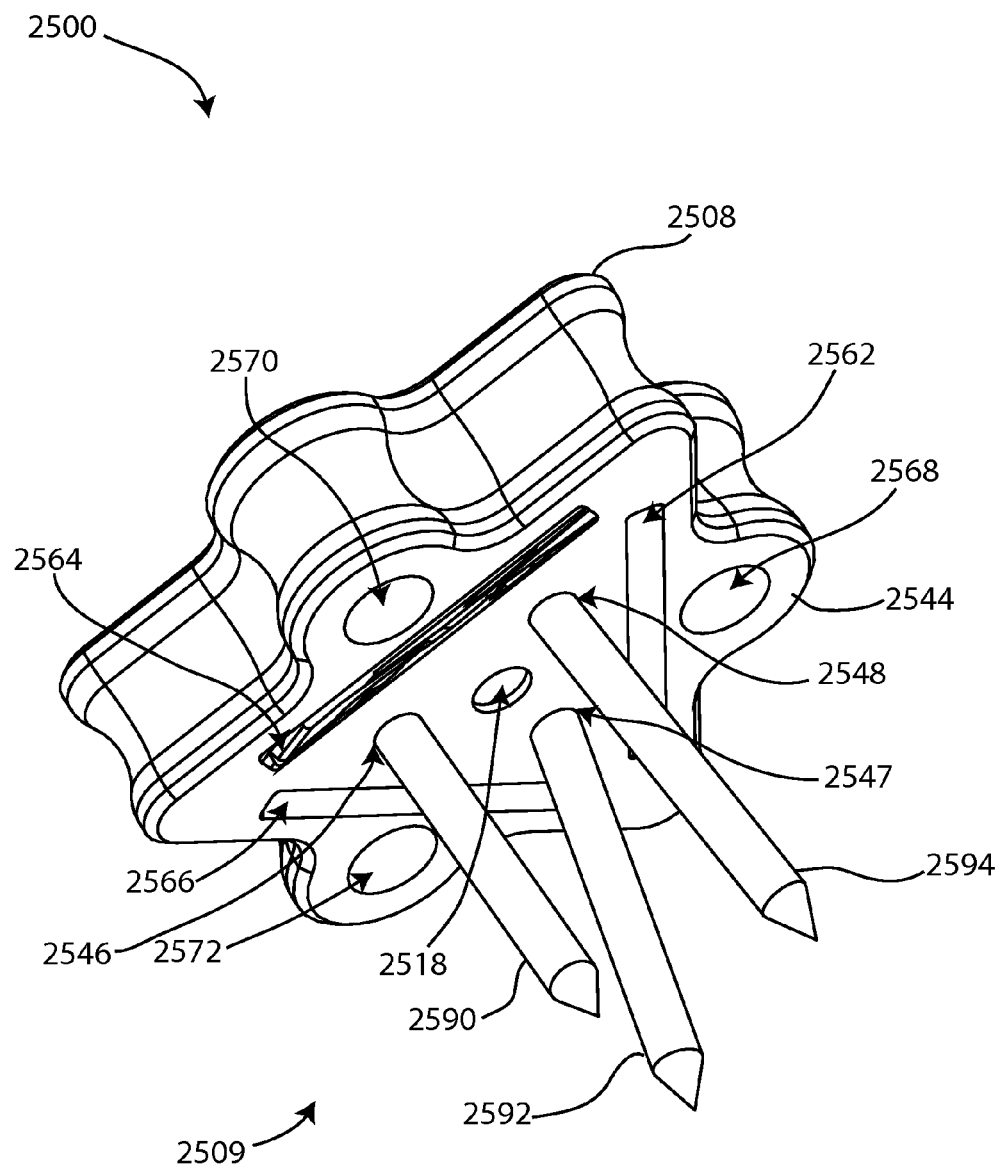


Fig. 19B

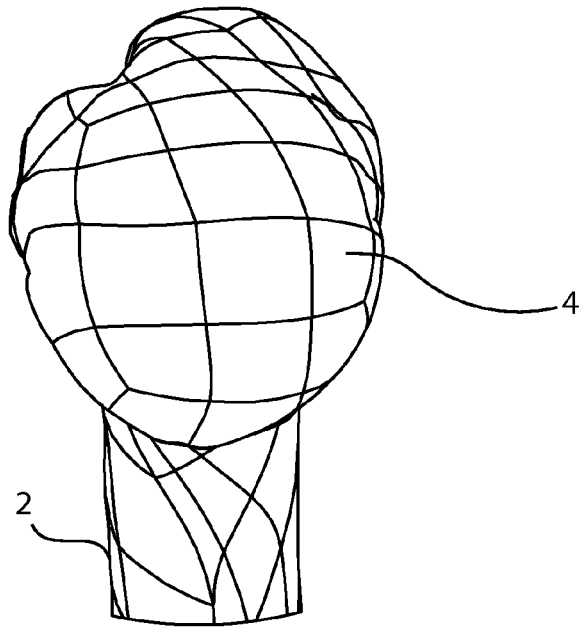


Fig. 20A

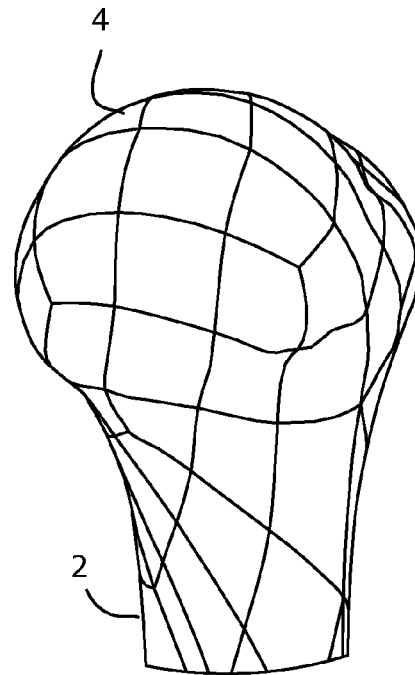


Fig. 20B

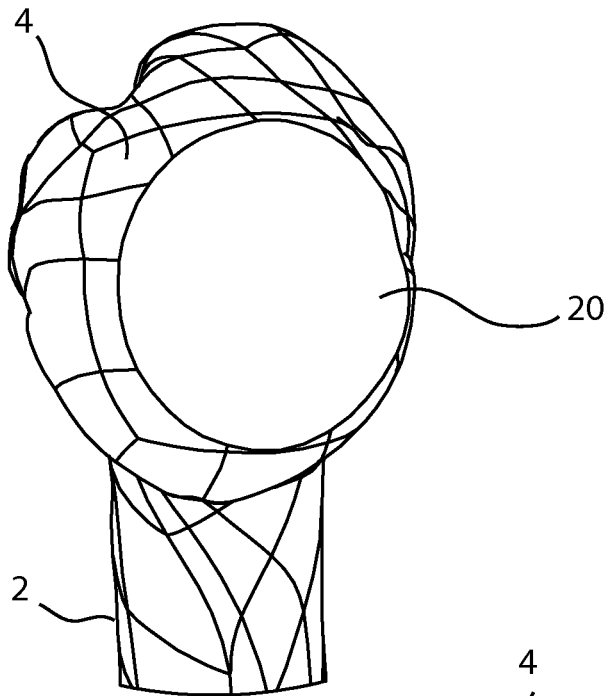


Fig. 21A

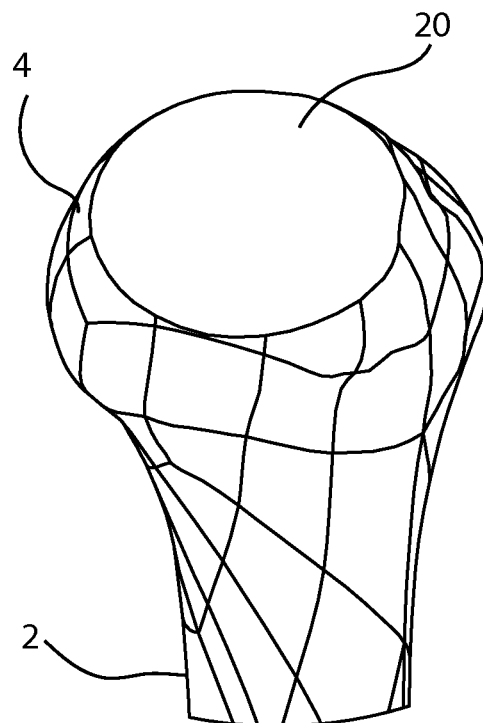


Fig. 21B

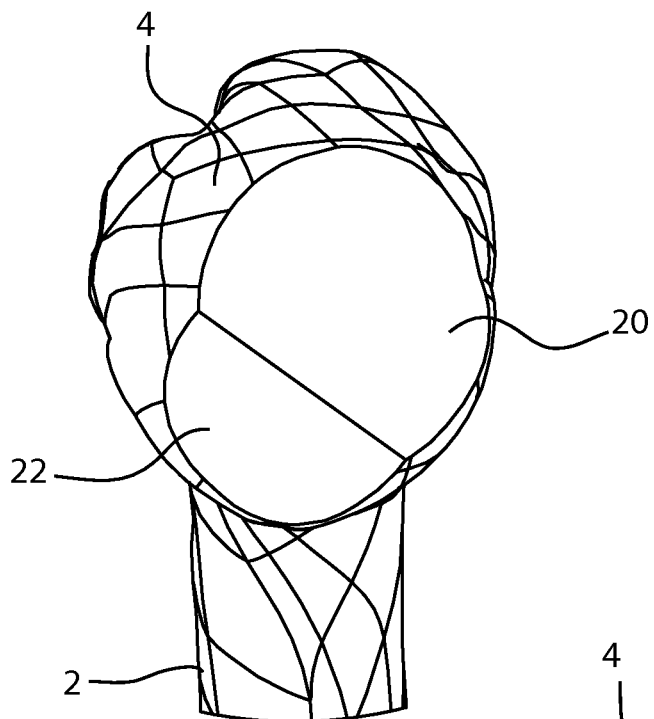


Fig. 22A

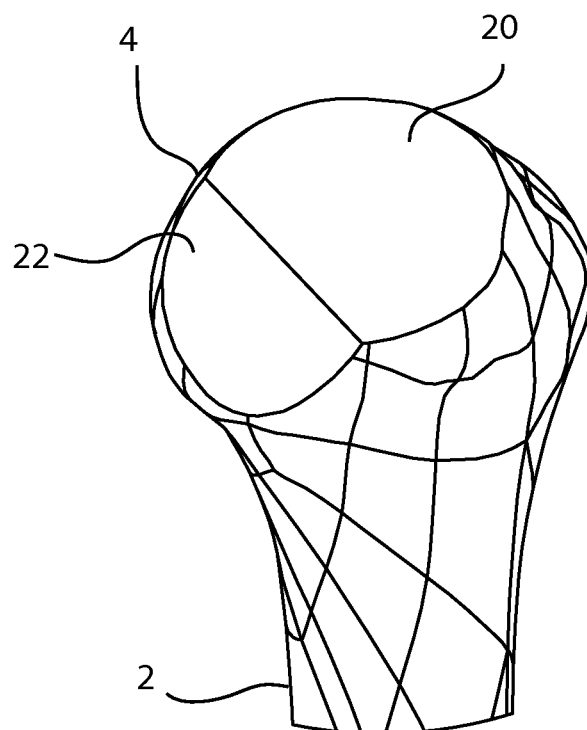


Fig. 22B

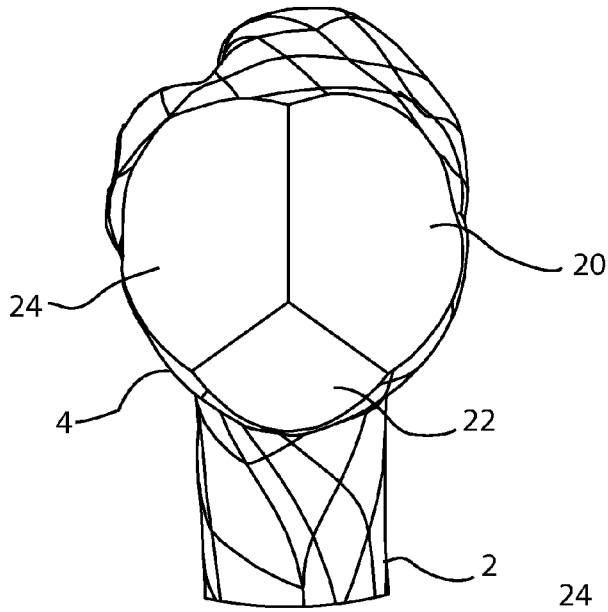


Fig. 23A

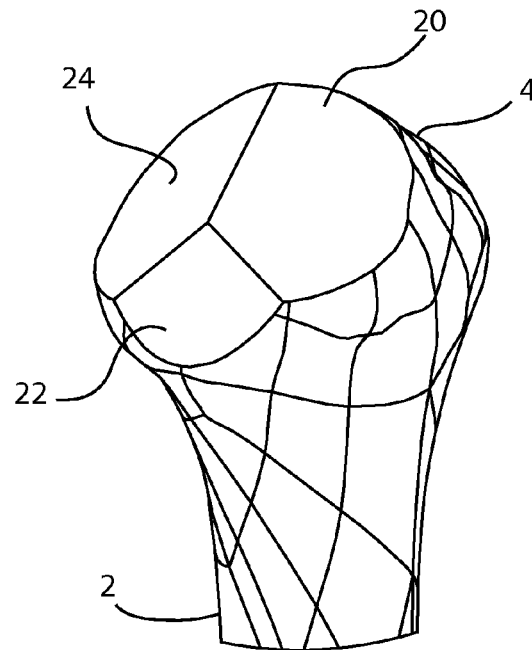


Fig. 23B

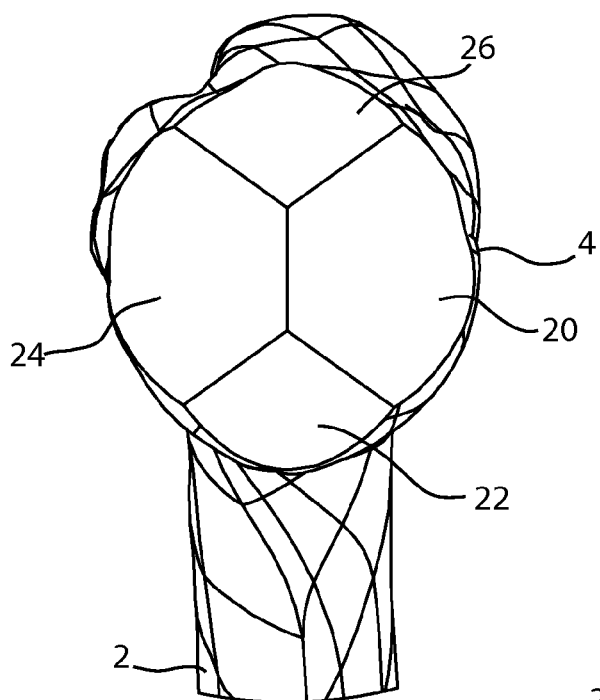


Fig. 24A

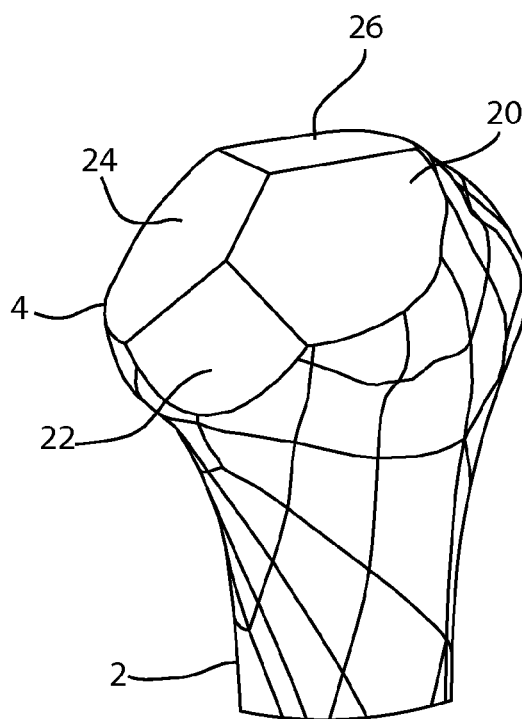


Fig. 24B

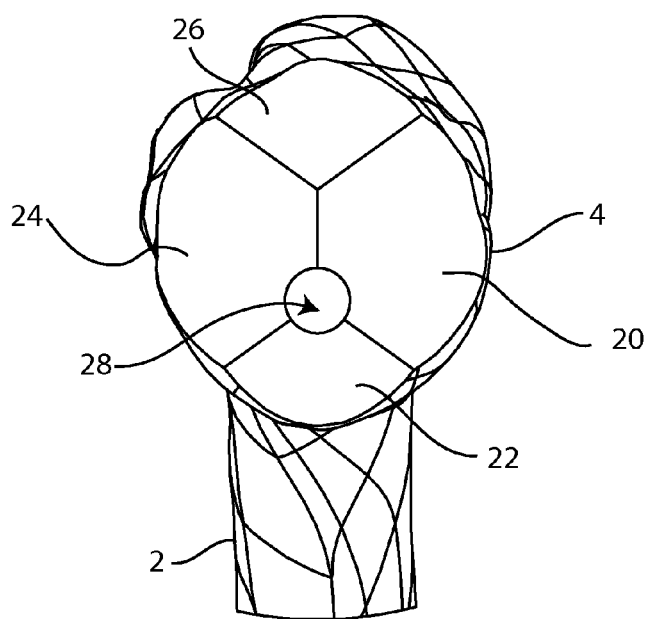


Fig. 25A

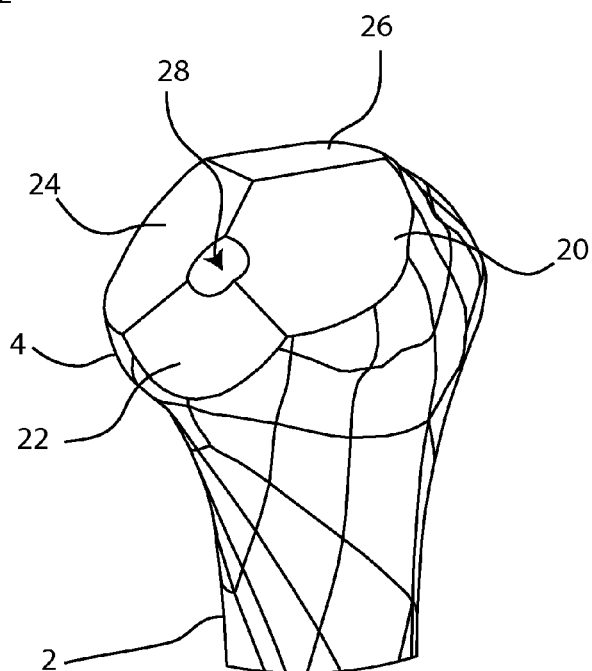


Fig. 25B

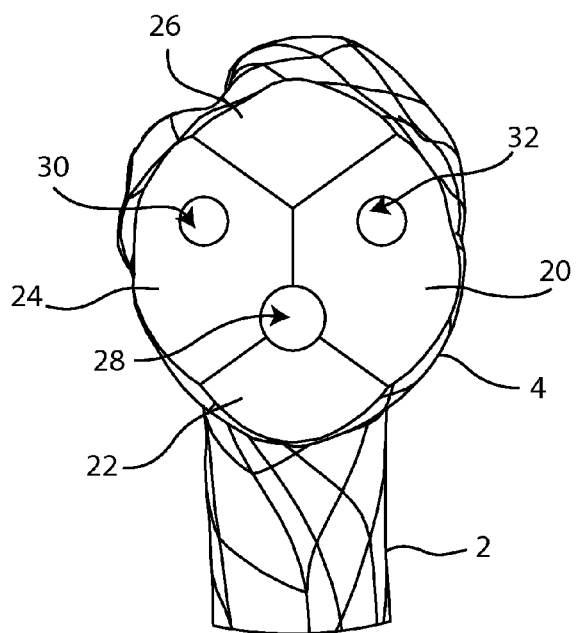


Fig. 26A

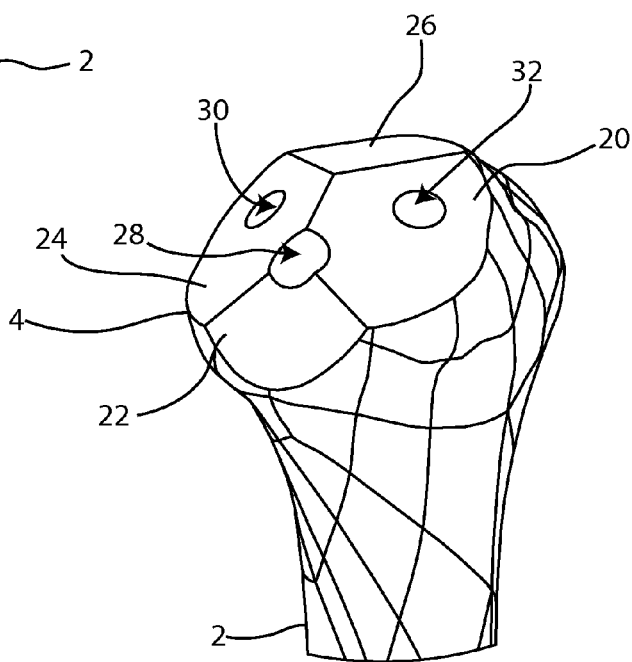


Fig. 26B

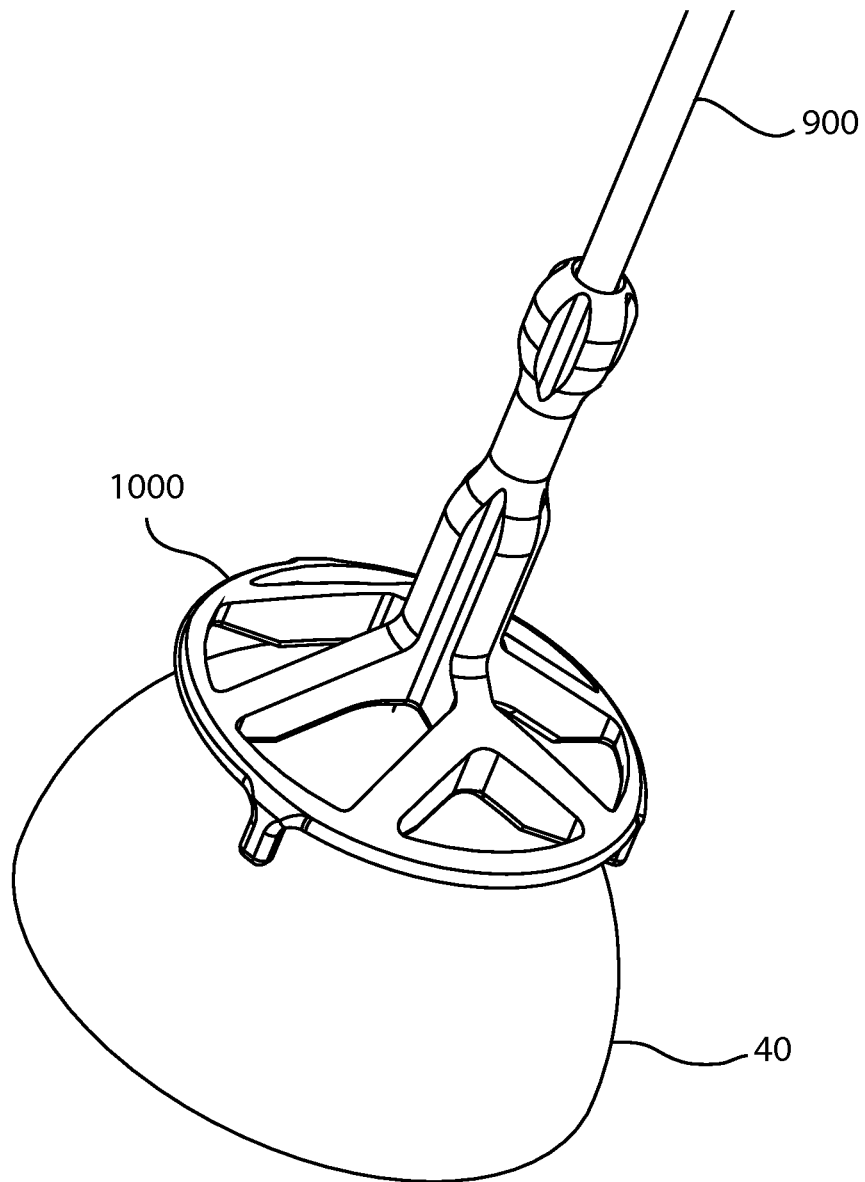


Fig. 27

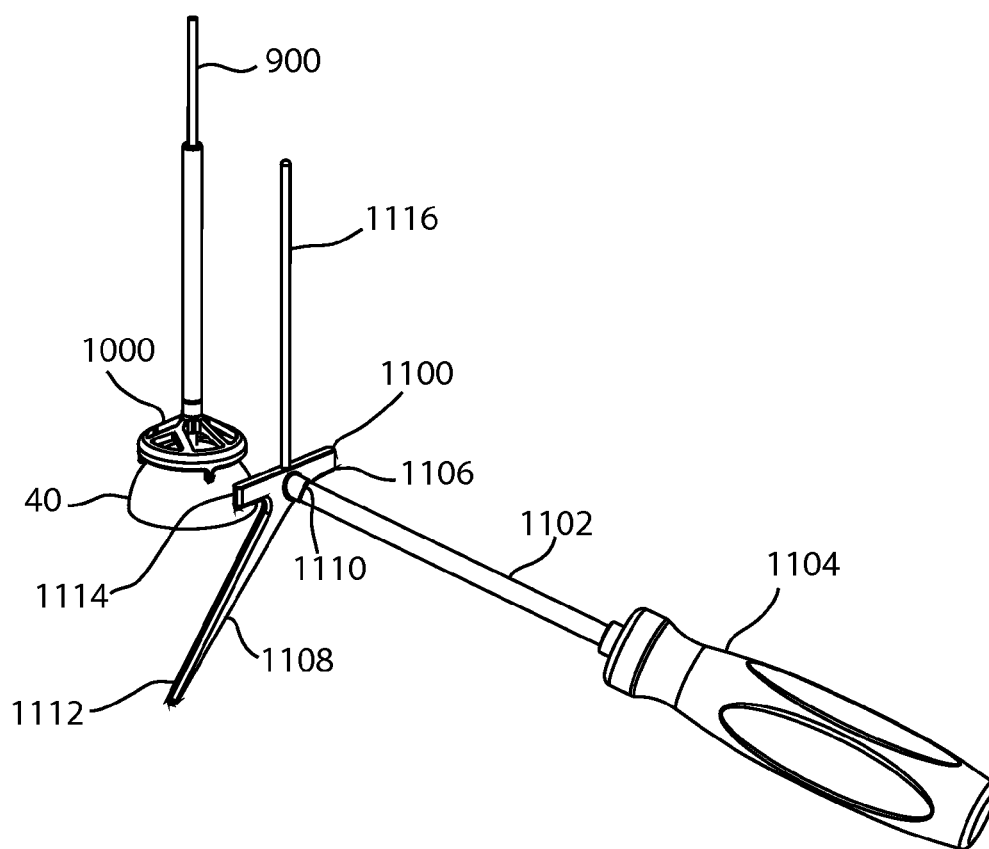


Fig. 28

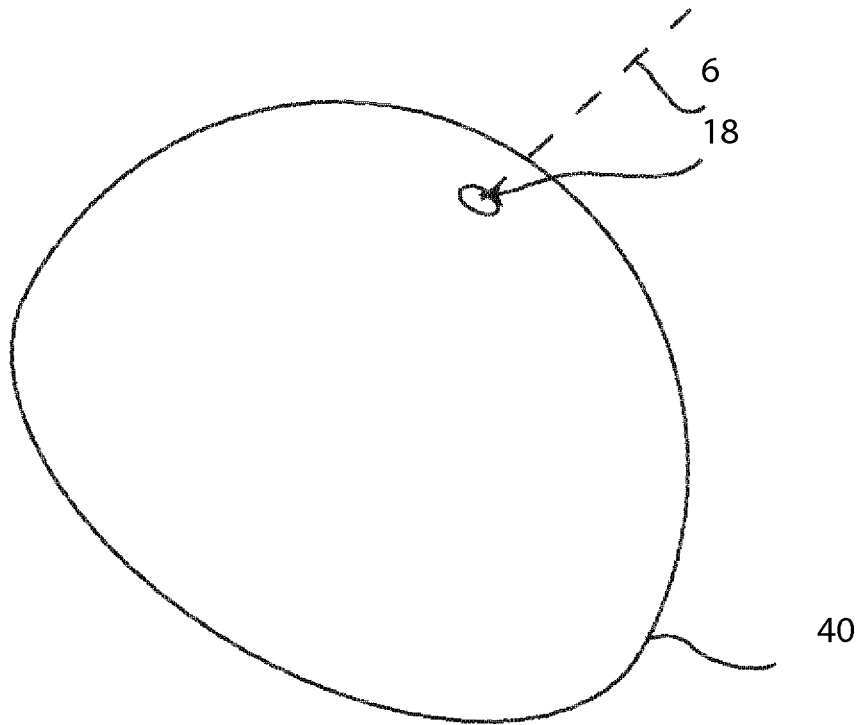


Fig. 29

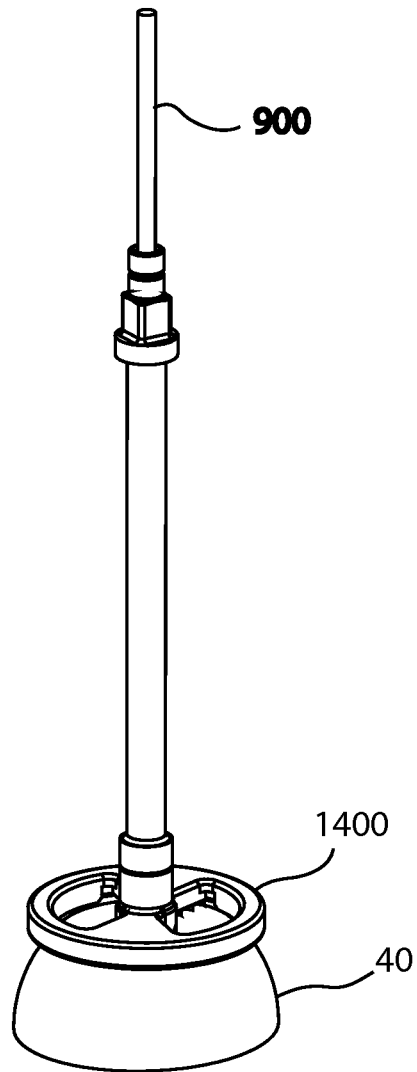


Fig. 30

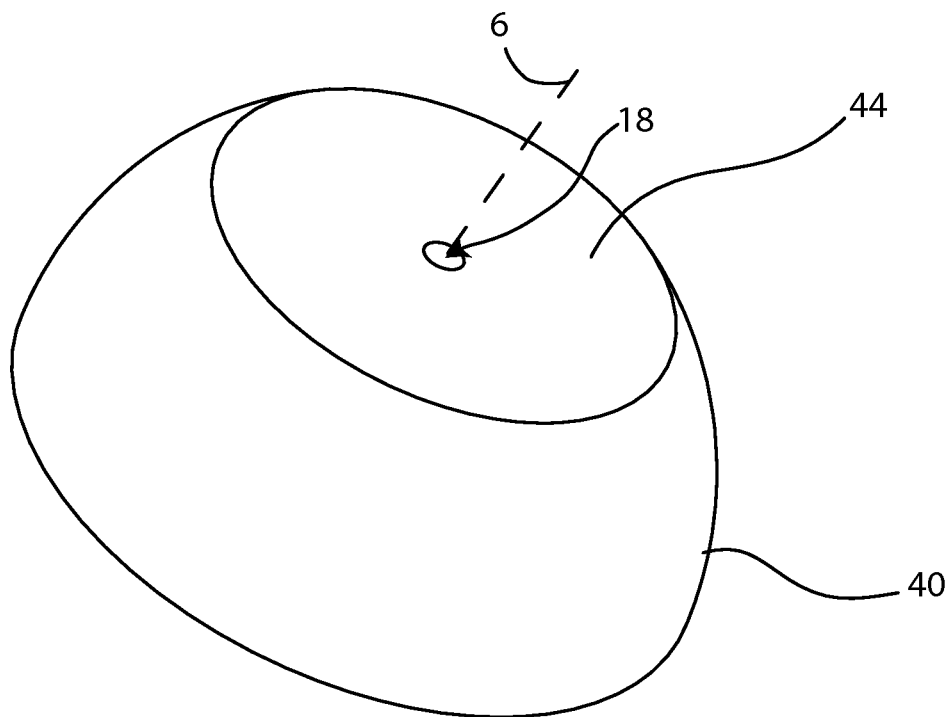


Fig. 31

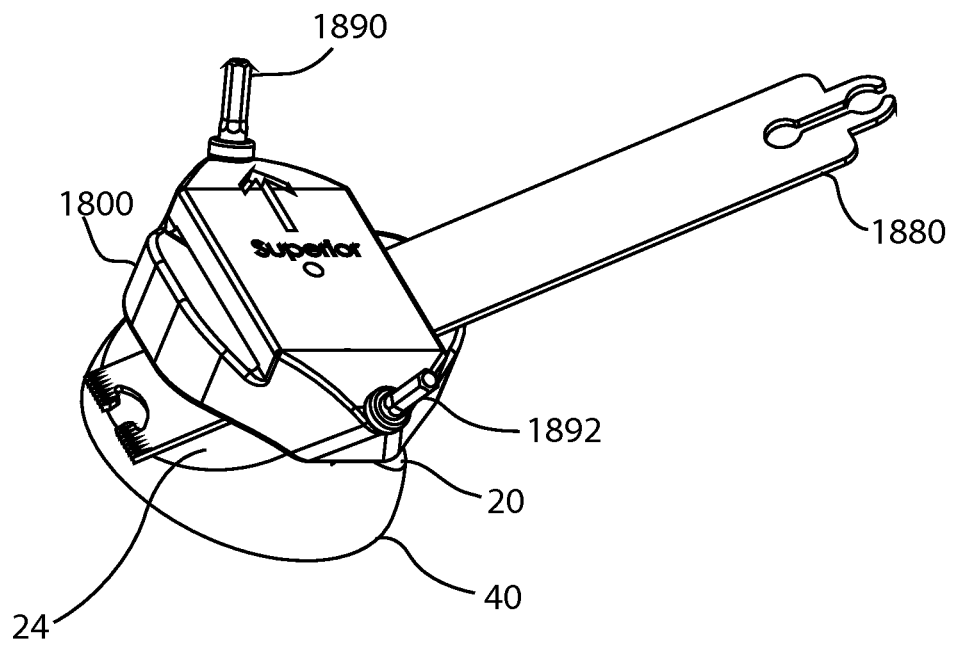


Fig. 32

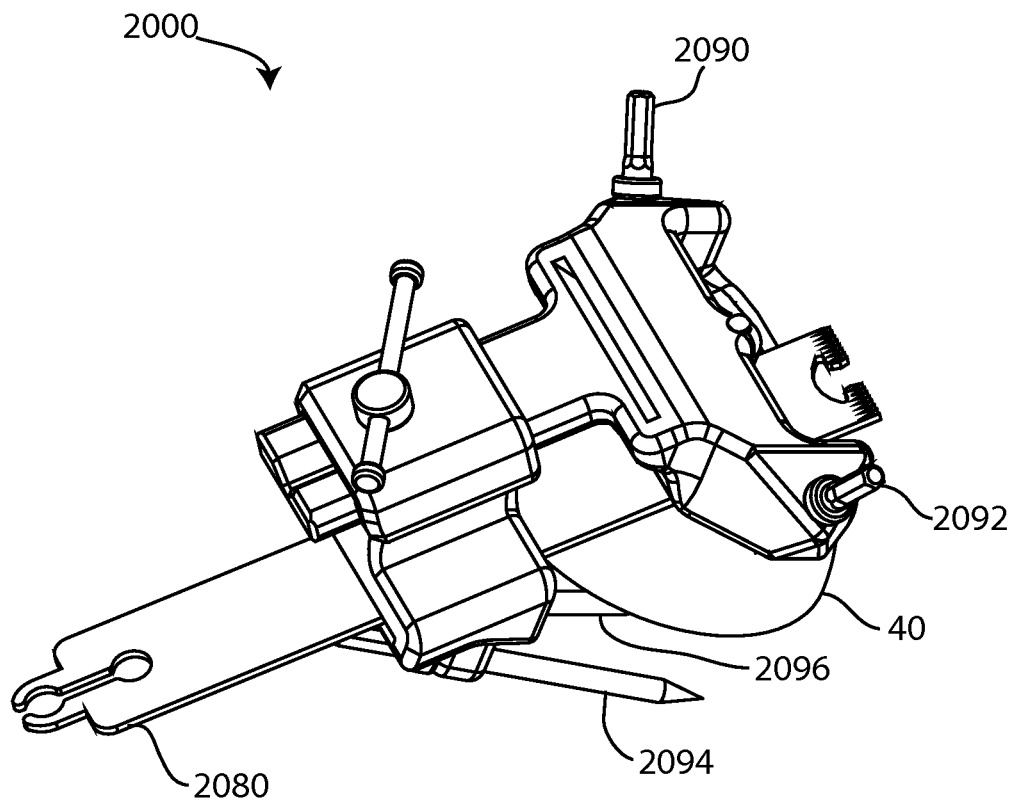


Fig. 33

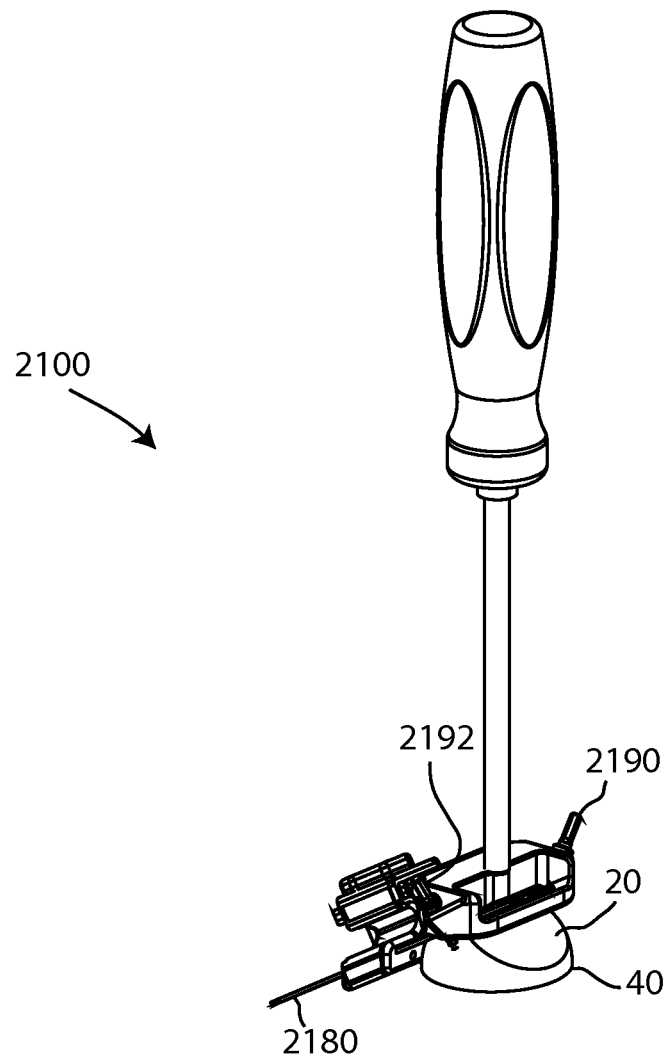


Fig. 34

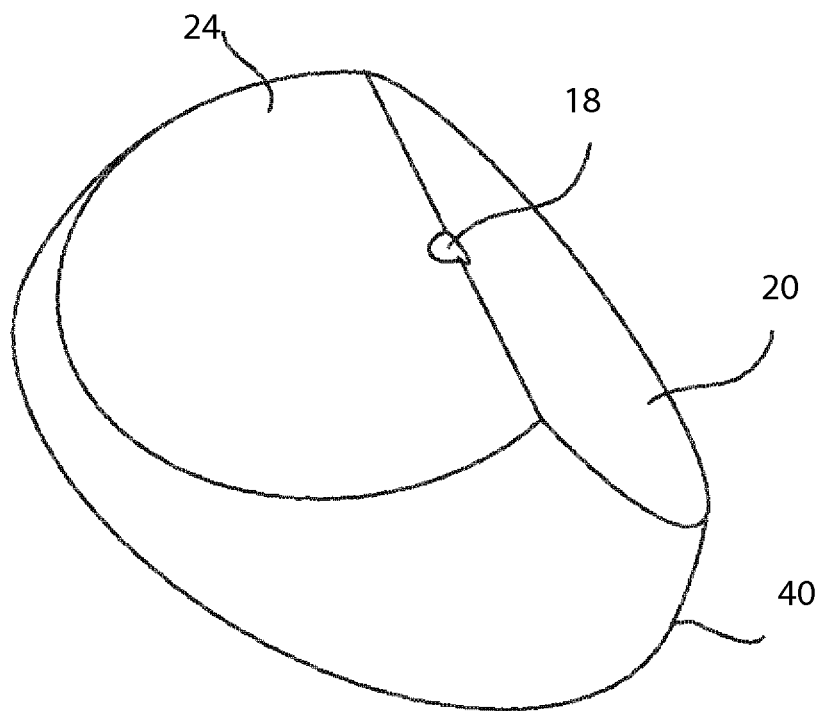


Fig. 35

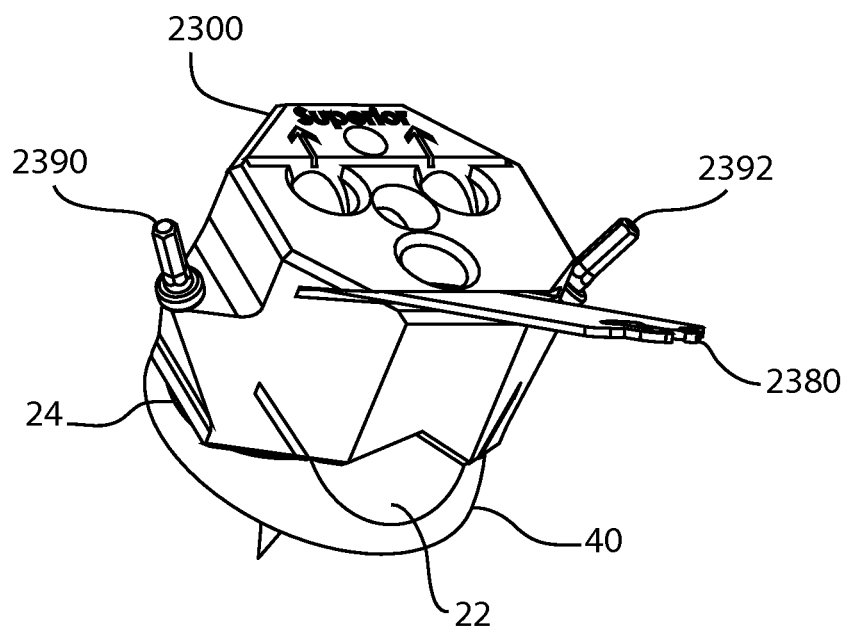


Fig. 36

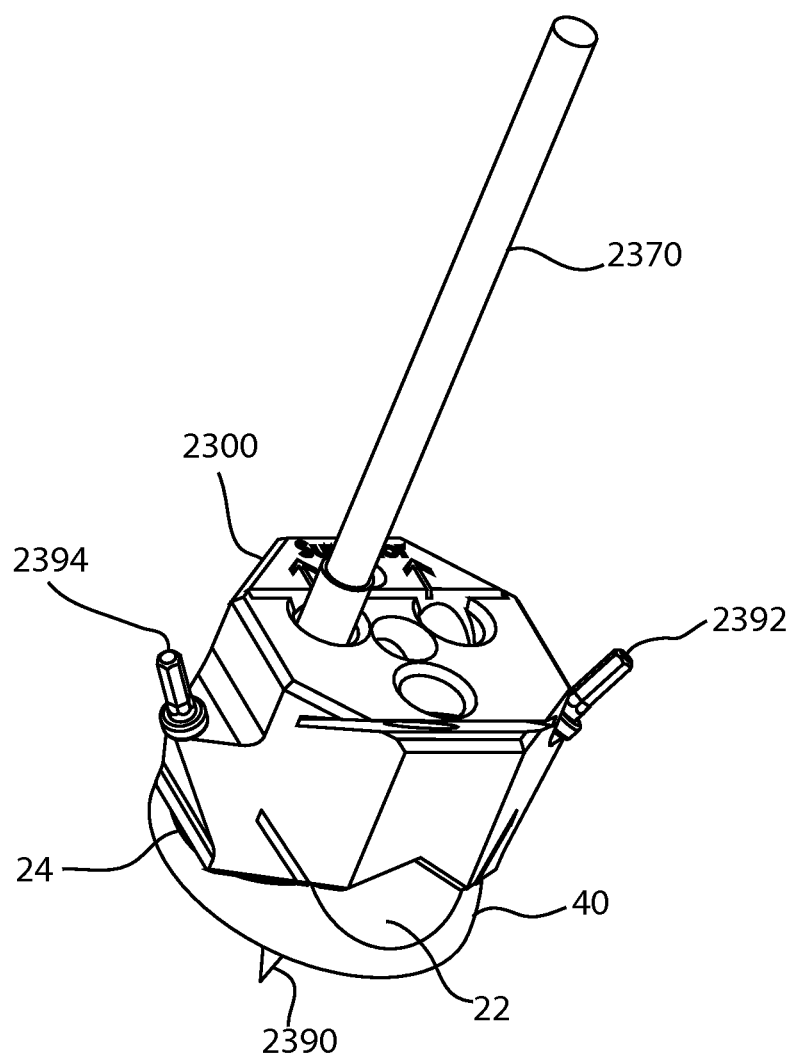


Fig. 37

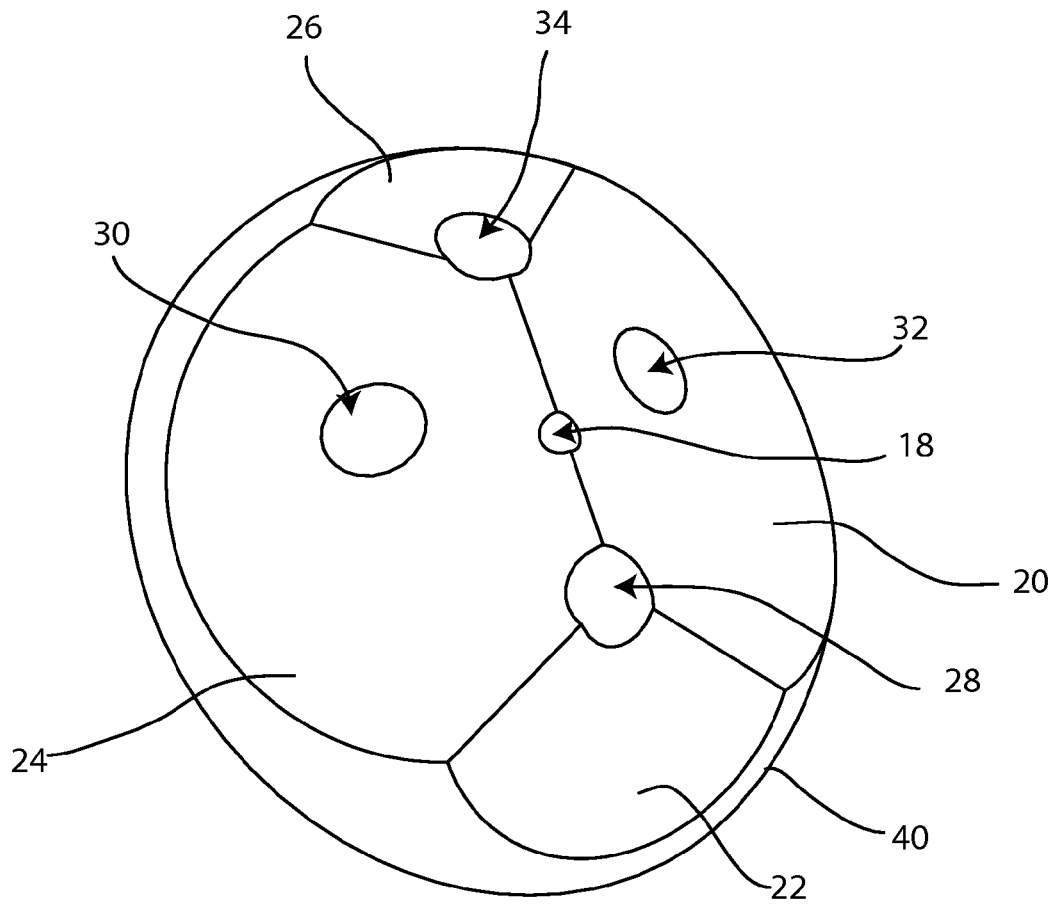


Fig.38

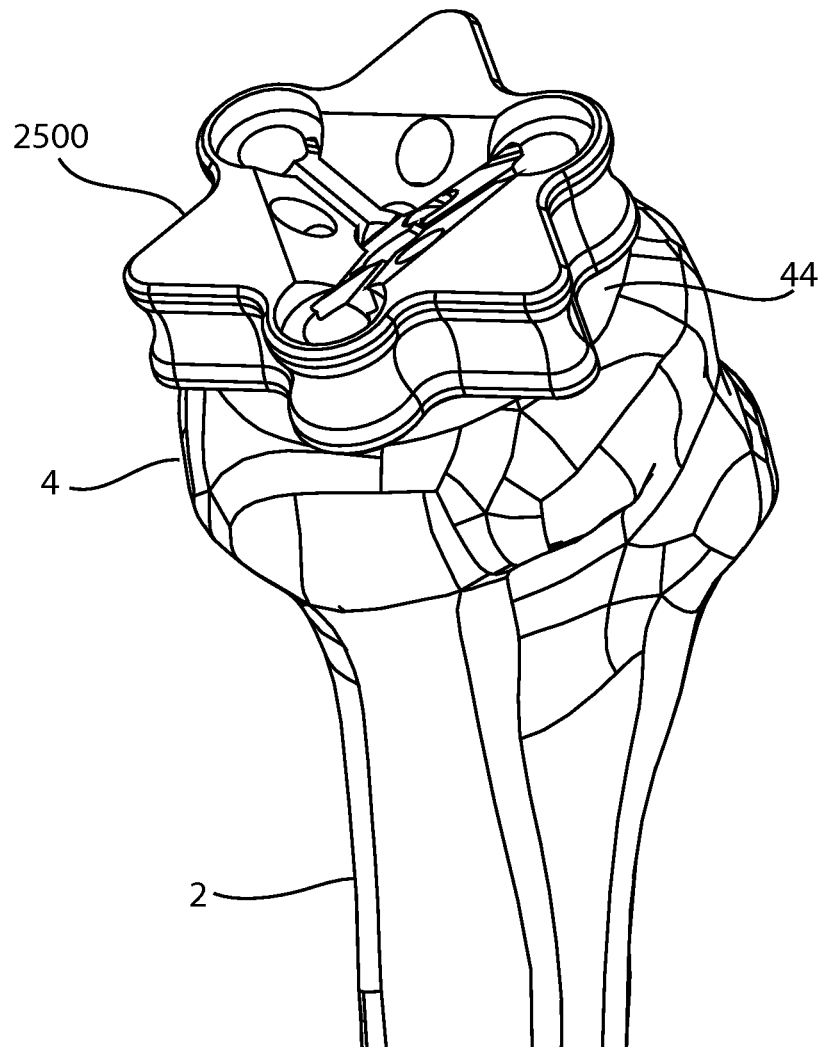


Fig. 39

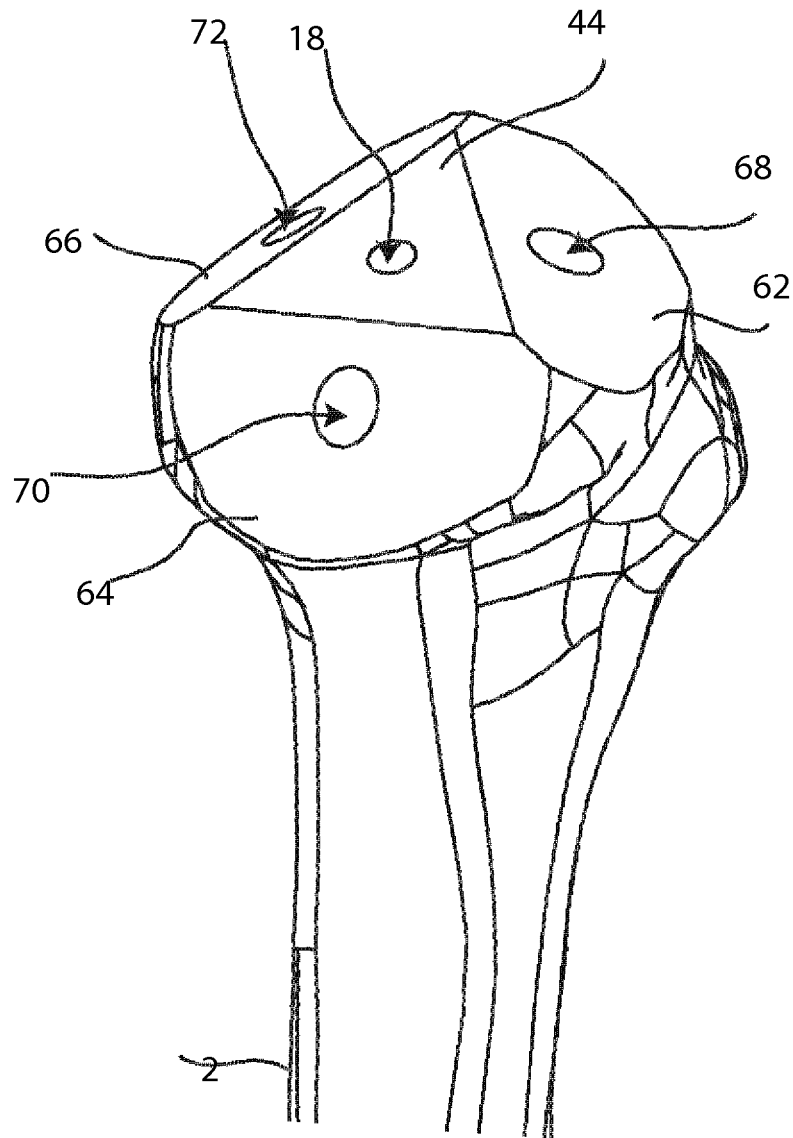


Fig. 40

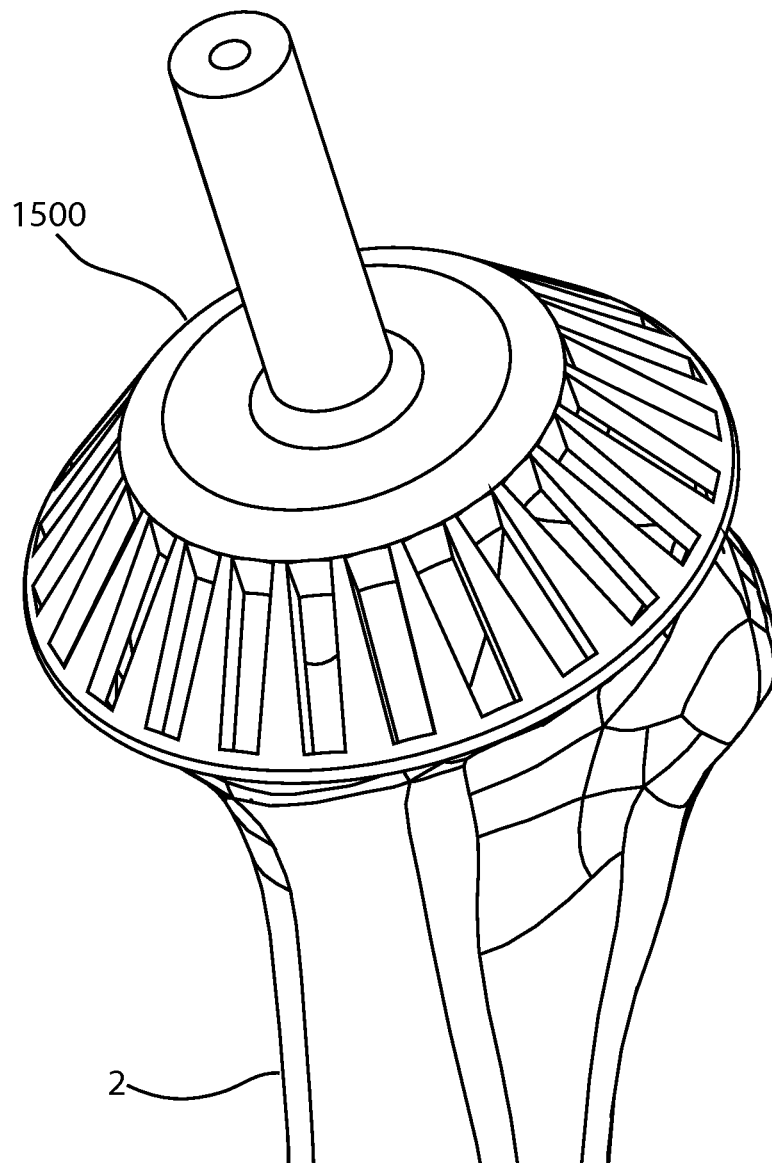


Fig. 41

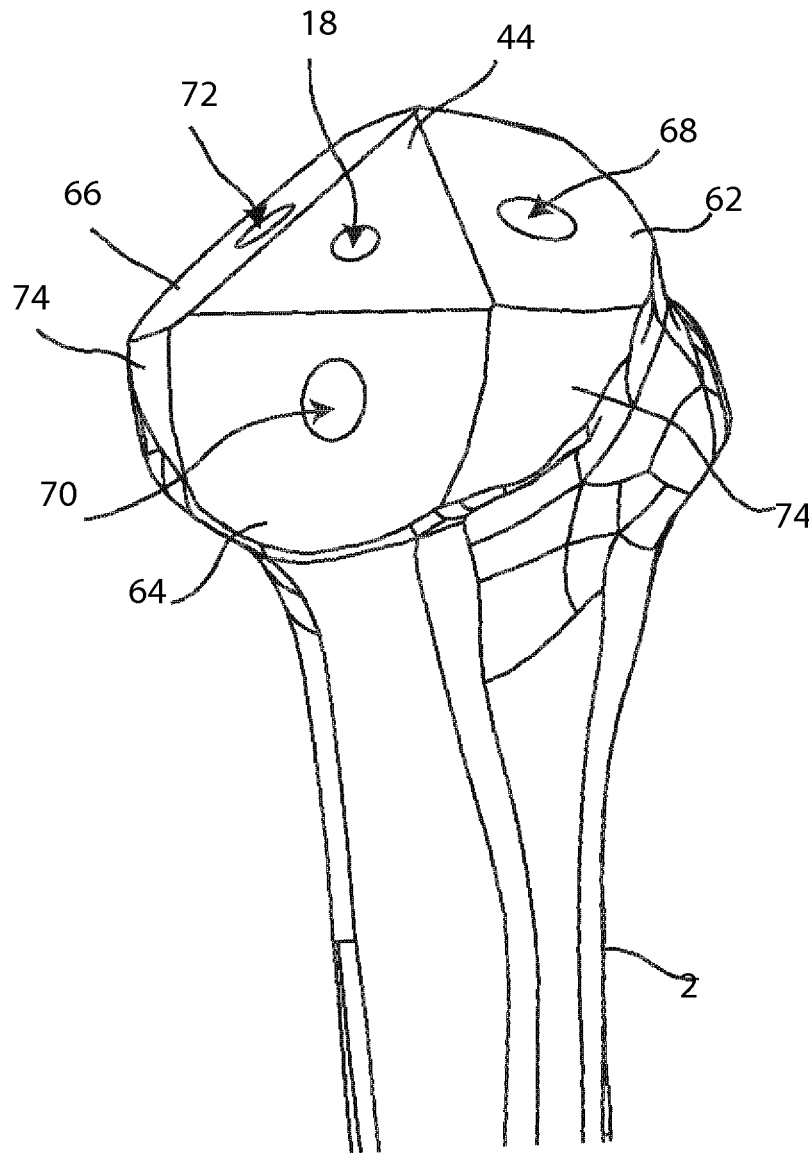


Fig. 42

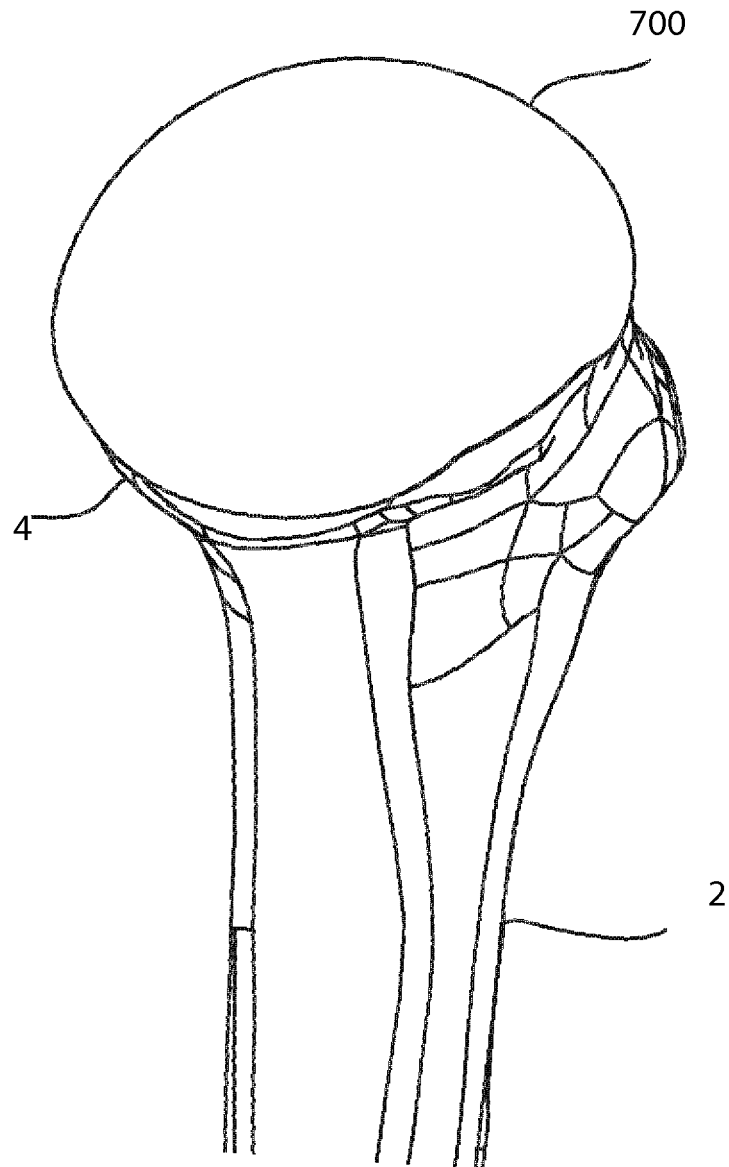


Fig. 43

1

HUMERAL ARTHROPLASTY**CROSS-REFERENCE TO RELATED APPLICATIONS**

This application claims the benefit of:

U.S. Provisional Patent Application No. 61/794,348, filed Mar. 15, 2013, entitled HUMERUS PROSTHETIC COMPONENT WITH MULTIPLE CIRCLES OF A SPHERE DESIGN AND ASSOCIATED INSTRUMENTATION.

The above referenced document is incorporated herein by reference in its entirety.

BACKGROUND

In total shoulder arthroplasty, a glenoid implant is attached to a prepared glenoid or scapula, and a humeral implant is attached to a prepared humerus. The humeral implant usually includes a convex articular surface, at a proximal end thereof which engages and moves relative to a concave articular surface formed in the glenoid implant, although this arrangement is sometimes reversed so that the humeral implant includes the convex articular surface and the glenoid implant includes the concave articular surface. The ligaments and muscles of the shoulder surround the implants and maintain the humeral implant against the glenoid implant, while at the same time allowing relative movement therebetween.

Current anatomic prostheses for the proximal humerus generally fall into two types: stemmed prostheses and resurfacing prostheses.

Stemmed prostheses are quite common. Stemmed prostheses combine a hemispherical head replacement with a stem which extends into the shaft (diaphysis) of the humerus to anchor the prosthesis. Stemmed prostheses often require the removal of the entire hemisphere of humeral head bone, as well as drilling, reaming and/or broaching into the adjacent shaft of the humerus to seat the component. The hemispherical head component and stem are typically solid metal and can be of considerable weight. Stemmed prostheses also frequently require the surgeon to place the humeral head articular bearing surface in a position which is either fixed relative to the shaft of the humerus, or has modular adjustable connection mechanisms allowing partial adjustment between the placement of the hemispherical head component and the stem placed in the shaft of the humerus. This may not always match the actual anatomy of the patient, especially if deformity is present. Although many current prostheses provide for adjustments such as retroversion, offset, or neck-shaft angle, these adjustments are always limited to some degree, or constrained, by the stem to which the prosthetic humeral head is attached.

Resurfacing prostheses have a hollow hemisphere which rests on top of the humeral bone with a solitary peg or post in the humeral head for anchoring stability. Resurfacing prostheses have the advantage of resting directly on top of the bone of the upper humerus and do not have a stem that extends into the shaft of the humerus. Therefore the surgeon is free to place the prosthesis based on each individual patient's anatomy. Resurfacing prostheses also do not require the removal of the entire humeral head bone; simply the upper articular end is reshaped to accept the prosthesis sitting on top. The prosthesis itself acts as a surface cover, and the volume of bone underneath in the hemisphere remains. This preserves more of the patient's bone stock and if revision surgery is needed, allows for a much simpler re-operation because the shaft has not yet been violated.

2

The preservation of bone in the upper humerus with a resurfacing prosthesis may unfortunately become a disadvantage when the surgeon performs a total shoulder arthroplasty. In this operation, the surgeon also places a prosthesis into the glenoid cavity of the scapula. With the bone of the upper humerus still in the way, access to the glenoid may be very difficult and placing the glenoid prosthesis properly can be challenging.

BRIEF DESCRIPTION OF THE DRAWINGS

While examples of the present technology have been shown and described in detail below, it will be clear to the person skilled in the art that variations, changes and modifications may be made without departing from its scope. As such, that which is set forth in the following description and accompanying drawings is offered by way of illustration only and not as a limitation. The actual scope of the invention is intended to be defined by the following claims, along with the full range of equivalents to which such claims are entitled.

Identical reference numerals do not necessarily indicate an identical structure. Rather, the same reference numeral may be used to indicate a similar feature or a feature with similar functionality. Not every feature of each example is labeled in every figure in which that example appears, in order to keep the figures clear. Similar reference numbers (e.g., those that are identical except for the first numeral) are used to indicate similar features in different examples.

FIG. 1A is an isometric view of a humeral component; FIG. 1B is a medial view of the humeral component of FIG. 1A; FIG. 1C is a cross sectional view of the humeral component of FIG. 1A, taken along section line 1C-1C of FIG. 1E; FIG. 1D is a superior view of the humeral component of FIG. 1A; FIG. 1E is a lateral view of the humeral component of FIG. 1A; and FIG. 1F is a cross sectional view of the humeral component of FIG. 1A, taken along section line 1F-1F of FIG. 1E;

FIG. 2A is an isometric view of another humeral component; FIG. 2B is a medial view of the humeral component of FIG. 2A; FIG. 2C is a cross sectional view of the humeral component of FIG. 2A, taken along section line 2C-2C of FIG. 2E; FIG. 2D is a superior view of the humeral component of FIG. 2A; FIG. 2E is a lateral view of the humeral component of FIG. 2A; and FIG. 2F is a cross sectional view of the humeral component of FIG. 2A, taken along section line 2F-2F of FIG. 2E;

FIG. 3A is an isometric view of yet another humeral component; FIG. 3B is a medial view of the humeral component of FIG. 3A; FIG. 3C is a cross sectional view of the humeral component of FIG. 3A, taken along section line 3C-3C of FIG. 3E; FIG. 3D is a superior view of the humeral component of FIG. 3A; FIG. 3E is a lateral view of the humeral component of FIG. 3A; and FIG. 3F is a cross sectional view of the humeral component of FIG. 3A, taken along section line 3F-3F of FIG. 3E;

FIG. 4A is an isometric view of yet another humeral component; and FIG. 4B is a lateral view of the humeral component of FIG. 4A;

FIG. 5A is an isometric view of yet another humeral component; and FIG. 5B is a lateral view of the humeral component of FIG. 5A;

FIG. 6A is a superior view of yet another humeral component; FIG. 6B is an anterior view of the humeral component of FIG. 6A; FIG. 6C is a medial view of the humeral component of FIG. 6A; FIG. 6D is an isometric view of the humeral component of FIG. 6A; FIG. 6E is an inferior view of the humeral component of FIG. 6A; FIG. 6F is a cross sectional view of the humeral component of FIG. 6A, taken along

3

section line 6F-6F of FIG. 6C, with superimposed cross sectional profiles of two other size humeral components; FIG. 6G is a cross sectional view of the humeral component of FIG. 6A, taken along section line 6G-6G of FIG. 6C, with superimposed cross sectional profiles of two other size humeral components; FIG. 6H is a front left perspective view of the humeral component of FIG. 6A; FIG. 6I is a back left perspective view of the humeral component of FIG. 6A; FIG. 6J is a back view of the humeral component of FIG. 6A; FIG. 6K is a front view of the humeral component of FIG. 6A; FIG. 6L is a right side view of the humeral component of FIG. 6A; FIG. 6M is a left side view of the humeral component of FIG. 6A; FIG. 6N is a top view of the humeral component of FIG. 6A; FIG. 6O is a bottom view of the humeral component of FIG. 6A; FIG. 6P is a cross sectional view of a left portion of the humeral component of FIG. 6A taken along line 6P-6P of FIG. 6J; and FIG. 6Q is a cross sectional view of a bottom portion of the humeral component of FIG. 6A taken along line 6Q-6Q of FIG. 6J;

FIG. 7A is an isometric view of yet another humeral component; FIG. 7B is a superior view of the humeral component of FIG. 7A; FIG. 7C is an anterior view of the humeral component of FIG. 7A; FIG. 7D is a lateral view of the humeral component of FIG. 7A; FIG. 7E is a cross sectional view of the humeral component of FIG. 7A, taken along section line 7E-7E of FIG. 7D; and FIG. 7F is a cross sectional view of the humeral component of FIG. 7A, taken along section line 7F-7F of FIG. 7D;

FIG. 8A is an isometric view of yet another humeral component; FIG. 8B is a lateral view of the humeral component of FIG. 8A; FIG. 8C is a cross sectional view of the humeral component of FIG. 8A, taken along section line 8C-8C of FIG. 8B; and FIG. 8D is a cross sectional view of the humeral component of FIG. 8A, taken along section line 8D-8D of FIG. 8B;

FIG. 9A is an isometric view of a pin and a template; and FIG. 9B is another isometric view of the template of FIG. 9A from a different viewpoint;

FIG. 10A is an isometric view of the pin of FIG. 9A and a planar reamer; and FIG. 10B is another isometric view of a portion of the pin and planar reamer of FIG. 10A from a different viewpoint;

FIG. 11A is an isometric view of a conical reamer; and FIG. 11B is another isometric view of the conical reamer of FIG. 11A from a different viewpoint;

FIG. 12A is a top view of a cutting guide; FIG. 12B is a cross sectional view of the cutting guide of FIG. 12A, taken along section line 12B-12B of FIG. 12A; FIG. 12C is a front view of the cutting guide of FIG. 12A; FIG. 12D is a side view of the cutting guide of FIG. 12A; FIG. 12E is a bottom view of the cutting guide of FIG. 12A; and FIGS. 12F, 12G, 12H, 12I, and FIG. 12J are isometric views of the cutting guide of FIG. 12A from several different viewpoints;

FIG. 13A is an isometric view of another cutting guide with the pin of FIG. 9A and two fasteners; and FIG. 13B is another isometric view of the cutting guide, pin, and fasteners of FIG. 13A from a different viewpoint;

FIG. 14 is an isometric view of yet another cutting guide with two fasteners;

FIG. 15A is an isometric view of yet another cutting guide with the pin of FIG. 9A and four fasteners; and FIG. 15B is another isometric view of the cutting guide, pin, and fasteners of FIG. 15A from a different viewpoint;

FIG. 16 is an isometric view of yet another cutting guide with two fasteners and a saw blade;

FIG. 17A is an isometric view of yet another cutting guide with three fasteners; FIG. 17B is another isometric view of the

4

cutting guide and fasteners of FIG. 17A from a different viewpoint; and FIG. 17C is another isometric view of the cutting guide and fasteners of FIG. 17A with a drill, from the viewpoint of FIG. 17A;

FIG. 18 is an isometric view of yet another cutting guide with two fasteners;

FIG. 19A is an isometric view of yet another cutting guide; and FIG. 19B is another isometric view of the cutting guide of FIG. 19A with three fasteners, from a different viewpoint;

FIG. 20A is an isometric view of an intact proximal humerus along the humeral neck axis; and FIG. 20B is an isometric view of the proximal humerus of FIG. 20A from a postero-medial viewpoint;

FIG. 21A is an isometric view of the proximal humerus of FIG. 20A along the humeral neck axis after a posterior bone resection has been made; and FIG. 21B is an isometric view of the proximal humerus of FIG. 21A from a postero-medial viewpoint;

FIG. 22A is an isometric view of the proximal humerus of FIG. 21A along the humeral neck axis after an inferior bone resection has been made; and FIG. 22B is an isometric view of the proximal humerus of FIG. 22A from a postero-medial viewpoint;

FIG. 23A is an isometric view of the proximal humerus of FIG. 22A along the humeral neck axis after an anterior bone resection has been made; and FIG. 23B is an isometric view of the proximal humerus of FIG. 23A from a postero-medial viewpoint;

FIG. 24A is an isometric view of the proximal humerus of FIG. 23A along the humeral neck axis after a superior bone resection has been made; and FIG. 24B is an isometric view of the proximal humerus of FIG. 24A from a postero-medial viewpoint;

FIG. 25A is an isometric view of the proximal humerus of FIG. 24A along the humeral neck axis after an inferior bone hole has been made; and FIG. 25B is an isometric view of the proximal humerus of FIG. 25A from a postero-medial viewpoint;

FIG. 26A is an isometric view of the proximal humerus of FIG. 25A along the humeral neck axis after anterior and posterior bone holes have been made; and FIG. 26B is an isometric view of the proximal humerus of FIG. 26A from a postero-medial viewpoint;

FIG. 27 is an isometric view of the template and pin of FIG. 9A operatively arranged relative to a simplified humeral head represented by a hemisphere;

FIG. 28 is an isometric view of the template, pin, and simplified humeral head of FIG. 27 operatively arranged relative to an alignment guide;

FIG. 29 is an isometric view of the simplified humeral head of FIG. 27 after a central pin hole has been made;

FIG. 30 is an isometric view of the planar reamer and pin of FIG. 10A operatively arranged relative to the simplified humeral head of FIG. 29;

FIG. 31 is an isometric view of the simplified humeral head of FIG. 30 after a planar bone resection has been made perpendicular to the pin hole;

FIG. 32 is an isometric view of the cutting guide and fasteners of FIG. 13A and a saw blade operatively arranged relative to the simplified humeral head of FIG. 31;

FIG. 33 is an isometric view of the cutting guide and fasteners of FIG. 15A and a saw blade operatively arranged relative to the simplified humeral head of FIG. 31;

FIG. 34 is an isometric view of the cutting guide and fasteners of FIG. 16 and a saw blade operatively arranged relative to the simplified humeral head of FIG. 31;

FIG. 35 is an isometric view of the simplified humeral head of FIG. 32 after anterior and posterior bone resections have been made;

FIG. 36 is an isometric view of the cutting guide and fasteners of FIG. 17A and a saw blade operatively arranged relative to the simplified humeral head of FIG. 35;

FIG. 37 is an isometric view of the cutting guide, fasteners, and simplified humeral head of FIG. 36 operatively arranged relative to the drill of FIG. 17C;

FIG. 38 is an isometric view of the simplified humeral head of FIG. 37 after superior and inferior bone resections and superior, inferior, anterior, and posterior bone holes have been made;

FIG. 39 is an isometric view of the cutting guide and fasteners of FIG. 19B operatively arranged with a proximal humerus;

FIG. 40 is an isometric view of the proximal humerus of FIG. 39, after inferior, antero-superior, and postero-superior bone resections and bone holes have been made;

FIG. 41 is an isometric view of the conical reamer of FIG. 11A operatively arranged with the proximal humerus of FIG. 40;

FIG. 42 is an isometric view of the proximal humerus of FIG. 41, after a conical resection has been made; and

FIG. 43 is an isometric view of the proximal humerus of FIG. 42, after the humeral component of FIG. 7 has been implanted.

DETAILED DESCRIPTION

Standard medical planes of reference and descriptive terminology are employed in this specification. A sagittal plane divides a body into right and left portions. A mid-sagittal plane divides the body into bilaterally symmetric right and left halves. A coronal plane divides a body into anterior and posterior portions. A transverse plane divides a body into superior and inferior portions. Anterior means toward the front of the body. Posterior means toward the back of the body. Superior means toward the head. Inferior means toward the feet. Medial means toward the midline of the body. Lateral means away from the midline of the body. Axial means toward a central axis of the body. Abaxial means away from a central axis of the body. Ipsilateral means on the same side of the body. Contralateral means on the opposite side of the body. These descriptive terms may be applied to an animate or inanimate body.

One of the objectives of the present technology is to provide a prosthesis for the articular surface of the proximal humerus that allows for a bone preserving and anatomically accurate surgical operation. The disclosed prosthesis requires several small bone cuts to remove a small amount of bone from the upper humerus, but significantly less than a stemmed prosthesis. However the small amount of bone removed may be just enough to allow improved access to a surgeon who also is placing a glenoid prosthesis, especially if the glenoid prosthesis uses an oblique angle of insertion. The disclosed humeral prosthesis still rests on the surface of the upper humerus and does not extend into the humeral shaft, unless the surgeon chooses to use a longer stemmed example.

The disclosed humeral prosthesis can be modified by varying the size, angle and relative location of each individual circle of a sphere relative to the other circles. The prosthesis may be altered in discrete regions to adapt the component precisely to cover or avoid certain surrounding anatomical structures, such as the rotator cuff tendon insertions of the teres minor, infraspinatus, supraspinatus, and subscapularis

muscles. This cannot be done with a prosthesis designed as a single hemisphere and having an articular margin which lies on a plane.

Another design, known as a stemless hemiarthroplasty prosthesis, also uses a hemispherical humeral head implant placed on top of the upper humerus after a standard humeral head cut has been made. Though this design does not require the placement of a stem, the solid large metal head is of the same volume and weight as a comparable head used in a stemmed design, but is anchored by a shallow fixation apparatus.

An objective of the present technology is to disclose a prosthesis for the articular surface of the proximal humerus having overlapping circles of a sphere.

Another objective of the present technology is to disclose a prosthesis for the articular surface of the proximal humerus having an ellipsoid shape of the humeral articular surface.

Still another objective of the present technology is to disclose a prosthesis for the articular surface of the proximal humerus having a long stem example of a resurfacing type prosthesis.

Another objective of the present technology is to disclose a cutting guide instrument used to prepare the bone to seat the humerus prosthesis.

Advantages of the present technology include the multiple joined circle-of-a-sphere design, which requires less removal of bone than a standard hemiarthroplasty. Due to significantly reduced volume, the metal humeral component weighs significantly less than a standard hemispherical humeral component of corresponding size, but provides nearly equal surface area coverage of the proximal humeral articular surface. The reduced weight of the humeral component may improve shoulder kinematics. The reduced weight of the humeral component may also contribute to improved long-term stability by reducing loosening forces placed on the anchoring elements. Reduced volume of metal may also potentially reduce material costs of manufacturing the implant.

The humeral canal is not violated during the surgical procedures disclosed herein, reducing blood loss and marrow-fat emboli release into the blood. The canal is also preserved for future stemmed arthroplasty components if revision surgery is ever required. This does not apply in the case of the long stem example.

The undersurface design resulting from overlapping planar bone cuts provides resistance to rotational forces and is potentially more stable than a single flat cut. This may provide for improved long-term stability of the component. By making multiple oblique cuts through the humeral head surface, a greater proportion of the component will be resting again the strong outer cortical bone of the humerus than a standard hemispherical prosthesis.

The present design does not require or reference the humeral canal to determine proper location for bone cuts, thus the surgeon is free to position the humeral component to best fit each patient's individual anatomy. This is even more important in cases where deformity has altered the normal shape of the humerus.

The articular surface of the humeral prosthesis can be ellipsoid to better match the normal anatomy of the humerus. Current stemmed and resurfacing arthroplasty designs, due to the variable-offset feature of stemmed designs and the bone preparation process of resurfacing designs, include only spherical humeral heads.

The most inferior circle of the prosthesis extends inferiorly to cover the most medial aspect of the medial humeral neck bone, in order to reduce the incidence of impingement of the medial humerus against a glenoid prosthetic component.

Retrieval studies of failed glenoid components have shown that inferior impingement is a significant contributor to glenoid loosening.

By placing the prosthesis more precisely in a location that better replicates the normal anatomy, motion across the glenohumeral joint may be more smooth and stable, and eccentric forces placed upon the glenoid prosthesis may be reduced.

The current prosthesis can be finely adjusted by varying the size, angle and relative location of each individual circle of a sphere relative to the other circles. This allows the prosthesis to be altered in discrete regions for clinical purposes.

Other objectives and advantages of this technology will become apparent from the following description taken in conjunction with the accompanying drawings wherein are set forth, by way of illustration and example, certain embodiments of the technology. The drawings contained herein constitute a part of this specification and include exemplary embodiments of the present technology and illustrate various objects and features thereof.

Referring to FIGS. 1A-1F, a humeral component **100** includes an articular surface **102** and a bone-facing side **104** which is opposite to the articular surface.

The humeral component **100** has a smooth, polished articular bearing surface **102** which may articulate with a natural glenoid socket or a glenoid prosthetic component. The glenoid prosthetic component may be of the type disclosed in U.S. Provisional Patent Application No. 61/776,398, filed Mar. 11, 2013, and entitled OBLIQUE-INSERTION ANCHORING MECHANISM FOR GLENOID PROSTHETIC COMPONENT; or the type disclosed in U.S. patent application Ser. No. 14/042,258, filed Sep. 30, 2013, and entitled GLENOID ARTHROPLASTY. The contents of these documents are incorporated herein by reference. The glenoid component may be polyethylene or another biocompatible material.

The prosthetic humeral component may be designed as multiple overlapping circles of a sphere, where the sphere forms the articular surface **102**. A "circle of a sphere" is a circle defined by the intersection of a sphere and a plane. If the plane contains the center of the sphere, then the circle is called a "great circle"; otherwise, it is a "small circle." A "spherical cap" is a three-dimensional portion of a sphere cut off by an intersecting plane. If the plane passes through the center of the sphere, the spherical cap is called a "hemisphere." If the height of the spherical cap is less than the radius of the sphere, the spherical cap is called a "minor spherical cap." If the height of the spherical cap is greater than the radius of the sphere, the spherical cap is called a "major spherical cap." In this specification, any reference to a circle of a sphere is also a reference to the corresponding spherical cap, and any reference to a spherical cap is also a reference to the corresponding circle of the sphere.

Together these overlapping circles of a sphere, and corresponding spherical caps, form an articular surface which is nearly hemispherical, or partly spherical, but with significantly less volume of material than a solid hemisphere due to the multiple planar surfaces on the bone facing side **104**, which in a solid hemisphere would be flat. The articular surface area created by the overlapping circles of a sphere nearly covers the native articular surface of the proximal humerus. Referring to FIG. 1A, each one of the planar surfaces corresponds to one of the overlapping circles of a sphere or spherical caps. All of the spherical surfaces are co-radial; they share the same spherical center and all spherical radii are equal, so that the articular surface **102** is an uninterrupted spherical surface. Some examples of the present technology

utilize four overlapping circles of a sphere, but other examples may have three, five or more overlapping circles of a sphere.

In an alternate version of the technology, the prosthetic humeral component **100** may have an ellipsoid or ovoid articular surface **102**, rather than a spherical articular surface. The circles of an ellipsoid or ovoid, and the corresponding caps, may be overlapped to create the same effect of covering a similar amount of surface area with a reduced volume of material. The ellipsoid or ovoid articular surface has a first radius (or first diameter) in a first plane or along a first axis which is dimensionally different from a second radius (or second diameter) in a second plane or along a second axis. The first radius may be larger or smaller than the second radius. Referring to FIGS. 1C, 1E, and 1F, the radius of articular surface **102** in FIG. 1C may be dimensionally different from the radius of articular surface **102** in FIG. 1F when the articular surface **102** is ellipsoid or ovoid instead of spherical. For example, an ellipsoid or ovoid articular surface may have a larger diameter along the superior-inferior axis in the coronal plane than in the transverse plane, or vice versa. The increased radius of curvature of an ellipsoid or ovoid bearing surface in a given direction may reduce the constraint of the humeral head within the glenohumeral joint in that direction. This reduced constraint may result in reduced eccentric forces applied to the bearing surface and reduced risk of implant loosening. The increased radius of curvature may be oriented relative to the prevailing direction of articulation of a given joint, or relative to an articulation direction in which impingement, loosening, or other stress-related effects are known to occur. These ellipsoid or ovoid shapes may also be narrower at the superior end and broader at the inferior end. The ellipsoid or ovoid shape may better replicate the normal articular surface of the humeral head, better replicating the kinematics of the shoulder during articulation, and better matching the morphology of the natural articulating surface, allowing for better fit and transition between the implant and the bone, at least in some patients.

Humeral components according to the present technology may also be designed as a hemisphere, spherical cap, ellipsoid cap, or ovoid cap with a tapered polygonal socket forming the bone-facing side. The tapered polygonal socket may be designed by extruding a polygonal shape from the flat side of the hemisphere or cap toward the articular surface while tapering the sides of the polygonal shape inward. The polygonal shape may be a triangle, square, rectangle, pentagon, or other polygonal shape, and may be regular or irregular, and may be symmetrically or asymmetrically disposed relative to the center of the hemisphere or cap. The sides of the polygonal shape may all have the same taper angle, although one or more sides may have a different taper angle. It can be appreciated that the bone-facing side **104** of humeral component **100** may be designed as a tapered rectangular socket, and similarly for humeral components **200**, **300**, **400**, **500**, **600** discussed below.

Humeral component **100** may include four planar surfaces **120**, **122**, **124**, **126** in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface **102**, as seen best in FIG. 1A. Other examples may include three, five, or more planar surfaces in a concave arrangement. More specifically, one example may include planar surfaces **120**, **122**, **124**. The planar surfaces diverge as they extend away from the middle of the articular surface **102**, and intersect the articular surface to establish an articular margin **106** around a perimeter of the humeral component **100**. The articular margin may be described as scalloped or having one or more indentations

129. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surfaces 120, 124 intersect along a line 119, planar surfaces 120, 126 intersect along a line 121, planar surfaces 120, 122 intersect along a line 123, planar surfaces 124, 126 intersect along a line 125, and planar surfaces 124, 122 intersect along a line 127. The lines 119, 121, 123, 125, 127 may also be referred to as intersections, edges, or internal corners, and may include fillet radii, as best seen in FIG. 1E. Referring to FIG. 1E, lines 119, 123, 127 intersect at a first point 111; and lines 119, 121, 125 intersect at a second point 113. Lines 123, 121 and 127, 125 also intersect when extended. Line 119 in this example may extend in a superior-inferior direction when the humeral component 100 is implanted.

The humeral component 100 may have a roughened or porous bone-facing side 104, or undersurface, which rests on the prepared bone of the humerus when the humeral component is implanted. These roughened or porous surfaces assist in bony apposition between the implant and the underlying subcondylar bone encouraging bony ingrowth into the porosity of the bone-facing side once the humeral component is implanted. From this undersurface or bone-facing side 104, at least one anchoring element 128 projects outwardly; the example shown includes three anchoring elements 128, 130, 132. The anchoring elements project into the humeral bone when the humeral component is implanted, and may anchor the humeral component to prevent loosening or micromotion. The anchoring elements may be pegs which are round, cruciate, or have fins, or have another cross sectional shape for bone fixation. The anchoring elements may include fenestrations. Some of the examples disclosed herein utilize three pegs, but the number of pegs may vary. The pegs may be parallel, converging, diverging, or skew. The pegs may be smooth, matte, rough, or porous to promote bone cement fixation or bone ingrowth. The illustrated anchoring elements 128, 130, 132 are cylindrical and parallel to one another. Anchoring element 128 is longer than anchoring elements 130, 132, and may therefore be suited for implantation in an inferior aspect of the humeral head/neck.

Humeral component 100 is bilaterally symmetric about a plane through line 119, and may therefore be implanted in right or left shoulders. Humeral component 100 may be implanted so that planar surface 126 covers a superior aspect of the humeral head, planar surface 122 covers an inferior aspect of the humeral head, planar surfaces 120 and 124 cover anterior and posterior portions of the humeral head, anchoring element 128 extends through the inferior aspect of the humeral head and optionally into the humeral neck, and anchoring elements 130, 132 extend into anterior and posterior portions of the humeral head. The outer portion, or rim, of planar surface 126 faces at least a portion of the rotator cuff, and, because planar surface 126 is indented to form the indentation 129 along the articular margin 106, a space exists between the rim of planar surface 126 and the rotator cuff. This space provides relief, or room, for the rotator cuff to function without excessively rubbing against the outer portion, or rim, of the humeral component 600, thus reducing the risk of rotator cuff damage.

In one example, the inferior-most peg may be curved and elongated, forming a stem which extends distally into the diaphysis of the humerus, following the curve of the medial neck of the humerus. This inferior peg or stem may be manufactured as one piece with the bearing surface component, or the peg or stem may be modular, supplied in varying thickness

and lengths. A modular peg may be attached to the bearing portion of the component via a Morse taper, screw-in or other connection mechanism.

In another embodiment, the location of the pegs on the backside of the prosthetic component may project in a more vertical direction. This embodiment may be suitable for a surgeon utilizing a subscapularis-preserving surgical technique where the only exposure to the humerus is from the superior direction.

The prosthesis may be fixed in place with bone cement, or it may have a roughened surface or porous coating on the undersurface for cementless (press-fit) use.

The entire humeral component 100 may be made of a solid metal piece. In other examples, the prosthesis may be made of another material, such as any of the materials commonly used in orthopaedic joint arthroplasty, such as ceramic, composite, polyethylene or pyrocarbon. Combinations of materials may also be used.

Referring to FIGS. 2A-2F, another humeral component 200 includes an articular surface 202 and a bone-facing side 204 which is opposite to the articular surface. Humeral component 200 includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component 100: planar surfaces 220, 222, 224, 226; lines 219, 221, 223, 225, 227; points 211, 213; and anchoring elements 228, 230, 232. In an alternate version of the technology, the prosthetic humeral component 200 may have an ellipsoid or ovoid articular surface 202, rather than a spherical articular surface. The planar surfaces 220, 222, 224, 226 are in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface 202, as seen best in FIG. 2A. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Fillet radii are present along lines 221, 225 and absent along lines 219, 223, 227. The illustrated anchoring elements 228, 230, 232 are cylindrical and parallel to one another. These anchoring elements include bilateral longitudinal grooves 236. Anchoring element 228 is longer than anchoring elements 230, 232, and may therefore be suited for implantation in an inferior aspect of the humeral head/neck.

Humeral component 200 is bilaterally symmetric about a plane through line 219, and may therefore be implanted in right or left shoulders. Humeral component 200 may be implanted so that planar surface 226 covers a superior aspect of the humeral head, planar surface 222 covers an inferior aspect of the humeral head, planar surfaces 220 and 224 cover anterior and posterior portions of the humeral head, anchoring element 228 extends through the inferior aspect of the humeral head and optionally into the humeral neck, and anchoring elements 230, 232 extend into anterior and posterior portions of the humeral head.

Referring to FIGS. 3A-3F, yet another humeral component 300 includes an articular surface 302 and a bone-facing side 304 which is opposite to the articular surface. Humeral component 300 includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component 100: planar surfaces 320, 322, 324, 326; lines 319, 321, 323, 325, 327; fillet radii; points 311, 313; and anchoring elements 328, 330, 332. In an alternate version of the technology, the prosthetic humeral component 300 may have an ellipsoid or ovoid articular surface 302, rather than a spherical articular surface. The planar surfaces 320, 322, 324, 326 are in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface 302, as seen best in FIG. 3A. Each one of the planar surfaces intersects each other planar

11

surface at an obtuse angle, although right angles and acute angles are also contemplated. The illustrated anchoring elements 330, 332 are cylindrical and parallel to one another. Anchoring element 328 is curved outwardly, and is longer than anchoring elements 330, 332, and may therefore be suited for implantation in an inferior aspect of the humeral head/neck. Anchoring element 328 also includes four longitudinal grooves 336, which are evenly arranged around anchoring element 328. Anchoring element 328 may be described as having a diamond-shaped or star-shaped cross section.

Humeral component 300 is bilaterally symmetric about a plane through line 319, and may therefore be implanted in right or left shoulders. Humeral component 300 may be implanted so that planar surface 326 covers a superior aspect of the humeral head, planar surface 322 covers an inferior aspect of the humeral head, planar surfaces 320 and 324 cover anterior and posterior portions of the humeral head, anchoring element 328 extends through the inferior aspect of the humeral head and optionally into the humeral neck, and anchoring elements 330, 332 extend into anterior and posterior portions of the humeral head.

Referring to FIGS. 4A-4B, yet another humeral component 400 includes an articular surface 402 and a bone-facing side 404 which is opposite to the articular surface. Humeral component 400 includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component 100: planar surfaces 420, 422, 424, 426; lines 419, 421, 423, 425, 427; fillet radii; points 411, 413; and anchoring elements 428, 430, 432. In an alternate version of the technology, the prosthetic humeral component 400 may have an ellipsoid or ovoid articular surface 402, rather than a spherical articular surface. The planar surfaces 420, 422, 424, 426 are in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface 402, as seen best in FIG. 4A. The planar surfaces diverge as they extend away from the middle of the articular surface 402, and intersect the articular surface to establish an articular margin 406 around a perimeter of the humeral component 400. The articular margin may be described as scalloped or having one or more indentations 429. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surface 426 has a smaller area than planar surface 422, and may be described as being indented, or centrally offset, particularly in comparison to planar surface 422. Humeral component 400 includes a fourth anchoring element 434. The illustrated anchoring elements 428, 430, 432, 434 are cylindrical and parallel to one another. Anchoring elements 428, 430, 432, 434 also include bilateral longitudinal grooves 436.

Humeral component 400 is bilaterally symmetric about a plane through line 419, and may therefore be implanted in right or left shoulders. Humeral component 400 may be implanted so that planar surface 426 covers a superior aspect of the humeral head, planar surface 422 covers an inferior aspect of the humeral head, planar surfaces 420 and 424 cover anterior and posterior portions of the humeral head, anchoring element 428 extends through the inferior aspect of the humeral head and optionally into the humeral neck, anchoring elements 430, 432 extend into anterior and posterior portions of the humeral head, and anchoring element 434 extends into the superior aspect of the humeral head. The outer portion, or rim, of planar surface 426 faces at least a portion of the rotator cuff, and, because planar surface 426 is indented to form the indentation 429 along the articular margin 406, a space exists between the rim of planar surface 426 and the

12

rotator cuff. This space provides relief, or room, for the rotator cuff to function without excessively rubbing against the outer portion, or rim, of the humeral component 600, thus reducing the risk of rotator cuff damage.

Referring to FIGS. 5A-5B, yet another humeral component 500 includes an articular surface 502 and a bone-facing side 504 which is opposite to the articular surface. Humeral component 500 includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component 100: planar surfaces 520, 522, 524, 526; lines 519, 521, 523, 525, 527; fillet radii; points 511, 513; and anchoring elements 528, 530, 532. In an alternate version of the technology, the prosthetic humeral component 500 may have an ellipsoid or ovoid articular surface 502, rather than a spherical articular surface. The planar surfaces 520, 522, 524, 526 are in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface 502, as seen best in FIG. 5A. The planar surfaces diverge as they extend away from the middle of the articular surface 502, and intersect the articular surface to establish an articular margin 506 around a perimeter of the humeral component 500. The articular margin may be described as scalloped or having one or more indentations 529. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surface 526 has a smaller area than planar surface 522, and may be described as being indented, or centrally offset, particularly in comparison to planar surface 522. Humeral component 500 includes a fourth anchoring element 534. The illustrated anchoring elements 528, 530, 532, 534 are cylindrical and parallel to one another. Anchoring element 528 may be longer than anchoring elements 530, 532, 534. Anchoring elements 528, 530, 532, 534 also include bilateral longitudinal grooves 536.

Humeral component 500 is bilaterally symmetric about a plane through line 519, and may therefore be implanted in right or left shoulders. Humeral component 500 may be implanted so that planar surface 526 covers a superior aspect of the humeral head, planar surface 522 covers an inferior aspect of the humeral head, planar surfaces 520 and 524 cover anterior and posterior portions of the humeral head, anchoring element 528 extends through the inferior aspect of the humeral head and optionally into the humeral neck, anchoring elements 530, 532 extend into anterior and posterior portions of the humeral head, and anchoring element 534 extends into the superior aspect of the humeral head. The outer portion, or rim, of planar surface 526 faces at least a portion of the rotator cuff, and, because planar surface 526 is indented to form the indentation 529 along the articular margin 506, a space exists between the rim of planar surface 526 and the rotator cuff. This space provides relief, or room, for the rotator cuff to function, thus reducing the risk of rotator cuff damage.

Referring to FIGS. 6A-6Q, yet another humeral component 600 includes an articular surface 602 and a bone-facing side 604 which is opposite to the articular surface. Humeral component 600 includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component 100: planar surfaces 620, 622, 624, 626; lines 619, 621, 623, 625, 627; fillet radii; points 611, 613; and anchoring elements 628, 630, 632. In an alternate version of the technology, the prosthetic humeral component 600 may have an ellipsoid or ovoid articular surface 602, rather than a spherical articular surface. The planar surfaces 620, 622, 624, 626 are in a concave arrangement in which the planar surfaces converge together as they approach the middle of the articular surface 602, as seen best in FIG. 6A.

13

The planar surfaces diverge as they extend away from the middle of the articular surface 602, and intersect the articular surface to establish an articular margin 606 around a perimeter of the humeral component 600. The articular margin may be described as scalloped or having one or more indentations 629. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surface 626 has a smaller area than planar surface 622, and may be described as being indented, or centrally offset, particularly in comparison to planar surface 622. Humeral component 600 includes a fourth anchoring element 634 and a conical surface 674. The illustrated anchoring elements 628, 630, 632, 634 are cylindrical and parallel to one another. Anchoring element 628 may be longer than anchoring elements 630, 632, 634. Anchoring element 634 may be shorter than anchoring elements 628, 630, 632. Anchoring elements 628, 630, 632, 634 also include bilateral longitudinal grooves 636. The conical surface 674 is present around an outermost portion of the bone-facing side 604, and is best seen in FIG. 6D in the vicinity of the outermost portions of lines 621, 623, 625, 627.

Humeral component 600 is bilaterally symmetric about a plane through line 619, and may therefore be implanted in right or left shoulders. Humeral component 600 may be implanted so that planar surface 626 covers a superior aspect of the humeral head, planar surface 622 covers an inferior aspect of the humeral head, planar surfaces 620 and 624 cover anterior and posterior portions of the humeral head, anchoring element 628 extends through the inferior aspect of the humeral head and optionally into the humeral neck, anchoring elements 630, 632 extend into anterior and posterior portions of the humeral head, and anchoring element 634 extends into the superior aspect of the humeral head. The outer portion, or rim, of planar surface 626 faces at least a portion of the rotator cuff, and, because planar surface 626 is indented to form the indentation 629 along the articular margin 606, a space exists between the rim of planar surface 626 and the rotator cuff. This space provides relief, or room, for the rotator cuff to function, thus reducing the risk of rotator cuff damage.

FIGS. 6F and 6G illustrate humeral component 600 in cross sectional views. In each view, two additional smaller size humeral components 600', 600'' are superimposed on humeral component 600 to show certain aspects of the design rationale governing the progression from one size to the next. The illustrated design rationale may apply to any of the humeral components disclosed herein. If humeral component 600 is referred to as a large size, then humeral component 600' is a medium size, and humeral component 600'' is a small size. However, these small, medium, and large size designations are for the purposes of illustration only. It is understood that a full size range of humeral components may include more than three sizes, including sizes larger than humeral component 600, sizes smaller than humeral component 600'', and/or sizes in between those illustrated herein.

The superimposed cross sections of humeral components 600, 600', 600'' reveal that the planar surfaces 620, 622, 624, 626; lines 619, 621, 623, 625, 627; fillet radii; points 611, 613; anchoring elements 628, 630, 632, 634, and conical surface 674 are all identical among the three different sizes. In other words, the same bone preparation—saw cuts, drilled holes, and conical ream—may be performed for all humeral component sizes, and any size humeral component may be implanted onto a particular prepared humerus.

The superimposed cross sections of humeral components 600, 600', 600'' also show that the various articular surfaces 602, 602', 602'' are neither concentric nor tangent. Instead,

14

each articular surface 602, 602', 602'' passes through a defined circle 603, which appears as a pair of points 603 in each FIGS. 6F and 6G. This defined circle 603 may be thought of as a gage circle which has a fixed relationship to the features of the bone-facing side 604. The defined circle may lie in the same plane as line 619, for example, or planar surfaces 744, 844 described below. The articular surface 602'' of the small humeral component 600'' protrudes farther above the circle 603 than do the articular surfaces 602', 602 of the medium and large humeral components 600', 600. Later in this specification, it will be shown that this defined circle 603 may correspond to a depth stop feature on a planar reamer.

Referring to FIGS. 7A-7F, yet another humeral component 700 includes an articular surface 702 and a bone-facing side 704 which is opposite to the articular surface. The articular surface is smooth and polished, and may be spherical, elliptical, or ovoid. Humeral component 700 may be designed with four overlapping circles of a sphere, or as a hemisphere with a tapered, triangular, flat-bottom socket forming the bone-facing side.

Humeral component 700 may include four planar surfaces 744, 762, 764, 766 in a concave arrangement in which the planar surfaces 762, 764, 766 converge together as they approach the middle of the articular surface 702 and the planar surface 744, as seen best in FIG. 7A. Other examples may include three, five, or more planar surfaces in a concave arrangement. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surfaces 744, 762 intersect along a line 757, planar surfaces 744, 764 intersect along a line 759, and planar surfaces 744, 766 intersect along a line 761. Planar surfaces 762, 764; 764, 766; and 766, 762 also intersect when extended. The lines 757, 759, 761 may also be referred to as intersections, edges, or internal corners, and may include fillet radii, as best seen in FIG. 7D. Referring to FIG. 7D, lines 757, 759 intersect at a first point 711; lines 759, 761 intersect at a second point 713; and lines 757, 761 intersect at a third point 715. Humeral component 700 also includes a conical surface 774, which is present in the vicinity of the outermost portions of lines 757, 759, 761, as best seen in FIG. 7D.

The humeral component 700 may have a roughened bone-facing side 704, or undersurface, which rests on the prepared bone of the humerus when the humeral component is implanted. From this undersurface or bone-facing side 704, at least one anchoring element 768 projects outwardly. The example shown includes three anchoring elements 768, 770, 772 protruding from planar surfaces 762, 764, 766, respectively. The anchoring elements project into the humeral bone when the humeral component is implanted, and may anchor the humeral component to prevent loosening or micromotion. The anchoring elements may be pegs which are round, cruciate, or have fins, or have another cross sectional shape for bone fixation. The anchoring elements may include fenestrations. Some of the examples disclosed herein utilize three pegs, but the number of pegs may vary. The pegs may be parallel, converging, diverging, or skew. The pegs may be smooth, matte, rough, or porous to promote bone cement fixation or bone ingrowth. The illustrated anchoring elements 768, 770, 772 are cylindrical and parallel to one another.

Humeral component 700 is bilaterally symmetric about a plane through section line 7F-7F of FIG. 7D, and trilaterally symmetric about an axis normal to planar surface 744. Humeral component 700 may therefore be implanted in right or left shoulders. Humeral component 700 may be implanted so that planar surface 764 covers an inferior aspect of the humeral head, planar surfaces 762 and 766 cover anterior-

15

superior and posterior-superior portions of the humeral head, anchoring element **770** extends through the inferior aspect of the humeral head and optionally into the humeral neck, and anchoring elements **768**, **772** extend into anterior and posterior portions of the humeral head. However, due to its trilateral symmetry, humeral component **700** may also be implanted so that planar surface **762** or planar surface **766** covers the inferior aspect of the humeral head instead of planar surface **764**.

Referring to FIGS. **8A-8D**, yet another humeral component **800** includes an articular surface **802** and a bone-facing side **804** which is opposite to the articular surface.

Humeral component **800** includes the following features, which may be substantially similar to, or the same as, the corresponding features of humeral component **700**: planar surfaces **844**, **862**, **864**, **866**; lines **857**, **859**, **861**; points **811**, **813**, **815**; conical surface **874**; anchoring elements **868**, **870**, **872**. In an alternate version of the technology, the prosthetic humeral component **800** may have an ellipsoid or ovoid articular surface **802**, rather than a spherical articular surface. The planar surfaces **844**, **862**, **864**, **866** are in a concave arrangement in which the planar surfaces **862**, **864**, **866** converge together as they approach the middle of the articular surface **802** and the planar surface **844**, as seen best in FIG. **8A**. Each one of the planar surfaces intersects each other planar surface at an obtuse angle, although right angles and acute angles are also contemplated. Planar surfaces **862**, **864** intersect along a line **863**, planar surfaces **864**, **866** intersect along a line **865**, and planar surfaces **862**, **866** intersect along a line **867**. No fillet radii are shown in this example. The illustrated anchoring elements **868**, **870**, **872** are cylindrical and parallel to one another. Anchoring element **870** also includes four longitudinal grooves **876** which are equally spaced around the anchoring element. Anchoring element **870** may be described as having a cruciate or plus-shaped cross section. Humeral component **800** includes a planar surface **878**, which is present in the vicinity of the outermost portions of planar surfaces **862**, **864**, **866**, as best seen in FIG. **8A**. Planar surface **878** may be parallel to planar surface **844**.

Humeral component **800** is bilaterally symmetric about a plane through section line **8C-8C** of FIG. **8B**, and trilaterally symmetric about an axis normal to planar surface **844**. Humeral component **800** may therefore be implanted in right or left shoulders. Humeral component **800** may be implanted so that planar surface **864** covers an inferior aspect of the humeral head, planar surfaces **862** and **866** cover anterior-superior and posterior-superior portions of the humeral head, anchoring element **870** extends through the inferior aspect of the humeral head and optionally into the humeral neck, and anchoring elements **868**, **872** extend into anterior and posterior portions of the humeral head. However, due to its trilateral symmetry, humeral component **800** may also be implanted so that either planar surface **862** or **866** covers the inferior aspect of the humeral head instead of planar surface **864**.

Referring to FIG. **9A**, a guide wire or pin **900** and a template **1000** are shown in an operative arrangement. The template **1000** may be used to establish the desired orientation of the implanted humeral component relative to the intact proximal humeral anatomy, and may guide insertion of the pin **900** into the humeral head. The desired orientation of the humeral component may relate to an axis which is normal to a central portion of the intact articular surface of the humeral head, or parallel to the intact humeral neck axis.

The pin **900** is a slender elongated shaft **902** which extends between a proximal end **904** and a distal tip **906**. The shaft **902** may be circular in cross-section as shown, or non-circular in

16

cross-section. The proximal end **904** may include a torque connector for connection to a T-handle, drill, or other torque source. The distal tip **906** may be threaded, fluted for cutting, pointed, faceted as in a trocar tip, rounded, or blunt.

Referring to FIGS. **9A-9B**, the template **1000** includes a shaft **1002** which extends between a proximal end **1004** and a distal working portion **1006**. The proximal end **1004** may include a handle or a coupling. The working portion **1006** includes a round perimeter rim **1008** which may be connected to the shaft **1002** by one or more arms **1010**. The example shown includes bilateral straight arms **1010**, **1012** interposed between bilateral bifurcated arms **1014**, **1016**. One or more apertures **1018** may extend between the arms; six apertures **1018** are shown in the example. The working portion **1006** has a bone-facing side **1020** and an opposite side **1022**. The bone-facing side may be concave as shown, convex, or flat. The opposite side **1022** may complement the bone-facing side **1020**. One or more projections **1024** may extend from the rim **1008**; three projections **1024**, **1026**, **1028** are shown, equally spaced around the rim **1008**. The shaft **1002** may include a central cannulation **1030** which receives the pin **900**.

Referring to FIG. **28**, an alignment guide **1100** is shown in use with the pin **900** and the template **1000** relative to a simplified humeral head **40**. The alignment guide **1100** may provide additional anatomical referencing beyond that provided by the template **1000**, in order to set the desired orientation of the implanted humeral component relative to the intact proximal humeral and forearm anatomy.

The alignment guide **1100** includes a shaft **1102** which extends between a proximal handle **1104** and a distal working portion **1106**. In use, the shaft **1102** is aligned with the patient's forearm in consideration of aligning the pin **900** in the desired rotational anteversion and retroversion of the patient. The working portion **1106** includes a plate **1108** and at least one socket **1110** for releasably or permanently coupling to the shaft **1102**. The plate **1108** may include a humeral shaft extension **1112**, an articular bar **1114**, and a post **1116**. The articular bar **1114** may cross the humeral shaft extension **1112** at an oblique angle to form a "T" shape. The post **1116** may extend perpendicular to the articular bar **1114** opposite the humeral shaft extension **1112**. The socket **1110** may be located in the area where the articular bar **1114** crosses the humeral shaft extension **1112**. The working portion **1106** may include a second socket (not visible in FIG. **28**) on an opposite side of the plate **1108** from the socket **1110**. The shaft **1102** may be releasably coupled to either socket to provide configurations suitable for right or left shoulder procedures.

Referring to FIGS. **10A-10B**, the pin **900** and a planar reamer **1400** are shown in an operative arrangement. The planar reamer **1400** may be used to cut a planar bone resection **44** which is perpendicular to the axis of the pin **900** and which may have an outer diameter corresponding to the defined circle **603**. The bone resection **44** may correspond to planar surfaces **744**, **844**, or it may correspond to lines **119**, **219**, **319**, **419**, **519**, **619**.

The planar reamer **1400** includes a shaft **1402** which extends between a proximal end **1404** and a distal working portion **1406**. The proximal end **1404** may include a handle or a coupling; a torque coupling **1405** is shown for coupling the planar reamer **1400** to a T-handle, drill, or other torque driver. The working portion **1406** includes a round perimeter rim **1408** which may be connected to the shaft **1402** by one or more arms **1410**. The example shown includes bilateral arms **1410**, **1412**. One or more apertures **1418** may extend between the arms; two apertures are shown in the example. The working portion **1406** has a bone-facing side **1420** and an opposite

17

side **1422**. The bone-facing side **1420** is flat. Cutting features **1424** are present on the bone-facing side **1420**. In this example, the cutting features **1424** include a series of alternating teeth **1426** and grooves **1428** with concentric circular patterns of crossing grooves **1429**, which may be referred to as chip breakers. Relief channels **1432** may be included around the outer portion of each arm **1410**, **1412** to provide clearance for the tools used to fabricate the cutting features **1424** and/or to delimit an outer diameter of the cutting features. A continuous smooth planar surface **1434** extends completely around the perimeter rim **1408** on the bone-facing side **1420**, forming a boundary within which all of the cutting features **1424** are contained. The surface **1434** may be coplanar with the cutting features **1424**, for example the peaks of the teeth **1426** or the valleys of the grooves **1428**. Alternatively, the surface **1434** may lie above or below the cutting features. The surface **1434** functions as a depth stop in use, as will be described later. An inner edge **1436** of the surface **1434**, excluding any interruption caused by the relief channels **1432**, may correspond to the defined circle **603** described above. The opposite side **1422** may complement the bone-facing side **1420**. The shaft **1402** may include a central cannulation **1430** which receives the pin **900**.

Another example of a planar reamer has a plurality of arms that extend radially from the shaft to the rim like spokes on a wheel. This example may or may not have the continuous smooth planar surface that extends completely around the perimeter rim on the bone-facing side. This example may have one or more radially extending cutting teeth per arm. Because this example has through openings between the cutting teeth, the bone and articular cartilage fragments are more easily cleared and the reamer is less likely to clog while reaming.

Referring to FIGS. 11A-11B, a conical reamer **1500** includes a shaft **1502** which extends between a proximal end **1504** and a distal working portion **1506**. The conical reamer **1500** may be used to cut a conical bone resection **74** which corresponds to conical surface **674**, **774**, **874**. The proximal end **1504** may include a handle or a coupling; a blunt proximal end is shown. The working portion **1506** includes a round perimeter rim **1508** which may be connected to the shaft **1502** by one or more arms **1510**. The example shown includes a plurality of radially extending arms **1510**. One or more apertures **1518** may extend between the arms; a plurality of apertures is shown in the example. However, a roughened file-like tissue-cutting surface may also extend the working portion **1506** allowing rasp-like tissue removal. The working portion **1506** has a bone-facing side **1520** and an opposite side **1522**. The bone-facing side includes a conical surface **1512** surrounding a central planar surface **1514** which is perpendicular to the shaft **1502**. Cutting features **1524** are present on the bone-facing side. In this example, the cutting features **1524** include a series of radial teeth **1526** on the leading side of each arm **1510** (depending on the direction of rotation, clockwise or counterclockwise). A relief channel **1532** may be included between the central planar surface **1514** and the conical surface **1512**. The planar surface **1514** functions as a depth stop in use, as will be described later. The opposite side **1522** may complement the bone-facing side **1520**. The shaft **1502** may include a central cannulation **1530** which receives the pin **900**.

Specific preparations of the proximal humeral bone surface are disclosed in order to accommodate the multi-planar undersurfaces of the prosthetic components so the undersurfaces rests flush against the bone. The proximal humeral bone may be prepared with the use of a cutting guide which rests on the head of the humerus. The cutting guide has slots which

18

guide a cutting tool such as an oscillating saw blade to make bone cuts corresponding to the particular design of the undersurface of the humeral prosthesis. The humeral cutting guide may be designed to be used by a surgeon utilizing a standard subscapularis tenotomy or lesser tuberosity osteotomy, but may also be adapted to a surgeon utilizing a subscapularis-preserving technique. Various cutting guides will now be described.

Referring to FIGS. 12A-12J, a cutting guide **1600** may be referred to as a cut and drill guide or as an all in one guide. The cutting guide **1600** may be used to guide a cutting tool, such as a saw blade, to cut four planar bone resections **20**, **22**, **24**, **26** corresponding to planar surfaces **120**, **122**, **124**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. The cutting guide **1600** may also be used to guide a cutting tool, such as a drill or reamer, to cut bone holes **28**, **30**, **32** corresponding to anchoring elements **128**, **130**, **132** of humeral component **100**, or the anchoring elements of humeral components **200**, **300**, **400**, **500**, **600**. The cutting guide **1600** may also serve the function of the template **1000**.

The cutting guide **1600** includes a cylindrical body **1608** terminating at one end in a spherical shell or cup **1610**. The cutting guide **1600** has a bone-facing side **1609** which includes the perimeter rim and concave interior of the spherical cup **1610**. Three holes **1628**, **1630**, **1632** extend lengthwise through the cutting guide **1600**, corresponding to the relative arrangement of anchoring elements **128**, **130**, **132** of humeral component **100**, or the anchoring elements of humeral components **200**, **300**, **400**, **500**, **600**. A fourth hole (not shown) may be included in the cutting guide **1600**, corresponding to anchoring elements **434**, **534**, **634** of humeral components **400**, **500**, **600**. One or more apertures **1612** may also extend lengthwise through the cutting guide **1600** to provide visualization windows and/or to reduce weight. Three apertures **1612**, **1613**, **1614** are shown in the example, interposed between the holes **1628**, **1630**, **1632**. Four slots **1620**, **1622**, **1624**, **1626** extend obliquely through the cutting guide **1600**, corresponding to the relative arrangement of planar surfaces **120**, **122**, **124**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. It will be appreciated that the number and arrangement of holes and/or slots in the illustrated cutting guide **1600** may be modified to correspond to the number and arrangement of anchoring elements and/or planar surfaces of humeral components **700**, **800**. One or more holes **1616** may extend through the cutting guide **1600** near the rim of the spherical cup **1610** to receive pins to fix the cutting guide **1600** to the humeral head prior to making any bone resections or holes; ten holes **1616**, **1646**, **1647**, **1648**, **1649**, **1650**, **1651**, **1652**, **1653**, **1654** are shown. Holes **1646**, **1647**, **1648**, **1651**, **1652**, **1653** are all parallel, and holes **1646**, **1653**; **1647**, **1652**; and **1648**, **1651** are coaxial. Referring to FIG. 12E, one or more projections **1656** may extend from the interior of the spherical cup **1610** to engage the articular surface of the humeral head. The example shows three projections **1656**, **1657**, **1658**.

Referring to FIGS. 13A-13B, a cutting guide **1800**, the pin **900**, and two fasteners **1890**, **1892** are shown in an operative arrangement. The cutting guide **1800** may be referred to as an anterior-posterior or A-P cutting guide or as a medial-lateral or M-L cutting guide. The cutting guide **1800** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **20**, **24** corresponding to planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **1800** includes a body **1808** with a bone-facing side **1809**. The bone-facing side **1809** includes a planar surface **1844**. Two slots **1820**, **1824** extend obliquely through the cutting guide **1800**, corresponding to the relative arrangement of planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. The slots **1820**, **1824** may intersect at the planar surface **1844**. One or more holes **1816** may extend through the cutting guide **1800** near opposing apices or ends of the body **1808** to receive fasteners **1890**, **1892** to fix the cutting guide **1800** to the humeral head prior to making any bone resections; two converging holes **1816**, **1846** are shown. A central hole **1818** may extend through the cutting guide **1800** to receive pin **900**.

Referring to FIGS. **14A-14B**, a cutting guide **1900** and two fasteners **1990**, **1992** are shown in an operative arrangement. The cutting guide **1900** may be referred to as an anterior-posterior or A-P cutting guide or as a medial-lateral or M-L cutting guide. The cutting guide **1900** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **20**, **24** corresponding to planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **1900** includes a shaft **1902** which extends between a proximal handle **1904** and a distal working portion **1906**. The distal working portion **1906** may be releasably or permanently coupled to the shaft **1902**. The distal working portion **1906** includes the following features, which may be substantially similar to, or the same as, the corresponding features of the cutting guide **1800**: body **1908**; bone-facing side **1909**; planar surface **1944**; slots **1920**, **1924**; and converging holes **1916**, **1946**. The slots **1920**, **1924** extend obliquely through the cutting guide **1900**, corresponding to the relative arrangement of planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. The slots **1920**, **1924** may intersect at the planar surface **1944**. A central socket or hole **1918** may receive shaft **1902**.

Referring to FIGS. **15A-15B**, a cutting guide **2000**, pin **900**, and four fasteners **2090**, **2092**, **2094**, **2096** are shown in an operative arrangement. The cutting guide **2000** may be referred to as a modular anterior-posterior or A-P cutting guide, or as a modular medial-lateral or M-L cutting guide. The cutting guide **2000** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **20**, **24** corresponding to planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **2000** includes a first body **2008** with a bone-facing side **2009**. The bone-facing side **2009** includes a planar surface **2044**. A slot **2020** extends obliquely through the first body **2008**, corresponding to the planar surface **120** of humeral component **100**, or the planar surface of humeral components **200**, **300**, **400**, **500**, **600**. One or more holes **2016** may extend through the first body **2008** near opposing apices or ends of the body to receive fasteners **2090**, **2092** to fix the first body **2008** to the humeral head prior to making any bone resections; two converging holes **2016**, **2046** are shown. A central hole **2018** may extend through the first body **2008** to receive pin **900**. The first body **2008** includes a protrusion **2010** which extends from the first body next to the slot **2020**. The protrusion **2010** may have a rectangular, notched, dovetail, or other cross sectional shape typical of a guide rail. A window **2011** or loop extends from the first body opposite the slot **2020**.

The cutting guide **2000** includes a rectangular second body **2012** with a slot **2014** that is complementary to the protrusion

2010 and sized for a clearance fit. The slot **2014** slidably receives the protrusion **2010**. The second body **2012** includes a fastener **2017** which locks the second body to the protrusion **2010** at a desired location. A slot **2024** extends through the second body. When the second body **2012** is operatively assembled to the first body **2008** and the cutting guide **2000** is secured to a humeral head, slot **2024** corresponds to the planar surface **124** of humeral component **100**, or the planar surface of humeral components **200**, **300**, **400**, **500**, **600**. One or more holes **2046** may extend through the second body **2012** to receive fasteners **2094**, **2096** to fix the second body to the humerus prior to making any bone resections; three diverging holes **2046**, **2047**, **2048** are shown.

Referring to FIG. **16**, a cutting guide **2100**, pin **900**, and four fasteners **2090**, **2092**, **2094**, **2096** are shown in an operative arrangement. The cutting guide **2100** may be referred to as a modular anterior-posterior or A-P cutting guide or as a modular medial-lateral or M-L cutting guide. The cutting guide **2100** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **20**, **24** corresponding to planar surfaces **120**, **124** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **2100** includes a shaft **2102** which extends between a proximal handle **2104** and a distal working portion **2106**. The working portion **2106** includes a first body **2108** and a rectangular second body **2112**. The first body **2108** includes the following features, which may be substantially similar to, or the same as, the corresponding features of the first body **2008**: bone-facing side **2109**; planar surface **2144**; slot **2120**; converging holes **2116**, **2146**; protrusion **2110**; and window **2111** or loop. A central socket or hole **2118** may receive shaft **2102**. The second body **2112** includes the following features, which may be substantially similar to, or the same as, the corresponding features of the second body **2012**: slot **2114**; fastener **2116**; slot **2124**; holes **2146**, **2147**, **2148**.

Referring to FIGS. **17A-17C**, a cutting guide **2300** and three fasteners **2390**, **2392**, **2394** are shown in an operative arrangement. The cutting guide **2300** may be referred to as a cut and drill guide or as a superior-inferior or S-I cutting guide. The cutting guide **2300** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **22**, **26** corresponding to planar surfaces **122**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. The cutting guide **2300** may also be used to guide a cutting tool, such as a drill or reamer, to cut bone holes **28**, **30**, **32** corresponding to anchoring elements **128**, **130**, **132** of humeral component **100**, or the anchoring elements of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **2300** includes a body **2308** with a bone-facing side **2309**. The bone-facing side **2309** includes intersecting planar surfaces **2320**, **2324**. Three holes **2328**, **2330**, **2332** extend lengthwise through the cutting guide **2300**, corresponding to the relative arrangement of anchoring elements **128**, **130**, **132** of humeral component **100**, or the anchoring elements of humeral components **200**, **300**, **400**, **500**, **600**. A fourth hole **2334** may be included in the cutting guide **2300**, corresponding to anchoring elements **434**, **534**, **634**. Two slots **2322**, **2326** extend obliquely through the cutting guide **2300**, corresponding to the relative arrangement of planar surfaces **122**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. One or more holes **2316** may extend through the cutting guide **2300** near opposing apices or ends of the body **2308** to receive fasteners **2392**, **2394** to fix the cutting guide **2300** to the

21

humeral head prior to making any bone resections; two converging holes **2316**, **2346** are shown. A central hole **2318** may extend through the cutting guide **2300** to receive fastener **2390**. Fastener **2390** may be countersunk or otherwise recessed into the cutting guide **2300** to avoid occluding the slots **2322**, **2326**. Cutting guide **2300** may be secured by fastener **2390** alone, by fasteners **2392**, **2394**, by any two of fasteners **2390**, **2392**, **2394**, or by all three fasteners.

Referring to FIG. **18**, a cutting guide **2400** and two fasteners **2492**, **2494** are shown in an operative arrangement. The cutting guide **2400** may be referred to as a cut and drill guide or as a superior-inferior or S-I cutting guide. The cutting guide **2400** may be used to guide a cutting tool, such as a saw blade, to cut two planar bone resections **22**, **26** corresponding to planar surfaces **122**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. The cutting guide **2400** may also be used to guide a cutting tool, such as a drill or reamer, to cut bone holes **28**, **30**, **32** corresponding to anchoring elements **128**, **130**, **132** of humeral component **100**, or the anchoring elements of humeral components **200**, **300**, **400**, **500**, **600**.

The cutting guide **2400** includes a shaft **2402** which extends between a proximal handle **2404** and a distal working portion **2406**. The distal working portion **2406** may be releasably or permanently coupled to the shaft **2402** by threads or by releasable connection mechanisms. The distal working portion **2406** includes the following features, which may be substantially similar to, or the same as, the corresponding features of the cutting guide **2300**: body **2408**; bone-facing side **2409**; intersecting planar surfaces **2420**, **2424** (not visible in FIG. **18**); holes **2428**, **2430**, **2432**, **2434**; slots **2422**, **2426**; and converging holes **2416**, **2446**. The slots **2422**, **2426** extend obliquely through the cutting guide **2400**, corresponding to the relative arrangement of planar surfaces **122**, **126** of humeral component **100**, or the planar surfaces of humeral components **200**, **300**, **400**, **500**, **600**. A central socket or hole **2418** may receive shaft **2402**.

Referring to FIGS. **19A-19B**, a cutting guide **2500** and three fasteners **2590**, **2592**, **2594** are shown in FIG. **19B** in an operative arrangement. The cutting guide **2500** may be referred to as a cut and drill guide. The cutting guide **2500** may be used to guide a cutting tool, such as a saw blade, to cut three planar bone resections **62**, **64**, **66** corresponding to planar surfaces **762**, **764**, **766** of humeral component **700**, or planar surfaces **862**, **864**, **866** of humeral component **800**. The cutting guide **2500** may also be used to guide a cutting tool, such as a drill or reamer, to cut bone holes **68**, **70**, **72** corresponding to anchoring elements **768**, **770**, **772** of humeral component **700**, or anchoring elements **868**, **870**, **872** of humeral component **800**.

The cutting guide **2500** includes a star-shaped body **2508** with a bone-facing side **2509** which includes a planar surface **2544**. Three holes **2568**, **2570**, **2572** extend lengthwise through the cutting guide **2500**, corresponding to the relative arrangement of anchoring elements **768**, **770**, **772** of humeral component **700**, or anchoring elements **868**, **870**, **872** of humeral component **800**. Three slots **2562**, **2564**, **2566** extend obliquely through the cutting guide **2500**, corresponding to the relative arrangement of planar surfaces **762**, **764**, **766** of humeral component **700**, or planar surfaces **862**, **864**, **866** of humeral component **800**. One or more holes **2516** may extend through a central portion of the cutting guide **2500** to receive fasteners **2590**, **2592**, **2594** to fix the cutting guide **2500** to the humeral head prior to making any bone resections or holes; three skew holes **2546**, **2547**, **2548** are shown. The fasteners **2590**, **2592**, **2594** may be countersunk or otherwise recessed into the cutting guide **2500** to avoid occluding the slots **2562**,

22

2564, **2566**. A central hole **2518** may extend through the cutting guide **1800** to receive pin **900**.

Referring to FIGS. **20A-20B**, a proximal humerus **2** includes a humeral head **4**. Referring to FIGS. **21A-26B**, a method of preparing a proximal humerus for implantation of a humeral component **100**, **200**, **300**, **400**, **500**, **600** may include some or all of the steps of cutting a first planar bone resection **20** to remove a posterior aspect of the humeral head **4**; cutting a second planar bone resection **22** to remove an inferior aspect of the humeral head **4**; cutting a third planar bone resection **24** to remove an anterior aspect of the humeral head **4**; cutting a fourth planar bone resection **26** to remove a superior aspect of the humeral head **4**; cutting a first bone hole **28** in an inferior aspect of the humeral head **4**; cutting second bone hole **30** in an anterior aspect of the humeral head **4**; cutting a third bone hole **32** in a posterior aspect of the humeral head **4**; and cutting a conical bone resection **74** on the humeral head **4** (as shown in FIG. **42**). The steps may be performed in any order, and additional steps may be performed.

With continued reference to FIGS. **21A-26B**, with brief reference to FIGS. **12A-12J**, another method of preparing a proximal humerus for implantation of a humeral component **100**, **200**, **300**, **400**, **500**, **600** may include some or all of the steps of placing the bone-facing side **1609** of the cutting guide **1600** against an intact humeral head **4**; aligning the cutting guide **1600** in a desired orientation relative to the intact proximal humeral anatomy so that the projections **1656**, **1657**, **1658** contact the humeral head; securing the cutting guide **1600** to the proximal humerus by driving at least one pin through any of the holes **1616**, **1646**, **1647**, **1648**, **1649**, **1650**, **1651**, **1652**, **1653**, **1654**; cutting four planar bone resections **20**, **22**, **24**, **26** by actuating a saw through each slot **1620**, **1622**, **1624**, **1626**; cutting three bone holes **28**, **30**, **32** by actuating a drill through each hole **1628**, **1630**, **1632**; removing the pins, the cutting guide **1600**, and bone fragments or debris; and optionally cutting a conical bone resection **74** with conical reamer **1500**.

Additional methods of preparing a proximal humerus for implantation of a humeral component may include some or all of the steps of establishing a humeral head axis; cutting anterior and posterior planar bone resections; cutting superior and inferior planar bone resections; and cutting bone holes. Each step is described below as a separate method.

Referring to FIGS. **27-29**, with brief reference to FIGS. **9A-9B**, a method of establishing a humeral head axis **6** may include some or all of the steps of placing the bone-facing side **1020** of the template **1000** against an intact humeral head **40**, which is shown in simplified form as a hemisphere; aligning the humeral shaft extension **1112** of the alignment guide **1100** with the humeral shaft; aligning the articular bar **1114** of the alignment guide **1100** with the articular margin of the humeral head **40**; aligning the template **1000** in a desired orientation relative to the intact proximal humeral anatomy so that the projections **1024**, **1026**, **1028** contact the humeral head **40**, wherein aligning the template **1000** may include aligning the shaft **1002** parallel with the post **1116**; driving the pin **900** through the cannulation **1030** and into the humeral head **40**; and removing the template **1000** and alignment guide **1100**. FIG. **29** shows the simplified humeral head **40** with a central bone hole **18** created by driving the pin **900** into the humeral head **40**. The humeral head axis **6** is the central longitudinal axis of the hole **18**, and may be normal to a central portion of the intact articular surface of the humeral head **40**, or parallel to the humeral neck axis.

Referring to FIGS. **30** and **31**, with brief reference to FIGS. **10A-10B**, a method of cutting a planar bone resection **44** may

23

occur after the method of establishing the humeral head axis 6, and may include some or all of the steps of inserting the pin 900 into the cannulation 1430 of the planar reamer 1400; advancing the planar reamer 1400 over the pin 900 to contact the humeral head 40; cutting the planar bone resection 44 by actuating the planar reamer 1400 until the continuous smooth planar surface 1434, or the inner edge 1436 of the surface, contacts the humeral head to stop further bone removal by the planar reamer 1400; and removing the planar reamer. FIG. 31 shows the simplified humeral head 40 with the planar bone resection 44 around the bone hole 18. The planar bone resection 44 is normal to the humeral head axis 6.

Referring to FIGS. 32 and 35, with brief reference to FIGS. 13A-14, a method of cutting anterior and posterior planar bone resections 20, 24 may occur after the method of cutting the planar bone resection 44, and may include some or all of the steps of inserting the pin 900 into the central hole 1818 of the cutting guide 1800; advancing the cutting guide 1800 over the pin 900 to contact the humeral head 40, wherein the planar surface 1844 contacts the planar bone resection 44; securing the cutting guide 1800 to the humeral head 40 by driving at least one fastener 1890, 1892 through any of the holes 1816, 1846; removing the pin 900; cutting two planar bone resections 20, 24 by actuating a saw through each slot 1820, 1824; and removing the fastener(s) 1890, 1892 and the cutting guide 1800. FIG. 35 shows the simplified humeral head 40 with the planar bone resections 20, 24. Cutting guide 1800 may be replaced by cutting guide 1900 in this method, in which case the shaft 1902 and handle 1904 may be used to push the distal working portion 1906 against the humeral head 40 for added stability during one or more of the steps of securing the cutting guide 1900 to the humeral head 40; removing the pin 900; and cutting two planar bone resections 20, 24.

Referring to FIGS. 33-35, with brief reference to FIGS. 15A-16, another method of cutting anterior and posterior planar bone resections 20, 24 may occur after the method of cutting the planar bone resection 44, and may include some or all of the steps of inserting the pin 900 into the central hole 2018 of the first body 2008 of the cutting guide 2000; advancing the first body 2008 over the pin 900 to contact the humeral head 40, wherein the planar surface 2044 contacts the planar bone resection 44; securing the first body 2008 to the humeral head 40 by driving at least one fastener 2090, 2092 through any of the holes 2016, 2046; removing the pin 900; inserting the protrusion 2010 into the slot 2014 of the second body 2012; advancing the second body 2012 over the protrusion 2010 to contact the humeral head 40; securing the second body 2012 to the protrusion 2010 by actuating the fastener 2017; securing the second body 2012 to the humeral head by driving at least one fastener 2094, 2096 through any of the holes 2046, 2047, 2048; cutting two planar bone resections 20, 24 by actuating a saw through each slot 2020, 2024; and removing the fastener(s) 2090, 2092, 2094, 2096 and the cutting guide 2000. FIG. 35 shows the simplified humeral head 40 with the planar bone resections 20, 24. Cutting guide 2000 may be replaced by cutting guide 2100 in this method, in which case the shaft 2102 and handle 2104 may be used to push the first body 2008 against the humeral head 40 for added stability during one or more of the steps of securing the first body 2108 to the humeral head 40; removing the pin 900; inserting the protrusion 2110 into the slot 2114 of the second body 2112; advancing the second body 2112 over the protrusion 2110 to contact the humeral head 40; securing the second body 2112 to the protrusion 2110; securing the second body 2112 to the humeral head; and cutting two planar bone resections 20, 24.

24

Referring to FIGS. 36-38, with brief reference to FIGS. 17A-18, a method of cutting superior and inferior planar bone resections 22, 26 and bone holes 28, 30, 32, 34 may occur after the method of cutting anterior and posterior planar bone resections 20, 24, and may include some or all of the steps of placing the cutting guide 2300 against the humeral head 40 so that the planar surface 2320 contacts the planar bone resection 20 and the planar surface 2324 contacts the planar bone resection 24; securing the cutting guide 2300 to the humeral head 40 by driving at least one fastener 2390, 2392, 2394 through any of the holes 2316, 2318, 2346; cutting two planar bone resections 22, 26 by actuating a saw through each slot 2322, 2326; cutting four bone holes 28, 30, 32, 34 by actuating a drill through holes 2328, 2330, 2332, 2334; and removing the fastener(s) 2390, 2392, 2394 and the cutting guide 2300. FIG. 38 shows the simplified humeral head 40 with the planar bone resections 22, 26 and bone holes 28, 30, 32, 34. Cutting guide 2300 may be replaced by cutting guide 2400 in this method, in which case the shaft 2402 and handle 2404 may be used to push the cutting guide 2400 against the humeral head 40 for added stability during one or more of the steps of securing the cutting guide 2300 to the humeral head 40; cutting two planar bone resections 22, 26; and cutting four bone holes 28, 30, 32, 34.

Referring to FIGS. 39-40, with brief reference to FIGS. 19A-19B, a method of cutting inferior, antero-superior, and postero-superior planar bone resections 64, 62, 66 and bone holes 70, 68, 72 may occur after the method of cutting the planar bone resection 44, and may include some or all of the steps of inserting the pin 900 into the central hole 2518 of the cutting guide 2500; advancing the cutting guide 2500 over the pin 900 to contact the humeral head 4, wherein the planar surface 2544 contacts the planar bone resection 44; securing the cutting guide 2500 to the humeral head 4 by driving at least one fastener 2590, 2592, 2594 through any of the holes 2546, 2547, 2548; removing the pin 900; cutting three planar bone resections 62, 64, 66 by actuating a saw through holes 2562, 2564, 2566; cutting three bone holes 68, 70, 72 by actuating a drill through each hole 68, 70, 72; and removing the cutting guide 2500 and fastener(s) 2590, 2592, 2594. FIG. 40 shows the humeral head 4 with the planar bone resections 62, 64, 66 and bone holes 68, 70, 72.

Referring to FIGS. 41-42, with brief reference to FIGS. 11A-11B, a method of cutting a conical bone resection 74 may occur after any of the methods of cutting planar bone resections and/or bone holes, and is illustrated as if it occurs after the method of cutting inferior, antero-superior, and postero-superior planar bone resections 64, 62, 66 and bone holes 70, 68, 72. The method of cutting the conical bone resection 74 may include some or all of the steps of inserting the pin 900 into the cannulation 1530 of the conical reamer 1500; advancing the conical reamer 1500 over the pin 900 to contact the humeral head 4; cutting the conical bone resection 74 by actuating the conical reamer 1500 until the planar surface 1514 contacts the humeral head to stop further bone removal by the conical reamer 1500, wherein the planar surface 1514 may contact the planar surface 44; and removing the conical reamer. FIG. 42 shows the humeral head 4 with the conical bone resection 74 around the humeral head 4.

Referring to FIG. 43, humeral component 700 is shown implanted on the humeral head 4 of FIG. 42.

The components disclosed herein may be fabricated from metals, alloys, polymers, plastics, ceramics, glasses, composite materials, or combinations thereof, including but not limited to: PEEK, titanium, titanium alloys, commercially pure titanium grade 2, ASTM F67, Nitinol, cobalt chrome, stainless steel, ultra high molecular weight polyethylene (UHM-

25

WPE), biocompatible materials, and biodegradable materials, among others. Different materials may be used for different parts. Coatings may be present. Different materials may be used within a single part. Any component disclosed herein may be colored, coded or otherwise marked to make it easier for a user to identify the type and size of the component, the setting, the function(s) of the component, and the like.

It should be understood that the present systems, kits, apparatuses, and methods are not intended to be limited to the particular forms disclosed. Rather, they are to cover all combinations, modifications, equivalents, and alternatives falling within the scope of the claims.

The claims are not to be interpreted as including means-plus- or step-plus-function limitations, unless such a limitation is explicitly recited in a given claim using the phrase(s) “means for” or “step for,” respectively.

The term “coupled” is defined as connected, although not necessarily directly, and not necessarily mechanically.

The use of the word “a” or “an” when used in conjunction with the term “comprising” in the claims and/or the specification may mean “one,” but it is also consistent with the meaning of “one or more” or “at least one.” The term “about” means, in general, the stated value plus or minus 5%. The use of the term “or” in the claims is used to mean “and/or” unless explicitly indicated to refer to alternatives only or the alternative are mutually exclusive, although the disclosure supports a definition that refers to only alternatives and “and/or.”

The terms “comprise” (and any form of comprise, such as “comprises” and “comprising”), “have” (and any form of have, such as “has” and “having”), “include” (and any form of include, such as “includes” and “including”) and “contain” (and any form of contain, such as “contains” and “containing”) are open-ended linking verbs. As a result, a method or device that “comprises,” “has,” “includes” or “contains” one or more steps or elements, possesses those one or more steps or elements, but is not limited to possessing only those one or more elements. Likewise, a step of a method or an element of a device that “comprises,” “has,” “includes” or “contains” one or more features, possesses those one or more features, but is not limited to possessing only those one or more features. Furthermore, a device or structure that is configured in a certain way is configured in at least that way, but may also be configured in ways that are not listed.

In the foregoing Detailed Description, various features are grouped together in several examples for the purpose of streamlining the disclosure. This method of disclosure is not to be interpreted as reflecting an intention that the examples of the invention require more features than are expressly recited in each claim. Rather, as the following claims reflect, inventive subject matter lies in less than all features of a single disclosed example. Thus, the following claims are hereby incorporated into the Detailed Description, with each claim standing on its own as a separate example.

The invention claimed is:

1. An arthroplasty prosthesis comprising:

an articular surface; and

a bone-facing side opposite the articular surface;

wherein the bone-facing side comprises a concave arrangement of at least three planar surfaces, wherein the at least three planar surfaces converge toward the articular surface, wherein the first planar surface intersects the second planar surface along a first line, wherein the second planar surface intersects the third planar surface along a second line, wherein the third planar surface intersects the first planar surface along a third line, wherein the first, second, and third lines converge together as the first, second, and third lines approach the articular sur-

26

face, wherein the at least three planar surfaces intersect the articular surface to establish an articular margin of the prosthesis, wherein the articular margin includes an indentation located where a selected one of the at least three planar surfaces intersects the articular surface.

2. The prosthesis of claim 1, wherein the at least three planar surfaces intersect each other.

3. The prosthesis of claim 1, wherein, when the prosthesis is operatively implanted with the bone-facing side facing a prepared humeral head and the articular surface facing into a shoulder joint, the indentation faces and is spaced apart from at least a portion of a rotator cuff.

4. The prosthesis of claim 1, wherein the bone-facing side comprises a concave arrangement of at least four planar surfaces.

5. The prosthesis of claim 4, wherein the at least four planar surfaces converge toward the articular surface.

6. The prosthesis of claim 4, wherein three of the at least four planar surfaces are radially arranged about a remaining one of the at least four planar surfaces.

7. The prosthesis of claim 1, wherein the articular surface has a shape selected from the group consisting of a spherical shape, an ellipsoid shape, and an ovoid shape.

8. The prosthesis of claim 1, wherein the at least three planar surfaces converge toward a central portion of the articular surface, wherein the at least three planar surfaces intersect a peripheral portion of the articular surface to establish the articular margin of the prosthesis.

9. An arthroplasty prosthesis comprising:

an articular surface; and

a bone-facing side opposite the articular surface, wherein the bone-facing side comprises a first planar surface, a second planar surface, and a third planar surface, wherein the first, second, and third planar surfaces converge toward a center of the articular surface and diverge toward a perimeter of the articular surface, wherein the first planar surface intersects the second planar surface along a first line, wherein the second planar surface intersects the third planar surface along a second line, wherein the third planar surface intersects the first planar surface along a third line, wherein the first and second lines intersect, wherein the first, second, and third lines converge.

10. The prosthesis of claim 9, wherein the first, second, and third planar surfaces converge toward the articular surface.

11. The prosthesis of claim 9, wherein the bone-facing side comprises a fourth planar surface, wherein the fourth planar surface intersects at least one planar surface along a third line, wherein the at least one planar surface is selected from the group consisting of the first, second, and third planar surface.

12. The prosthesis of claim 11, wherein the first, second, third, and fourth planar surfaces are in a concave arrangement and converge toward the articular surface.

13. The prosthesis of claim 11, wherein the first, second, and third planar surfaces are radially arranged about the fourth planar surface.

14. The prosthesis of claim 9, wherein the articular surface has a shape selected from the group consisting of a spherical shape, an ellipsoid shape, and an ovoid shape.

15. An arthroplasty prosthesis comprising:

an articular surface; and

a bone-facing side opposite the articular surface, wherein the bone-facing side comprises a socket with at least three planar side walls, wherein the at least three planar side walls taper inwardly as the socket extends from the bone-facing side toward the articular surface, wherein the at least three planar side walls intersect a perimeter of

the articular surface, wherein the at least three planar side walls intersect each other.

16. The prosthesis of claim **15**, wherein the socket comprises a fourth planar wall.

17. The prosthesis of claim **16**, wherein the fourth planar wall is a side wall, wherein the at least three planar side walls and the fourth planar wall converge toward the articular surface.

18. The prosthesis of claim **16**, wherein the at least three planar side walls are radially arranged about the fourth planar wall.

19. The prosthesis of claim **15**, wherein the articular surface has a shape selected from the group consisting of a spherical shape, an ellipsoid shape, and an ovoid shape.

20. The prosthesis of claim **15**, wherein the at least three planar side walls taper inwardly as the socket extends from the bone-facing side toward a central portion of the articular surface.

* * * * *